

1 Synthetic intracellular nanostructures enhance cytotoxic T cell function via 2 assembly-driven chemical engineering

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14 15 Abstract

16 Nature achieves diverse biological functions through structure formation. Inspired by the controlled
17 formation of polypeptide nanostructures in cells, synthetic methods have been developed to assemble
18 artificial nanostructures and organelle-like compartments within living cells. While these synthetic
19 intracellular assemblies have mostly been used to disrupt cellular processes, their potential to induce
20 a gain of function within cells remains unexplored. Here, we introduce redox-sensitive *isopeptides* that
21 transform into self-assembling linear peptides inside human cytotoxic T cells in response to intracellular
22 levels of glutathione. The *in situ* formation of synthetic peptide nanostructures in cytotoxic T cells leads
23 to cellular stiffening, establishing a direct interface between biochemically driven peptide assembly
24 and mechanobiological effects. This change in biophysical properties, along with increased
25 phosphorylation of signaling proteins associated with T cell activation, correlates with a significant
26 enhancement in the efficacy of cytotoxic T cells to eliminate cancer cells. Our findings elucidate the
27 cellular impact of synthetic peptide nanostructures assembled within living cytotoxic T cells and
28 demonstrate their ability to modulate and enhance effector immune cell responses.

29 30 Introduction

31 Naturally occurring intracellular nanostructures, such as microtubules, actin filaments, and
32 intermediate filaments that form the cytoskeleton, play a critical role in fundamental cellular
33 processes, including metabolism, division and motility.¹ These complex, dynamic protein assemblies
34 span the cytosol and provide a blueprint for the development of synthetic materials designed to form
35 nanostructures in synthetic cells, a growing frontier in biomolecular engineering.² Moreover, the
36 creation of synthetic architectures inside the complex environment of mammalian cells represents a
37 significant milestone in nanomedicine and synthetic biology, providing a bottom-up approach that
38 mimics natural intracellular assemblies and opens new avenues for supramolecular drug design.³

39 To date, advances in the creation of intracellular assemblies have primarily focused on the formation
40 of synthetic nanostructures within cancerous cells with the goal of disrupting cellular metabolism and
41 inducing apoptosis.^{4,5} State-of-the-art strategies involve the use of bioresponsive molecules that can
42 undergo chemical transformations in response to endogenous stimuli, enabling spatiotemporal control

43 and selectivity over the assembly formation.^{3,6-10} However, these efforts to construct synthetic
44 intracellular nanostructures have so far been limited to malignant cells^{4,5}, leaving the potential to
45 modulate the behavior of non-cancerous cells, particularly immune cells, unexplored.

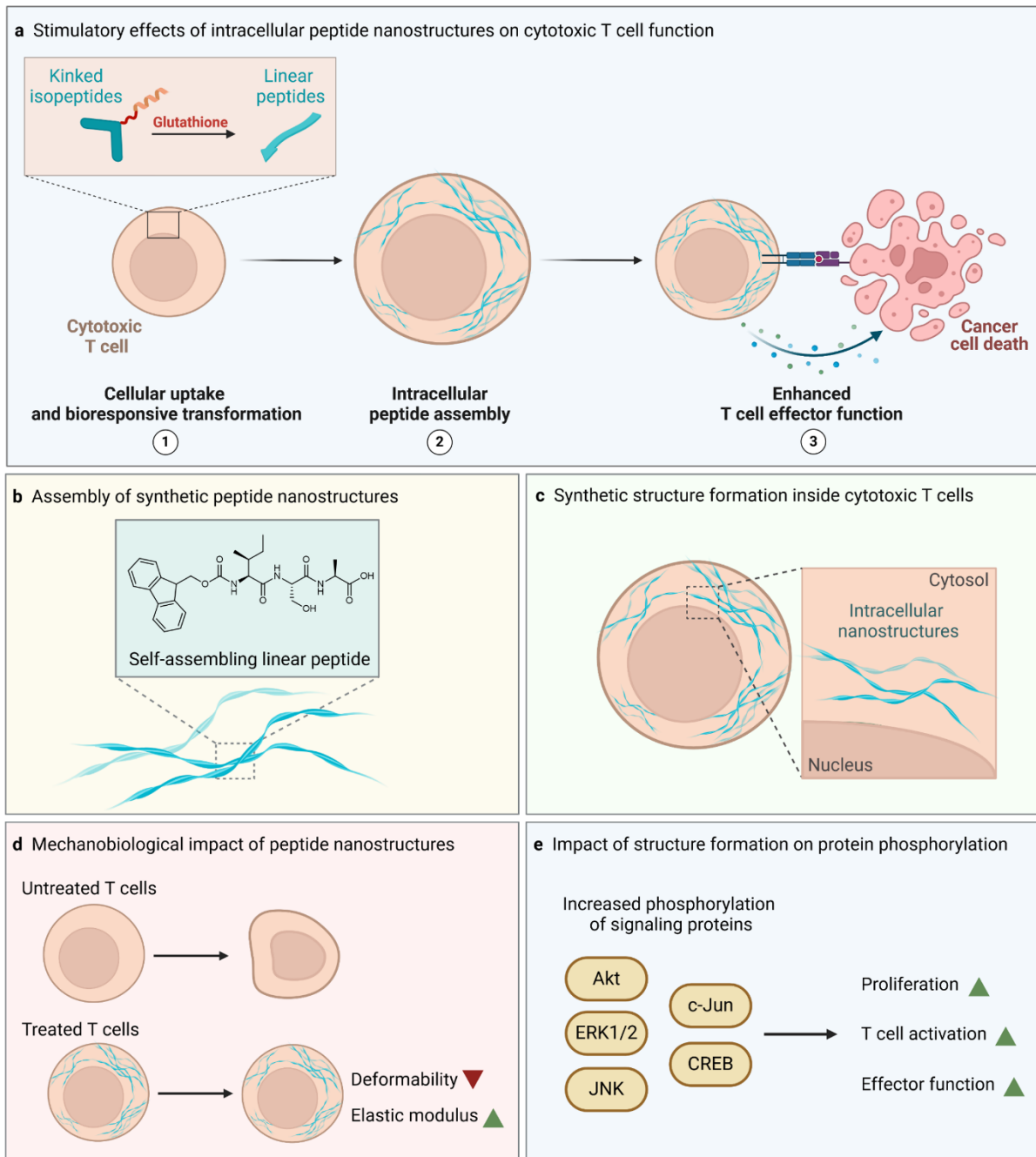
46 Our work explores a new direction in this field by harnessing synthetic intracellular nanostructures for
47 the immunomodulation of cytotoxic T cells. Cytotoxic CD8⁺ T cells play a crucial role in the immune
48 response by directly targeting and eliminating cancerous or virus-infected cells.¹¹ The unmatched
49 specificity of T cells in recognizing target cells is a key advantage in T cell-based therapies and their
50 efficacy in inducing apoptosis is tightly linked to their activation status, which involves complex
51 intracellular signaling pathways.¹² High cytotoxic effector function in T cells is desirable, as it enables a
52 more robust and effective response against tumors, contributing to better therapeutic outcomes in
53 adoptive cell therapy. The mechanical properties of T cells, such as stiffness and deformability,
54 correlate with their activation and migration capabilities, as well as their ability to interact with target
55 cells.¹³ Enhancing the functional capacity of cytotoxic T cells by biochemical and biophysical means is
56 therefore a central goal in immunotherapy.

57 In current clinical approaches, T cells are often modified outside the body through genetic engineering
58 before being reinfused into the patient to combat cancer.^{14,15} While ongoing efforts aim to enhance T
59 cell efficacy by refining genetic engineering techniques, fewer strategies explore modulation of T cells
60 through chemical engineering, for instance, via extracellular interactions with nanomaterials.¹⁶⁻¹⁸ In our
61 work, we propose a complementary strategy by intracellular chemical engineering: the *in situ* self-
62 assembly of synthetic nanostructures within cytotoxic T cells to enhance T cell cytotoxicity. This
63 approach holds the potential to further enhance T cell functionality beyond the limits of genetic
64 modifications.

65 In T cells, glutathione, a reducing agent abundant in the cytosol¹⁹, plays a critical role in maintaining
66 redox homeostasis and facilitating metabolic reprogramming during T cell activation. It acts as an
67 antioxidant to counterbalance the increased mitochondrial production of reactive oxygen species
68 (ROS).²⁰⁻²² As ROS scavenging is essential for T cell activation, proliferation and effector function,
69 activated T cells have been shown to contain significantly higher levels of intracellular glutathione
70 compared to resting T cells.^{21,23} Therefore, the glutathione-induced transformation of a bioresponsive
71 assembly precursor within T cells is a promising strategy for the *in situ* generation of intracellular
72 nanostructures that boost T cell activation dynamics and cytotoxic effector function against cancer
73 cells. Shifting the focus from disrupting malignant cells to enhancing the beneficial functions of healthy
74 cells, such as cytotoxic T cells, will be a next-generation technology for more sophisticated cell-material
75 interactions. Modulating the behavior of these immune cells through *in situ*-formed artificial
76 nanostructures would also have significant implications for immunotherapy.

77 Herein, we introduce glutathione-responsive *isopeptides* capable of undergoing a multistep reaction
78 cascade upon cellular entry, resulting in the *in situ* formation of peptide nanostructures inside human
79 cytotoxic T cells (Fig. 1). We report a significant stimulatory effect of these peptide nanostructures on
80 cytotoxic T cell function, leading to enhanced cytotoxicity against breast cancer cells. Using confocal
81 laser scanning microscopy (CLSM) and correlative light and electron microscopy (CLEM), we visualize
82 the formation and localization of these nanostructures. Importantly, the enhancement of T cell effector
83 function is directly correlated with intracellular nanostructure formation. Additionally, we examine
84 activation of stimulatory T cell signaling of peptide-treated versus untreated T cells and evaluate the
85 impact of synthetic intracellular nanostructures on T cell mechanical properties. This analysis aims to
86 elucidate the biophysical and molecular mechanisms driving the observed functional enhancements.
87 To our knowledge, this is the first study to demonstrate that synthetic intracellular nanostructures can

88 support and enhance beneficial cellular functions, offering a novel strategy to modulate immune cell
 89 responses.



90
 91 **Figure 1 Schematic overview of T cell engineering through intracellular synthetic nanostructures. a |** Glutathione-responsive
 92 kinked *isopeptides* undergo a bioresponsive transformation inside cytotoxic T cells, leading to the formation of linear, self-
 93 assembling peptides. This intracellular peptide assembly within human cytotoxic T cells enhances T cell-mediated cytotoxicity
 94 against cancer cells. **b |** The supramolecular properties and structural characteristics of the nanofiber-forming peptides were
 95 investigated. **c |** The *in situ* structure formation inside cytotoxic T cells was visualized using confocal laser scanning microscopy
 96 and correlative light and electron microscopy. **d |** Intracellular structure formation influences the mechanical properties of
 97 cytotoxic T cells, reducing their deformability and increasing the elastic modulus. **e |** Increased phosphorylation of key
 98 signaling proteins associated with T cell proliferation, activation, and effector function was observed following *in situ*
 99 nanostructure formation.

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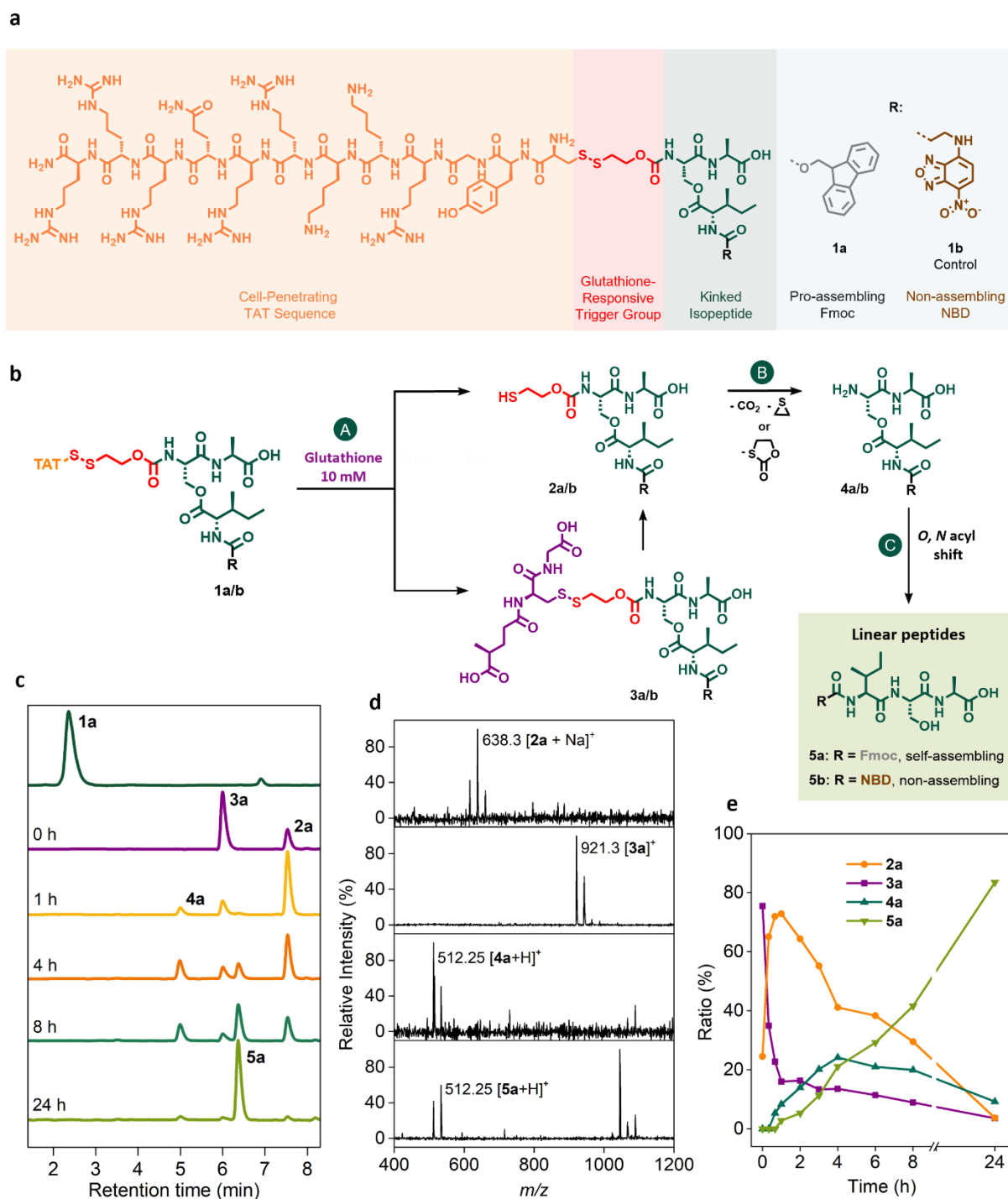
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102 Results

103 Design, synthesis and transformation of glutathione-responsive *isopeptides*

104 The glutathione-responsive *isopeptide* **1a**, along with the control *isopeptide* **1b**, consists of three key
105 structural components: (1) the cell-penetrating peptide sequence TAT (transactivator of transcription)
106 derived from human immunodeficiency virus (HIV), (2) a glutathione-responsive trigger group that can
107 undergo reductive degradation and (3) the kinked *isopeptide* with an aromatic *N*-terminal group
108 (Fig. 2a). This *N*-terminal group either promotes supramolecular assembly (Fmoc in **1a**) or prevents
109 assembly of the linear product (NBD in **1b**) resulting from the glutathione-triggered transformation
110 (Fig. 2a).

111 The synthesis of the kinked *isopeptides* **1a** and **1b** was achieved through a combination of solid-phase
112 peptide synthesis and solution-phase synthesis (Scheme S1). To analyze the glutathione-induced
113 transformation of the *isopeptides* (Fig. 2b), we investigated the kinetics of this multistep reaction
114 cascade (Fig. 2b) using liquid chromatography-mass spectrometry (LC-MS) (Fig. 2c). By analyzing the
115 *m/z* values of the emerging peaks in the LC traces, we identified and assigned the reactive
116 intermediates and final products of the glutathione-induced conversion (Fig. 2c,d).

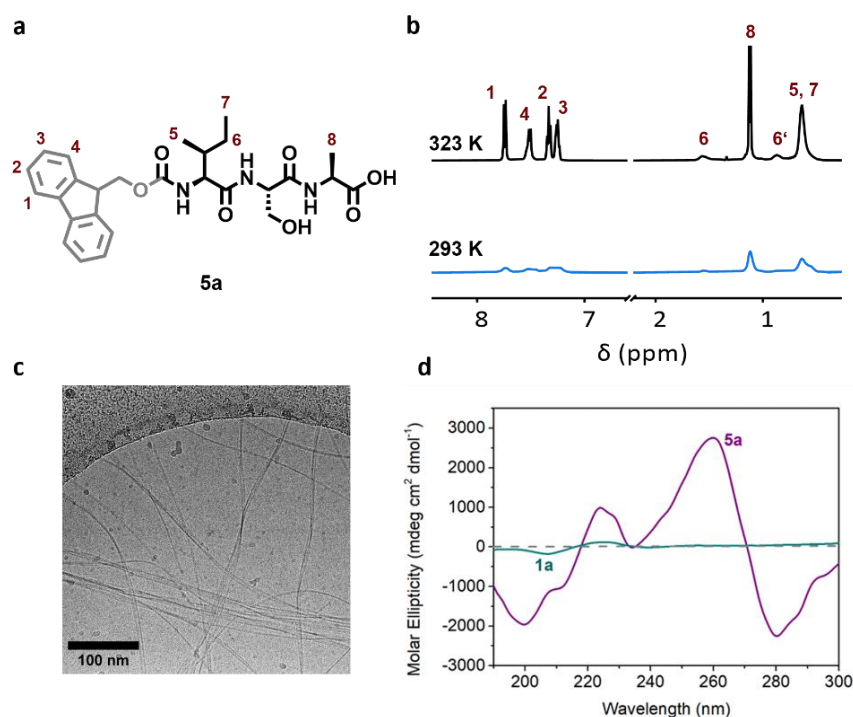


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118 **Figure 2 Chemical structure and multistep conversion of glutathione-responsive iso-peptides.** a | Chemical structures of
 119 glutathione-responsive iso-peptides **1a** (with a Fmoc (9-fluorenylmethoxycarbonyl) group) and **1b** (with an NBD
 120 (nitrobenzodiazole) unit). b | Reaction scheme illustrating the multistep conversion of pro-assembling iso-peptides **1a** or the
 121 control iso-peptide **1b** into the self-assembling linear peptide **5a** or the non-assembling linear peptide **5b**. c | LC-MS kinetic
 122 analysis of the glutathione-induced linearization of **1a** in NH_4HCO_3 buffer (50 mM, pH 7.4) and methanol (v/v 1:1) in the
 123 presence of intracellular concentrations of glutathione (reduced glutathione: 10 mM; oxidized glutathione: 1 mM) at room
 124 temperature. d | Convolutal MS spectra identifying the intermediates **2a** ($t_R = 7.53$ min), **3a** ($t_R = 6.00$ min) and **4a** ($t_R = 4.98$
 125 min) as well as the final linear peptide **5a** ($t_R = 6.37$ min) during the LC-MS analysis. e | Molar ratio of intermediates **2a**, **3a**, **4a**
 126 and final product **5a** after the addition of glutathione-containing buffer, based on the peak integration at 254 nm.

127 In the presence of intracellular levels of glutathione (reduced glutathione: 10 mM; oxidized
 128 glutathione: 1 mM)²⁴ in NH_4HCO_3 buffer (50 mM, pH 7.4), iso-peptide **1a** underwent instant
 129 degradation, so that upon the first LC-MS injection, its signal ($t_R = 2.36$ min) was no longer detectable

130 (Fig. 2c). Instead, two cleavage products, **2a** ($t_R = 7.53$ min) and **3a** ($t_R = 6.00$ min), were identified.
 131 These two intermediate products result from the nucleophilic attack of glutathione on the disulfide
 132 bond of **1a**, occurring at either of the two sulfur atoms (Fig. 2b). As the disulfide bond of the glutathione
 133 adduct **3a** is similarly susceptible to reductive cleavage, the transformation of **3a** also gave rise to the
 134 isopeptide with a free thiol group **2a** over time. After one hour, the unprotected isopeptide **4a**
 135 ($t_R = 4.98$ min) was detected as the product of the self-immolation of the trigger group (Fig. 2c). The
 136 subsequent *O,N* acyl shift caused the linearization of **4a**, indicated by the increasing peak
 137 corresponding to the linear peptide **5a** ($t_R = 6.37$ min). After 24 h, the linear self-assembling
 138 Fmoc-ISA **5a** became the most prominent peak in the LC trace (Fig. 2c), reflecting a conversion of 84%
 139 of the initial isopeptide **1a** into the self-assembling linear monomer **5a** (Fig. 2e).



140
 141 **Figure 3 Supramolecular assembly of linear peptide.** **a** | Chemical structure of **5a** with labeled protons. **b** | ¹H NMR analysis
 142 of self-assembly behavior of **5a** (1 mg/ml) in deuterated phosphate buffer (50 mM) and DMSO-*d*₆ (9:1) at 293 K and 323 K.
 143 **c** | Cryo-TEM image of peptide nanofibers formed by linear peptide **5a** (1 mg/ml) in Dulbecco's phosphate buffered saline
 144 (DPBS) (pH 7.4) and DMSO (99:1). Scale bar 100 nm. **d** | Circular dichroism spectra of linear peptide **5a** and isopeptide **1a**
 145 (500 μM each) in phosphate buffer (10 mM, pH 7.4). The spectrum of **5a** shows characteristic signals of attractive peptide
 146 backbone interactions and aromatic interactions between Fmoc groups, while the spectrum of **1a** shows no signals indicating
 147 chirality.

148 The supramolecular assembly behavior of the linear peptide **5a** was analyzed using nuclear magnetic
 149 resonance (NMR) spectroscopy, circular dichroism (CD) spectroscopy, transmission electron
 150 microscopy (TEM) and cryogenic transmission electron microscopy (cryo-TEM) (Fig. 3).

151 Temperature-dependent ¹H NMR spectroscopy of the linear peptide **5a** revealed significant peak
 152 broadening at room temperature (293 K), which is characteristic of supramolecular interactions
 153 between peptide monomers in aqueous solution (deuterated phosphate buffer (50 mM) and DMSO-*d*₆
 154 (9:1)) (Fig. 3b and Fig. S21). Upon heating the solution to 323 K, sharp signals corresponding to the
 155 aromatic Fmoc head group and side chain groups of peptide **5a** emerged (Fig. 3a,b), indicating a higher
 156 amount of detectable monomeric peptide **5a** in solution at elevated temperatures.

157 CD spectroscopy was used to further characterize the secondary structure of linear Fmoc-ISA **5a** and
 158 kinked isopeptide **1a** (Fig. 3d). The CD spectrum revealed a nanoscale chirality of the self-assembling
 159 peptide **5a**, which arises from the chiral arrangement of the peptide monomers within the assembled

160 nanostructure.²⁵ The spectrum of **5a** displays a maximum at 260 nm that is characteristic for the $\pi \rightarrow \pi^*$
161 transitions of the aromatic Fmoc groups²⁶. Additionally, another maximum was observed at 224 nm
162 indicating a $n \rightarrow \pi^*$ transition of the carbonyl groups in the peptide backbone due to hydrogen
163 bonding.^{27,28} In contrast, the non-assembling kinked *isopeptide* **1a** showed no discernable chirality of
164 the secondary structure, underlining the necessity of the transformation from kinked **1a** to linear **5a** to
165 achieve the desired supramolecular interaction required for structure formation (Fig. 3d).

166 Dry-state TEM images of the linear peptide **5a** revealed its ability to self-assemble into long nanofibers
167 in Dulbecco's phosphate buffered saline (DPBS) with 1% DMSO (Fig. S23). To investigate the impact of
168 incorporating another linear peptide modified with a fluorophore, which is crucial for detecting
169 nanostructures inside living cells, we studied the co-assembly of fluorescent Coumarin343-
170 functionalized peptide **5c** with **5a** in a 5:1 ratio. TEM images confirmed that the presence of peptide **5c**
171 did not disrupt nanofiber formation (Fig. S24). Similarly, when Cyanine5 (Cy5)-functionalized
172 peptide **5d** was co-assembled with peptide **5a** at a 99:1 ratio, the nanofiber integrity was preserved. In
173 contrast, co-assembly of the kinked assembly precursors **1a** and **1c** (Coumarin343-modified) (5:1 ratio)
174 or **1a** and **1d** (Cy5-modified) (99:1 ratio) did not produce any observable superstructures (Fig. S24),
175 emphasizing again the importance of the glutathione-induced linearization to induce self-assembly.
176 Additionally, the more hydrophilic nitrobenzodiazole (NBD)-modified control *isopeptide* **1b** and its
177 corresponding linear peptide **5b** also did not form any nanostructures, which allows evaluating cellular
178 uptake and glutathione-induced rearrangement without subsequent peptide assembly (Fig. S24).

179 Cryo-TEM provided further insights into the peptide nanostructures of the Fmoc-functionalized
180 peptide **5a** in an aqueous environment (DPBS with 1% DMSO). Consistent with dry-state TEM, cryo-
181 TEM images revealed long, thin nanofibers of linear peptide **5a** with a slightly twisted morphology
182 (Fig. 3c and Fig. S25 and S26). The twisted fibers exhibited an average thickness of 6.8 ± 0.3 nm at the
183 twists and 11.0 ± 0.2 nm at the non-twisted regions (Fig. S26). The critical aggregation concentration
184 (CAC) of the linear peptides was determined via a Proteostat aggregation assay, which is a
185 fluorescence-based technique used to detect β -sheet driven assembly formation. The CAC for linear
186 peptide **5a** in DPBS with 1% DMSO was found to be 10 μ M (Fig. S27). For the co-assemblies with either
187 the Coumarin343-containing linear peptide **5c** (5:1 ratio) or the Cy5-modified linear peptide **5d** (99:1
188 ratio), the CAC was 9.2 μ M and 4.6 μ M, respectively (Fig. S27). These results further confirm that the
189 incorporation of fluorescent monomers **5c** or **5d** does not hinder nanostructure formation.

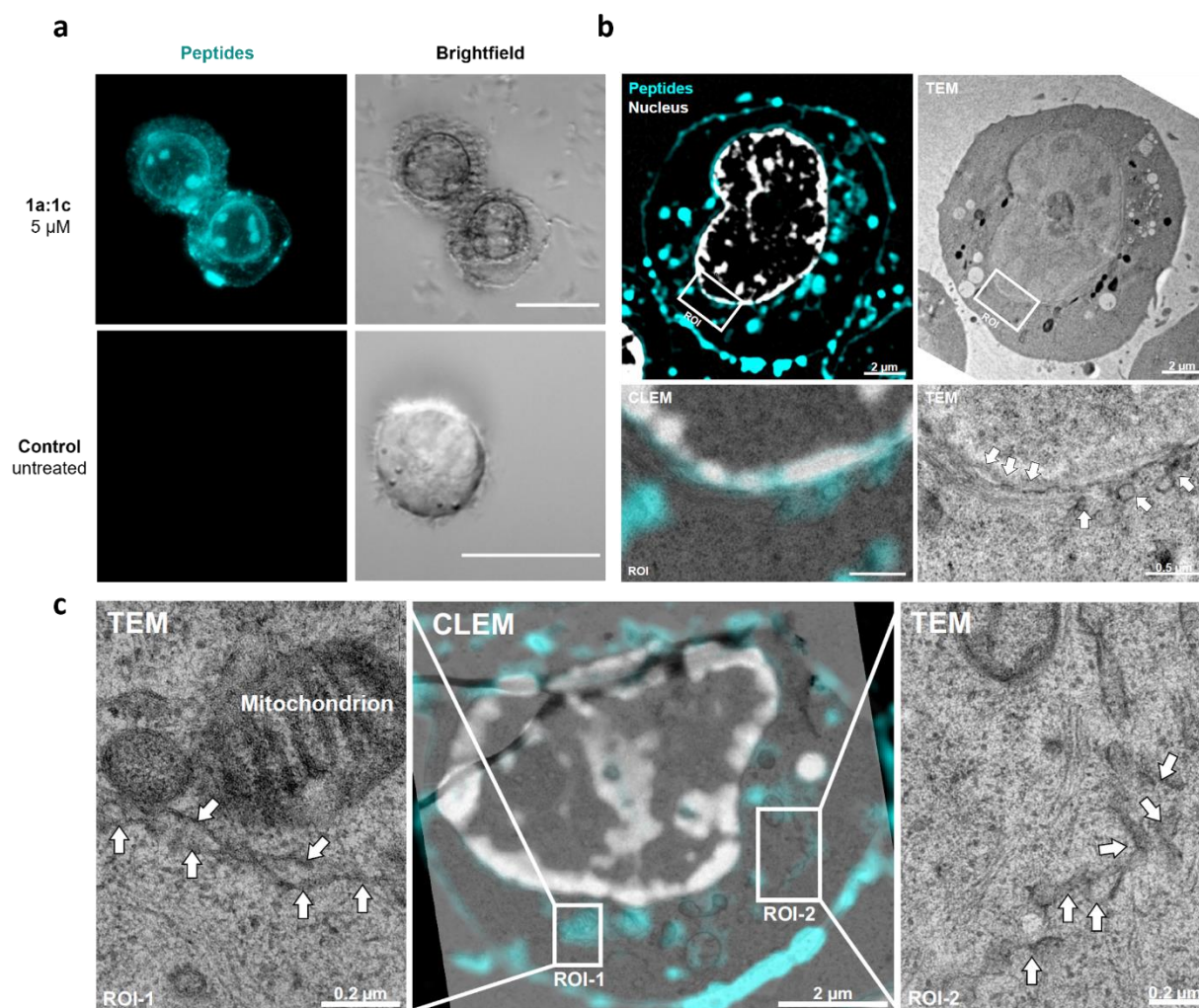
190 In summary, our analysis demonstrates that the multistep conversion of kinked *isopeptide* **1a** into the
191 linear self-assembling peptide **5a** can be effectively triggered by physiological levels of glutathione.
192 Physicochemical characterization of linear peptide **5a** further reveals its ability to form peptide
193 nanofibers at low micromolar concentrations, highlighting its potential for the *in situ* formation of
194 synthetic nanostructures in the intracellular environment.

195 Cellular uptake and *in situ* formation of peptide nanostructures in T cells

196 Next, we explored the glutathione-induced conversion of the *isopeptides* into the corresponding linear
197 peptides and subsequent nanostructure formation within cytotoxic T cells. First, primary human CD8⁺
198 T cells were activated *ex vivo* by isolating them from healthy donors and co-incubating with anti-
199 CD3/CD28 activation beads. This cross-linking of CD3 and CD28 receptors, combined with interleukin 2
200 (IL-2), induces T cell activation into an effector state and promotes polyclonal expansion.

201 We then investigated the uptake and co-assembly of the pro-assembling *isopeptide* **1a** together with
202 a fluorescently labeled *isopeptide* (either **1c** with Coumarin343 or **1d** with Cy5) in these *ex vivo*
203 expanded cytotoxic T cells (Fig. 4). CLSM of activated T cells treated with the *isopeptides* **1a:1c** (5:1) at
204 5 μ M for 1 hour revealed the formation of fluorescent peptide nanostructures in the cytosol, the

205 nucleus and in the perinuclear region, also visible as high-contrast regions in the brightfield images
206 (Fig. 4a).



207
208 **Figure 4 Cellular uptake and intracellular peptide nanostructure formation in cytotoxic T cells.** **a** | Confocal laser scanning
209 microscopy (CLSM) images of activated T cells incubated with 5 μM of glutathione-responsive isopeptides **1a** and **1c** (5:1)
210 (cyan) for 1 hour, demonstrating the formation of intracellular peptide nanostructures in the cytosol and perinuclear region.
211 Untreated T cells served as controls. Scale bar: 15 μm. **b** | Correlative light and electron microscopy (CLEM) images of activated
212 human CD8⁺ T cells treated with 5 μM of glutathione-responsive isopeptides **1a** and **1d** (99:1) (cyan) for 1 hour before freezing,
213 highlighting the formation of fluorescent peptide nanostructures at the nuclear membrane and perinuclear region. **c** | CLEM
214 images focusing on the localization of peptide nanostructures within the cytosol. The integrity of subcellular compartments
215 of T cells appear unaffected by intracellular structure formation.

216 Further validation of in situ peptide assembly was conducted using CLEM (Fig. 4b,c). Pre-activated and
217 *ex vivo* expanded cytotoxic T cells treated with isopeptides **1a:1d** (99:1) were analyzed, with Cy5-
218 labeled isopeptide **1d** selected for co-assembly due to its superior fluorescence properties. CLEM
219 images revealed fluorescent nanostructures distributed throughout the cytosol, perinuclear region,
220 and at the cell membrane (Fig. 4b,c). The observed fiber thickness ranged from approximately 3.5 to
221 7.5 nm, consistent with the cryo-EM findings for peptide nanofibers in buffered solution (see Fig. 3c).
222 Importantly, despite the widespread presence of peptide nanostructures within the cytosol and near
223 the nucleus, the overall integrity of the T cells, including organelles such as mitochondria, remained
224 intact (Fig. 4b,c). This indicates that incubation with isopeptides **1a:1d** at 5 μM for 1 hour did not
225 significantly disrupt cellular or subcellular structures. These results underscore that the self-assembly
226 of peptides at low concentrations does not compromise the cellular integrity of activated T cells.

227 In contrast, activated T cells treated with the NBD-functionalized control *isopeptide 1b* at 5 μ M for
228 1 hour exhibited no nanostructure formation and lower intracellular fluorescence (Fig. S34), reflecting
229 the lack of self-assembling capability of the linear NBD-modified peptide **5b** (Fig. S24). Cellular uptake
230 analysis of resting, i.e. non-activated, T cells treated with the pro-assembling *isopeptides 1a:1d* (99:1)
231 at 5 μ M for 1 hour showed markedly lower intracellular fluorescence compared to activated T cells
232 treated with the same peptides (Fig. S35). This aligns with the observation that fiber assembly is
233 glutathione-dependent and activated T cells have reportedly higher cytosolic glutathione levels.^{21,23}

234 **Functional impact of intracellular peptide nanostructures on cytotoxic T cells**

235 Next, we examined how the synthetic intracellular peptide nanostructures impact the morphology and
236 immunological function of cytotoxic T cells, specifically their ability to eliminate cancer cells. To
237 evaluate the cytotoxicity of *ex vivo* pre-activated CD8⁺ T cells against MCF-7 breast cancer cells, we
238 combined the cytotoxic T cells with a bispecific T cell engager (BiTE) – a dual-targeting antibody that
239 binds both the CD3 complex on T cells and the Human Epidermal Growth Factor Receptor 2 (HER2) on
240 MCF-7 cells – followed by a 24-hour co-culture incubation with the cancer cells.

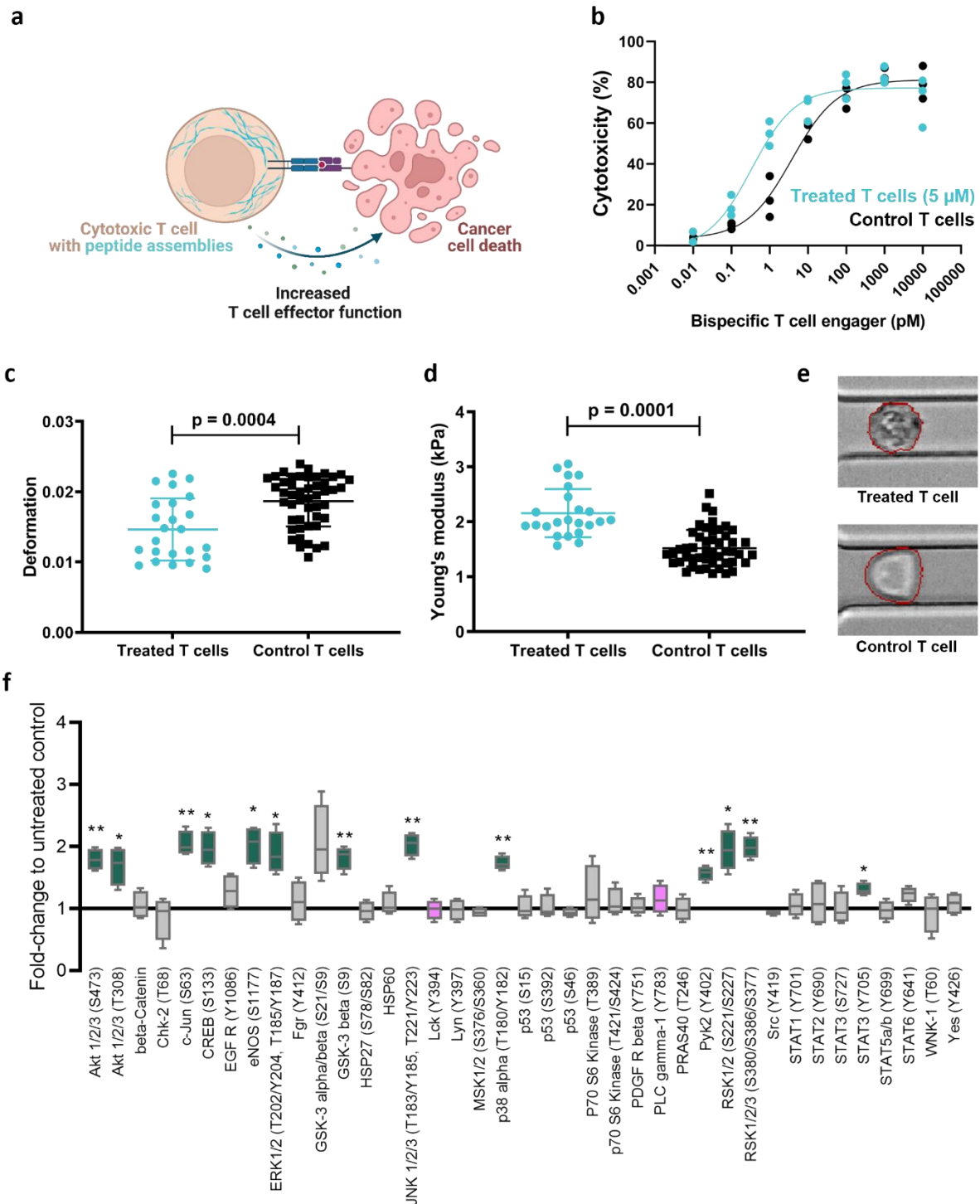
241 Treatment of cytotoxic T cells with glutathione-responsive *isopeptides 1a:1c* (5:1, 5 μ M) for 1 hour prior
242 to the addition of BiTE and co-culturing significantly enhanced their cytotoxicity against the cancer
243 cells. T cells pre-treated with these *isopeptides* exhibited a markedly lower IC₅₀ value for the bispecific
244 T cell engager of 0.34 pM compared to 3.81 pM in untreated control T cells (Fig. 5a,b). Similarly, the
245 use of *isopeptides 1a:1d* (99:1, 5 μ M), which includes the Cy5-labeled peptide used also for CLEM
246 analysis, yielded comparable enhancements in cytotoxicity, indicating that the choice of fluorescent
247 label does not impact the functional efficacy of the synthetic peptide nanostructures (Fig. S31). In
248 contrast, T cells pre-treated with control *isopeptide 1b*, which is internalized but only releases a linear
249 NBD-modified peptide incapable of forming intracellular nanostructures, did not exhibit increased
250 cytotoxicity (Fig. S30). These findings suggest that the observed enhancement in cytotoxicity is due to
251 the formation of synthetic intracellular peptide nanostructures.

252 Towards revealing the functional mechanism behind the increased cytotoxic effect, we analyzed the
253 rheological changes in T cells treated with pro-assembling *isopeptides via* single cell real-time
254 deformation cytometry (RT-DC). T cell activation and adhesion to the antigen presenting cells (in this
255 case the HER2-presenting MCF7 breast cancer cells) is greatly influenced by the mechanical properties
256 of the T cells, which in turn are governed by cytoskeletal tensions and acto-myosin contractions.²⁹ Both
257 the actin and microtubule cytoskeleton play crucial roles in establishing T cell polarity, migration,
258 formation of the immunological synapse and the directed secretion of cytokines and cytolytic
259 granules.³⁰ RT-DC measurements revealed that T cells treated with *isopeptides 1a:1c* for 1 h at 5 μ M
260 exhibited notable changes in morphology and stiffness (Fig. 5c,d,e). Specifically, these T cells
261 demonstrated significantly reduced deformability (Fig. 5c) and an increased elastic modulus (Fig. 5d)
262 compared to the untreated controls. This indicates a general stiffening of the activated T cells that
263 results from the presence of synthetic intracellular nanostructures.

264 To elucidate the downstream signaling effects of peptide nanostructures within T cells, we correlated
265 enhanced T cell effector functions and mechanobiological changes with alterations in signaling protein
266 phosphorylation by a Phospho-Kinase Antibody Arrays (Fig. 5f and Fig. S32). We observed significant
267 changes in the phosphorylation of key signaling proteins, including Akt, c-Jun, CREB, ERK1/2 and JNK,
268 in cytotoxic T cells treated with pro-assembling *isopeptides 1a:1c* (Fig. 5f). These proteins are integral
269 components of pathways that drive T cell activation, proliferation and effector function. Elevated
270 phosphorylation of Akt, a central kinase in the PI3K/Akt pathway,³¹ suggests enhanced survival, along
271 with elevated expression of key adhesion and cytolytic molecules in T cells.³²⁻³⁴ The increased
272 phosphorylation of c-Jun, a member of the activator protein-1 (AP-1) family, further promotes the

273 expression of genes required for T cell activation and proliferation.^{35,36} Similarly, the higher levels of
274 phosphorylated transcription factor CREB were found in peptide-treated T cells, indicating activation
275 of gene expression essential for T cell effector function and cytokine production.³⁷ The elevated
276 phosphorylation levels of ERK1/2 and JNK, which are key mitogen-activated protein (MAP) kinases,
277 further support the notion of heightened T cell proliferation and effector function.³⁸⁻⁴⁰ In contrast, T
278 cells treated with the non-assembling control *isopeptide 1c*, which can enter cells and undergo
279 glutathione-induced transformation but lacks the ability to form assemblies, did not exhibit increased
280 phosphorylation of these proteins (Fig. S32). This finding highlights that the observed effects on
281 signaling proteins are specifically associated with the formation of synthetic peptide nanostructures
282 within T cells.

283 Collectively, these findings demonstrate that the glutathione-triggered formation of peptide
284 nanostructures not only alters the mechanobiological properties of T cells but also potentiates
285 intracellular signaling pathways linked to an enhanced T cell immune response.



286

287 **Figure 5 Enhancement of T cell cytotoxicity against MCF-7 cancer cells and alterations in mechanobiology and protein**
 288 **phosphorylation by intracellular peptide nanostructures. a** | Schematic illustration of the co-stimulation of T cell cytotoxicity
 289 via intracellular peptide assembly. **b** | Dose-response curve showing the cytotoxic effect of activated T cells against HER2-
 290 expressing MCF7 cancer cells in relation to the concentration of a bispecific T cell engager targeting HER2 and CD3. The black
 291 curve represents data for untreated T cells, while the blue curve shows data for T cells pre-treated with the *isopeptides* **1a:1c**
 292 (5:1) at 5 μ M for 1 hour, followed by washing and addition of the bispecific engager ($n = 3$ donors, mean of 2 technical
 293 replicates each). The IC_{50} of the bispecific engager for untreated T cells is 3.81 pM, compared to 0.34 pM for *isopeptide*-
 294 treated cells. **c** | Real-time deformability cytometry (RT-DC) analysis showing reduced deformation in T cells pre-treated with
 295 the *isopeptide* mixture **1a:1b** (5:1) at 5 μ M for 1 hour, relative to untreated controls. **d** | RT-DC measurements indicating an
 296 increased Young's modulus in T cells treated with the *isopeptide* mixture, reflecting enhanced cellular stiffness. **e** | Brightfield
 297 images of treated (**1a:1b** (5:1) at 5 μ M for 1 hour) and untreated control T cells during RT-DC measurements within a
 298 microfluidic channel. **f** | Proteome Profiler Human Phospho-Kinase Antibody Array analysis of T cells treated with the

299 isopeptides **1a:1c** (5:1) at 5 μ M for 1 hour (n = 2 donors, 2 on-membrane replicates), highlighting differential phosphorylation
300 in a panel of key signaling proteins essential for T cell activation.

301 **Conclusion**

302 In this study, we have demonstrated the chemical engineering of activated human cytotoxic T cells
303 through the *in situ* formation of intracellular synthetic peptide nanofibers that alter critical T cell
304 functions, ultimately improving the immune response against cancer cells. By using redox-sensitive
305 isopeptides, we successfully induced the assembly of synthetic nanostructures within the intracellular
306 environment of cytotoxic T cells, resulting in a significant boost to their cytotoxic effector function. The
307 formation of these peptide nanostructures not only altered the mechanical properties of the T cells,
308 leading to increased stiffness and decreased deformability, but also promoted central signaling
309 pathways involved in the activation and regulation of T cells. This dual impact on both the physical and
310 biochemical attributes of T cells underscores the potential of intracellular nanostructures as a tool for
311 modulating immune cell behavior beyond genetic engineering. By focusing on augmenting the intrinsic
312 functions of healthy immune cells, this work could pave the way for innovations in the field of
313 immunotherapy. The ability to fine-tune immune cell properties through controlled intracellular
314 assembly could potentially open up new possibilities for the design of next-generation therapies
315 targeting complex intracellular environments.

316

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339 **Contributions**

340 S.C., D.Y.W.N., O.S. and T.W. conceived the project. S.C. performed the synthesis and characterization
341 of peptides and related compounds. S.C. and Z.Z. conducted the LC-MS kinetics analysis. J.L. and P.R.
342 performed dry-state TEM measurements. S.C. and R.M. performed the CD spectroscopy analysis. S.C.
343 conducted the Proteostat aggregation assay. J.L., J.F. and Y.R. aided in the synthesis of control
344 compounds. S.S., F.M., I.L. and K.L. contributed cryo-EM measurements and analysis. S.C. and M.W.
345 performed NMR analysis. A.B. performed RT-DC measurements. O.S. performed cell uptake
346 experiments, imaging via CLSM, cytotoxicity assays and proteome profiler analysis. C.S. performed the
347 CLEM experiments and analysis. D.Y.W.N., O.S. and T.W. supervised the project. All authors have read
348 and approved the final manuscript.

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