Click Chemistry-Driven Dual Nanosystem for miR-122 Detection with Single-Base Specificity from Tumour Cells

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Abstract

MicroRNAs (miRNAs) are considered potential biomarkers due to their specific expression patterns in tissues and their changes in expression under pathological conditions. MicroRNA-122 (miR-122) is a vertebrate-specific miRNA known for its high expression in the liver, where it plays a role in hepatic metabolism, liver development and cellular differentiation. Dysregulation of miR-122 has been found in pathological conditions such as hepatocellular carcinoma or drug-induced liver injury (DILI). Currently, miRNA detection faces challenges such as improving point-of-care efficiency, obtaining direct results and accurately identifying miRNA isoforms. Overcoming these challenges is essential to improve the clinical efficacy of miR-122 detection as a diagnostic and prognostic biomarker in liver-related diseases. In this study, we present a click chemistry driven dual nanosystem designed for single-base specific miR-122 detection using a flow cytometer as the reading platform. Using the dual nanosystem, we analysed miR-122 expression in various tumour cell lines with specificity and robustness, showing a high correlation with results obtained from a TaqMan assay. We also detected miR-122 using a serum matrix and identified four single nucleotide variations at a specific position within the miR-122 sequence. Our approach involves a fully bioorthogonal strategy and includes signal amplification using two types of different nanoparticles together with the high affinity of peptide nucleic acid probes. The chemistry used in this dual nanosystem offers remarkable versatility and provides a promising opportunity to pioneer enzyme-free nanoparticle-based strategies based on click chemistry and bioorthogonality miRNA detection and isomiR studies, thus advancing the field of molecular diagnostics.

<u>Keywords</u>

Dual Nanosystem; Nanobiotechnology; Click Chemistry; Bioorthogonal Chemistry; microRNAs; miR-122; Molecular Diagnostics

Graphical Abstract



1. Introduction

MicroRNAs (miRNAs) are short non-coding RNAs, typically 18-24 nucleotides in length, that regulate biological processes by modulating gene expression through the RNA interference pathway¹. MiRNA profiles show tissue specificity and their expression is altered under pathological conditions, highlighting their potential as diagnostic biomarkers^{2,3}. MicroRNA-122 (miR-122) constitutes one of these examples serving as a liver-specific miRNA biomarker for the diagnosis of liver-related diseases^{4,5}. MiR-122 is exclusively found in vertebrates and represents approximately 70% of the total miRNAs present in hepatocytes, implying a fundamental role in cellular differentiation, liver development and lipid metabolism⁶. Dysregulation of miR-122 expression has been found in pathological conditions such as hepatocellular carcinoma, drug-induced liver injury (DILI), and hepatitis C virus infection^{7,8}. Despite progress, current miRNA-based diagnostic methods still face challenges. Continued efforts are needed to improve technologies that enable the direct detection of miRNAs at the patient's point-of-care, ensuring cost-effectiveness and efficiency in healthcare outcomes^{9,10}. In particular, one of the challenges in miRNA detection is the existence of multiple isoforms characterised by sequence variations within miRNAs, known as isomiRNAs or isomiRs^{11,12}. Although further studies are needed to fully understand the function of these isomiRs, they have been recognised as useful for classifying disease¹³. For instance, categorising the presence of isomiRs as a binary system of present or absent has enabled the classification of datasets across different types of cancer¹⁴. This suggests that the identification of isomiRs could have clinical significance. For miR-122, several isoforms have been described¹⁵, and high levels of isomiRs have been found in the blood and liver tissue in patients with acute liver injury¹⁶, and may be a better indicator for early diagnosis of acute liver injury than the standard proteins, which are only found in patients with DILI. Due to the small size of miRNA sequences and their limited sequence variation, often involving just a single nucleotide variation (SNV), current methods can struggle to distinguish SNVs in miRNA sequences⁷. Small RNA sequencing is currently the only technique capable of accurately detecting and quantifying isomiRs, but its complexity makes direct implementation for point-of-care and diagnostic settings difficult⁷. For these reasons, it is essential to further improve technologies that allow the direct detection of miRNAs and the detection of isomiRs.

In response to these challenges, in recent years, we have focused our efforts on developing Dynamic Chemistry Labelling (DCL) as a methodology for miRNA detection with single-base resolution. DCL serves as an enzyme-free and versatile isomiR detection method that can be applied to several biological samples, including serum, plasma, cell lysates and fixed cells^{17–20}. DCL is based on the use of abasic peptide nucleic acid (PNA) probes. These PNA probes are known mimics of nucleic acids, but instead of a sugarphosphate backbone, they have a peptide backbone composed of N-(2-aminoethyl)glycine units²¹. This modification results in a peptide backbone that lack charges, allowing them to exhibit a strong affinity for their DNA or RNA targets without experiencing electrostatic repulsion from the negatively charged sugar-phosphate backbone. As a result, they form more stable PNA-DNA or PNA-RNA duplexes than

natural DNA or RNA duplexes²². The PNA probes used in the DCL methodology have a modification in their peptide backbone, where they have an abasic site, a position within the sequence that lacks a nucleobase but contains a secondary amine. This abasic position can be strategically designed to selectively target a particular nucleotide of interest within the complementary miRNA sequence²³. Then, four chemically modified nucleobases featuring an aldehyde group, called SMART-Nucleobases, are used as highly specific labelling reagents. Among these SMART-Nucleobases, only the one that is complementary to the nucleobase of interest according to the Watson-Crick base-pairing rules can react in a dynamic chemical reaction with the secondary amine at the abasic position and then covalently bond to the abasic PNA probes to form an irreversible tertiary amine²³. The SMART-Nucleobases can be tagged with fluorescent markers or biomolecules to allow the detection of the integrated SMART-Nucleobase, and thus reading the specific nucleobase. To sum up, DCL transform the amount of target miRNAs into amounts of labelled PNA probes that can then be measured and quantified.

In this study, we present a click chemistry driven dual nanosystem that integrates DCL in solution with standard bead-based detection methods to provide a robust platform for the detection of miR-122 with single base specificity from tumour cell lines. The dual nanosystem presented employs two different types of nanoparticles: (i) fluorescentlylabelled polystyrene nanoparticles (PS-NPs) modified with cyclooctyne to capture the PNA:miR-122 complex via click chemistry, and (ii) fluorescently-labelled silica nanoparticles conjugated to streptavidin to detect biotinylated-labelled complexes through the use of biotinylated SMART-Nucleobases via biotin-streptavidin binding. The click chemistry reaction takes place between the azide-modified abasic PNA probe and the cyclooctyne modified PS-NPs, that capture the PNA:miR-122 complex. These PS-NPs are particularly notable for their compatibility with standard multistep chemistries and for enabling several orthogonal conjugation strategies²⁴⁻²⁶, allowing us to double functionalised them with a fluorophore and with the cyclooctyne moiety. The second type of fluorescently labelled silica nanoparticles are functionalised with streptavidin to detect the biotin derived from the specific SMART-Nucleobase that binds the nucleobase of interest. This approach was carried out using a conventional flow cytometer as a reading platform, which is a widely used tool in clinical laboratories and provides an accessible method for miRNA detection.

In recent years, click chemistry has gained considerable recognition as a powerful method for the rapid and efficient covalent linking of chemical groups. One of the bestknown click chemistry reactions is the copper-catalysed Alkyne-Azide Cycloaddition (CuAAC) reaction that both Meldal²⁷ and Sharpless²⁸ presented in 2002. It uses a Huisgen 1,3-dipolar cycloaddition to produce triazoles. This method involves the combination of organic azides with alkyne groups to form 1,2,3-triazoles. Importantly, these chemical groups exhibit low or no reactivity towards most functional groups commonly found in biomolecules such as nucleic acids, proteins, and lipids^{29–31}. Consequently, click chemistry is considered a bioorthogonal and biocompatible reaction, especially when Bertozzi demonstrated the copper-free Alkyne-Azide cycloaddition by using cyclooctyne as alkynes for these condensations³². The inherent speed and efficiency of this reaction, combined with its compatibility with nucleic acids, has made click chemistry highly applicable in the development of diagnostic tools³³. By incorporating click chemistry into the dual nanosystem system here presented, we benefit from its simplicity, which facilitates rapid and efficient covalent capture of PNA:miR-122 complexes on the surface of polystyrene nanoparticles, and allows us to perform DCL reactions in solution and use a standard flow cytometer for reading. Using the dual nanosystem presented here, we analysed miR-122 expression in different tumour cell lines with specificity and robustness, showing a high correlation with results obtained from a TaqMan assay and in a sensitive manner. We also detected miR-122 in a serum matrix and identified four SNVs at a specific position within synthetic miR-122 sequences.

2. Results and discussion

2.1. Dual nanosystem Engineering

Based on the native mature sequence of miR-122 (miRBase ID: hsa-miR-122-5p), we designed a complementary 18-mer abasic PNA probe with an abasic position in the central region, represented as $*GL^*$, containing a secondary amine and a glutamic acidlike side chain at its gamma position directly opposite a guanine (underlined in the hsamiR-122-5p sequence). The abasic PNA probe also contains an azide moiety via a spacer (two diethylene glycol units, miniPEG, shown as "OO") to allow the click chemistry reaction. In addition, we have introduced glutamic acid-like side chains at the gamma positions in the backbone of certain PNA units (shown as Cglu and Tglu) to facilitate the templated DCL reaction between SMART-Nucleobases and the secondary amine of the abasic site³⁴. We performed DCL reactions in solution using the abasic PNA probe and different target sequences such as ssDNA-122, ssRNA-122 and hsa-miR-122-5p extracted and pre-amplified from tumour cell lysates (Figure 1A), with all sequences listed in Table 1. When added to the solution, the abasic PNA probe hybridises with the miR-122 target, with the abasic position opposite a guanine. This guanine templates the incorporation of a biotinylated SMART-Cytosine (SMART-C-Biotin), forming a biotinylated PNA:miR-122 complex (Figure 1B). The chemical structures of the abasic PNA probe and SMART-C-Biotin are shown in detail in the inset of Figure 1B. Then, polystyrene nanoparticles, called BCN-Cy5-NPs (12), are added to the solution. These nanoparticles have cyanine-5 (Cy5) fluorescent tags and are coated with a cyclooctyne moiety (BCN), which facilitates copper-free click chemistry azide-labelled PNA probes, thereby capturing the biotinylated PNA:miR-122 complex. Next, silica nanoparticles, called Strep-LINARDA (L3), are added to the solution. These nanoparticles are labelled with yellow-green emitting fluorophores similar to cyanine-3 (Cy3) and coated with streptavidin to recognise the SMART-C-Biotin. Following the click chemistry reaction and streptavidin-biotin recognition, both nanoparticles, the BCN-Cy5-NPs (12) and Strep-LINARDA (L3), bind together through the PNA:miR-122 complex, forming a dual nanosystem (Figure 1C). Therefore, the higher the amount of miR-122 in the sample, the higher the number of biotinylated PNA:miR-122 complexes formed, and consequently, the higher the number of dual nanosystems detected. When analysed with a standard flow cytometer, the dual nanosystem generates two co-localised fluorescent signals,

Cy5+/Cy3+, which served as markers for miR-122 detection with single base specificity (**Figure 1D**). Further thetails about the chemical structure of the basic PNA and all the biotinylated SMART-Nucleobases can be found in *Supporting Information 1*. Moreover, we performed further studies on miR-122 sequences and additional targets, whose sequences are listed in *Supporting Information 2*.



Figure 1. Click chemistry driven dual nanosystem workflow. A. Hsa-miR-122-5p sequences are isolated from tumour cell lines and pre-amplified by PCR. B. The addition of abasic PNA probes that hybridise to the miR-122 target, together with the addition of the SMART-C-Biotin, initiates the DCL reaction, resulting in the formation of biotinylated PNA:miR-122 complexes. The inset shows the chemical structures of the abasic PNA probe and SMART-C-Biotin. C. Two types of nanoparticles are then added: First, polystyrene nanoparticles, BCN-Cy5 NPs (12), labelled with Cy5 and coated with cyclooctyne (BCN) moieties. These nanoparticles allow copper-free click chemistry to capture the PNA:miR-122 complex. Second, silica nanoparticles, Strep-LINARDA (L3), which are Cy3-labelled and coated with streptavidin for recognition of the biotinylated SMART-Nucleobase. When both nanoparticles are bound by the PNA:miR-122 complex, they form the dual nanosystem. D. Co-detection of Cy5+/Cy3+ signals using a standard flow cytometer indicates detection of miR-122 with single base specificity.

Probe and target	Sequence (N-term – C-term or 5'-3')		
Abasic PNA-122	Ac-Lys(N ₃)-OO-CACCAT Tglu GT*GL*A Cglu AC Tglu CCA-NH ₂		
hsa-miR-122-5p & ssRNA-122	UGGAGUGU <u>G</u> ACAAUGGUGUUUG		
ssDNA-122	TGGAGTGT <u>G</u> ACAATGGTG		
ssDNA-122-Cy5	Cy5-TGGAGT <u>G</u> TGACAATGGTG		
ssDNA-122 (T)	TGGAGTGT <u>T</u> ACAATGGTG		
ssDNA-122 (C)	TGGAGTGT <u>C</u> ACAATGGTG		
ssDNA-122 (A)	TGGAGTGT <u>A</u> ACAATGGTG		
hsa-miR-122-5p Amplicon form (isolated and amplified from tumour cell lines)			

Table 1: Sequences of abasic PNA probes and miR-122 targets used in the dual nanosystem.

Note: PNA sequences hybridise to complementary nucleic acids in an antiparallel fashion, meaning their C-terminal end faces the 5' end, while their N-terminal end faces the 3' end of the nucleic acid. Italic A, T, C and G represent PNA-based adenine, thymine, cytosine and guanine units. Cglu and Tglu represent

cytosine and thymine PNA units with glutamic acid-like side chains at their gamma positions. *GL* indicates the abasic position. Nucleotides that template the SMART-Nucleobase reaction with the abasic site of the PNA probe are underlined.

2.2. Synthesis, characterisation and validation of the dual nanosystem for miR-122 detection

In the synthesis of the components of the dual nanosystem, the synthesis of polystyrene nanoparticles, BCN-Cy5-NPs (12), begins with the generation of aminofunctionalised PS-NPs (1), which are then bifunctionalised using previously reported solid-phase synthesis methods²⁴. Monomers are conjugated to the amino PS-NPs (1) by activating the carboxyl group and forming amide bonds. These monomers have protective groups, specifically Fmoc and Dde moieties, which allow stepwise and orthogonal synthesis. This allows bifunctionalisation with Cy5 fluorophores and BCN moieties, avoiding cross reactions (Figure 2A). Once synthesised, BCN-Cy5 NPs (12) can be monitored by flow cytometry due to their Cy5 labelling. They can also conduct copperfree click chemistry by reacting with azide-labelled PNA in solution via the BCN moiety. The detailed synthesis for PS-NPs (1) is described in Supporting Information 3.1, while the full synthesis procedure for BCN-Cy5-NPs (12) is detailed in Supporting Information 3.2. The second type of silica nanoparticles, Strep-LINARDA (L3), are carboxylic acid functionalised and labelled with Cy3-like fluorophores. They were directly conjugated to streptavidin by activating the carboxylic acid group with EDC and sulfo-NHS (Figure 2B). The result was Strep-LINARDA (L3), which can recognise the biotinylated SMART-Nucleobases.



Figure 2. Nanoparticle synthesis. A. Synthesis of BCN-Cy5 NPs (12) starts with amino-functionalised PS-NPs (1). Protected monomers Fmoc-Gly-OH, Fmoc-PEG-OH, Fmoc-Lys(Dde)-OH and Fmoc-PEG-OH are sequentially coupled. Next, the Dde group is selectively removed to obtain to obtain PS-NPs (9) and the activated sulfo-Cy5-NHS ester is conjugated. The Fmoc group is then removed and the activated BCN succinimidyl ester is conjugated to obtain bifunctionalised BCN-Cy5-NPs (12). B. Synthesis of Strep-

LINARDA (L3) consist on the activation of the carboxylic groups using EDC and sulfo-NHS to allow the conjugation of streptavidin to obtain the Strep-LINARDA (L3) nanoparticles.

After the synthesis of both nanoparticles, their physicochemical characterisation was carried out. The size and homogeneity of the nanoparticles and their polydispersity index (PDI) were measured by Dynamic Light Scattering (DLS), which confirmed a similar nanoscale size and that both types of nanoparticles were monodispersed and homogeneous (Table 2, Figure 3A). In order to assess the change in the nanoparticle surface after the synthesis and its potential impact on surface stability, the zeta potential of the nanoparticles was also measured (Table 2, Figure 3A). A lower zeta potential was observed in the functionalised BCN-Cy5 NPs (12) and Strep-LINARDA (L3), compared to the PS-NPs (1), probably due to the presence of sulphonic groups, but these zeta potentials did not show a significant change on the nanoparticle surface, indicating that the nanoparticles remain stable after conjugations. In addition, the efficiency of Cv5 conjugation to BCN-Cy5-NPs (12) and the conjugation of streptavidin to Strep-LINARDA (L3) were evaluated, demonstrating successful conjugation rates in both cases (Table 2, Figure 3B). Transmission electron microscopy (TEM) confirmed the morphology and size of both types of nanoparticles (Figure 3C). Additional physicochemical characterisation was performed to assess the size, uniformity and zeta potential of the nanoparticles in all buffers used in this study, including in a serum matrix. Detailed of these results are shown in Supporting Information 4.1.

Parameters	NH2-PS-NPs (1)	BCN-Cy5-NPs (12)	Strep-LINARDA (L3)
Mean Hydrodynamic Diameter (nm)	415.6 ± 14.5	481.5 ± 12.5	362.5 ± 25.3
Mean Zeta Potential (mV)	41.65 ± 0.41	-14.8 ± 1.56	$\textbf{-25.91} \pm 0.71$
Polydispersity Index (PDI)	0.184	0.119	0.267
Conjugation efficiency	-	96.45 %	99.7 %
Loading molecules/NPs	-	2.57×10^{6}	2.69×10^{8}

 Table 2. Physicochemical parameters of nanoparticles

Then, we validated the ability of the dual nanosystem to detect miR-122 using a Fluorescence-Activated Cell Sorting cytometer, FACSVerse, following the experimental design described in **Table 3**. When analysed on FACSVerse, the BCN-Cy5-NPs (12) showed a Cy5+/Cy3- population, whereas the Strep-LINARDA (L3) showed a Cy5-/Cy3+ population (**Figure 3D**, in black). Then, we evaluated the efficacy of the BCN groups conjugated to the polystyrene nanoparticles. For this purpose, we designed a third type of polystyrene nanoparticles that were synthesised without the Cy5 dye but conjugated to BCN, called BCN-NPs (14) (see synthesis and structure in *Supporting Information 3.3*). We then used synthetic ssDNA-122 labelled with the Cy5 fluorophore (ssDNA-122-Cy5) as the target. When we mixed the BCN-NPs (14) with ssDNA-122-Cy5 in the absence of the abasic PNA probe, no population showing Cy5 fluorescence was detected (**Figure 3D**, left red dot plot). However, upon addition of the abasic PNA probe, the entire nanoparticle population showed Cy5 fluorescence (**Figure 3D**, right red dot plot). This indicates successful capture of the PNA:miR-122 complex formed in

solution by hybridisation via a copper-free click chemistry reaction. It also highlights that polystyrene nanoparticles do not adsorb oligonucleotides. Next, we evaluated the ability of the dual nanosystem to detect miR-122. To do this, a DCL reaction was performed according to the procedure described in section 2.6. When we evaluated the nanosystem in the absence of ssDNA-122 as a negative control, a Cy5+/Cy3- population was formed (Figure 3D, left blue dot plot). Remarkably, in the presence of ssDNA-122, there was a marked shift towards a significant double Cy5+/Cy3+ population, indicating the successful detection of ssDNA-122 (Figure 3D, right blue dot plot). Similarly, when we analysed ssRNA-122, we observed a significant double Cy5+/Cy3+ population (Figure **3D**, green). Figure **3E** illustrates the event counts (n=3) recorded in FACSVerse for each condition, highlighting the statistical significance of the dual nanosystems in detecting both ssDNA-122 and ssRNA-122 sequences. We performed an additional evaluation of the dual nanosystem using a different type of silica nanoparticles, DiagNano[™] (CD Bioparticles, UK), as a commercial alternative to Strep-LINARDA (L3). Our results confirmed the successful detection of miR-122, demonstrating the versatility of combining the nanosystem with other nanoparticle types. These results are presented in Supporting Information 4.2.



Figure 3. Dual nanosystem characterisation and miR-122 detection by FACSVerse. A. Size distribution (left) and zeta potential values (right) for PS NPs (1), BCN-Cy5-NPs (12) and Strep-LINARDA (L3). B. Calibration curves for Cy5 and streptavidin conjugation yielding 96.45% and 99.7% conjugation rates respectively. C. Size and morphology analysis by TEM of BCN-Cy5-NPs (12) (left) and Strep-LINARDA (L3) (right) (100 nm scale bar above, 500 nm scale bar below). D. Individual signals generated by both nanoparticles in black. Dot plots in red show BCN-NPs (14) incubated with ssDNA-122-Cy5 without the abasic PNA probe as a negative control (left), turning Cy5+ in the presence of the abasic PNA probe (right), confirming the click chemistry reaction. Dot plots in blue represent both nanoparticles in the

presence of all components but without ssDNA-122 target as a negative control (left), becoming Cy5+/Cy3+ in the presence of ssDNA-122 (right), highlighting miR-122 detection. The same scheme is shown in green for the detection of ssRNA-122. E. Event count (n=3) for both ssDNA-122 (blue) and ssRNA-122 (green). A significant increase in the Cy5+/Cy3+ subset occurs when the dual nanosystem is formed when either ssDNA-122 or ssRNA-122 is present, compared to simply mixing the nanoparticles (Mix NPs) or having the PNA probe without the target (NC). Error bars = standard deviation.

Name	Condition	Expected population*
BCN-Cy5 NPs (12)	Only nanoparticles 12	Cy5+/Cy3-
Strep-LINARDA (L3)	Only nanoparticles L3	Cy5-/Cy3+
Hybridisation NC	Only nanoparticles 14 were incubated with ssDNA-122-Cy5 in absence of the PNA probe	Су5-
Hybridisation CTRL	Only nanoparticles 14 were incubated with ssDNA-122-Cy5 in presence of the PNA probe	Cy5+
Mix NPs	Mixture of nanoparticles 12 and L3 in hybridisation buffer with no additional components	Cy5+/Cy3 & Cy5-/Cy3+
Dual NC	Presence of all system components, but no target miR-122	Cy5+/Cy3- & Cy5-/Cy3+
Dual NS (ssDNA-122)	DCL reaction with all the components using ssDNA-122 as target	Cy5+/Cy3+
Dual NS (ssRNA-122)	DCL reaction with all the components using ssRNA-122 as target	Cy5+/Cy3+

 Table 3. Experimental conditions for validation of miR-122 detection using the dual nanosystems in FACSVerse

*Expected nanoparticles populations based on their fluorescence assuming 100% efficiency. NC=Negative Control. Dual NC= Dual nanosystem Negative Control. Dual NS= Dual Nanosystem.

These results demonstrated the successful synthesis of both types of nanoparticles with homogeneity and stability after synthesis, as shown by their physicochemical characterisation. In addition, the results indicated that the click chemistry reaction takes place with high efficiency and specificity. Finally, these results showed that both types of nanoparticles bind and capture the PNA:miR-122 complex, forming a dual structure that can be easily monitored by flow cytometry, allowing the successful detection of miR-122.

2.3. Detection of miR-122 in a serum matrix, calibration curve and evaluation of single base specificity

Then, we proceeded to evaluate the ability of the dual nanosystem to detect miR-122 in a biological matrix to challenge the system. To do this, we performed the following experiments in 10% of human serum. Under these conditions, we established a calibration curve to determine the analytical performance and limit of detection (LoD), and evaluated the specificity in detecting nucleotide variations. We established the calibration curve by performing triplicate dilutions of ssDNA-122 within a range covering from 50 pmoles to 0.5 pmoles in 10% of human serum in a final volume of 50 μ L. Then, we calculated the average number of events within the double Cy5+/Cy3+ population based on a total of 10,000 events recorded in FACSVerse. The resulting average number of events showed a sigmoidal regression curve (R²=0.9) (**Figure 4A**, left) with a coefficient of variation ranging from 0.9% to 9.22%, indicating low variability of the data. We then determined the LoD using a 4-parameter logistic regression model (4PL). First, the limit of blank (LoB) was calculated using formula (1), and then this LoB value was substituted into the variable "y" in formula (2). The LoD was quantified as 2.329 pmol in 50 μ L.

$$LoB = Blank Average (n = 6) + 3.3 * SD_{Average}$$
(1)

$$y = Bottom + \frac{Top - Bottom}{1 + \left(\frac{x}{IC50}\right)^{HillSlope}}$$
(2)

We found that the signal from the blank corresponds, mostly, to the signal generated by the non-specific interaction between BCN-Cy5-NPs (12) and Strep-LINARDA (L3), hence impacting in the LoD. To investigate whether the dual nanosystem could achieve a lower LoD in the absence of this non-specific signal, we analysed the detection of dilutions of ssDNA-122-Cy5 using the unlabelled BCN-NPs (14). Thus, positive Cy5 signals within the double positive Cy5+/Cy3+ population reflect only the amount of ssDNA-122-Cy5 captured by click chemistry, excluding any non-specific signal. When analysing a 4PL, we found that the LoD was 1.08 femtomoles in 50 μ L (**Figure 4A**, right), which is more than 2,000 orders of magnitude lower, demonstrating the potential room for improvement of this dual nanosystem.



Figure 4. Calibration curve of miR-122 in serum matrix, SNV detection and MALDI-TOF analysis. A. Left, the calibration curve for the detection of ssDNA-122 in 10% serum showed a 4PL non-linear regression model in FACSVerse. LoD = 2.329 pmol. $R^2 = 0.9$. Right, calibration curve for the detection of ssDNA-122-Cy5 and unlabelled BCN-NPs (14). LoD = 1.08 fmoles. $R^2 = 0.98$. B. FACSVerse analysis of four SNVs representing four isomiR-122. Only when the complementary biotinylated SMART-Nucleobase (shown as SC, SA, SG or ST) is used, the dual nanosystem generates a significant Cy5+/Cy3+ population. C. MALDI-TOF analysis was performed on the four SNVs to evaluate the cross-reactivity between the SMART-Nucleobases. The spectra showed two main peaks representing the unreacted abasic PNA probe (left) and the probe with the biotinylated SMART-Nucleobase incorporated (right). The difference between these peaks indicated the molecular mass of the specific SMART-Nucleobase incorporated, enabling identification of the targeted nucleobase.

Next, we investigated the ability to discriminate nucleotide variations. For this end, the abasic PNA probe was hybridised in triplicate to four ssDNA-122 strands with sequences differing by only one nucleotide (A, C, G or T) in the position opposite to the abasic site (Table 1), thus mimicking four isomiR-122 variants. For each sequence, four individual DCL reactions were performed in 10% serum using one of the biotinylated SMART-Nucleobases (SMART-C-biotin, SMART-A-biotin, SMART-G-biotin, or SMART-T-biotin). Then, we analysed the results obtained in FACSVerse and confirmed that only the specific SMART-Nucleobase resulted in a statistically significant double Cy5+/Cy3+ population signal (Figure 4B). These results demonstrated the ability of the dual nanosystem to detect the specific SNV at a targeted nucleobase position within the miR-122 sequence. To further validate the dual nanosystem and broader applicability, we also used two additional abasic PNA probes to analysed two nucleotide positions in miR-21, another miRNA known for its role in tumour development³⁵. These data are shown in Supporting Information 4.3. With these results, we further confirm the possibility of using the dual nanosystem to study additional targets and probes, as well as the ability to study other nucleobase positions.

To further analyse the specificity of the biotinylated SMART-Nucleobases and whether there was any cross-reactivity between them, we performed MALDI-TOF analysis. For this, four individual DCL reactions were performed, each using one of the four ssDNA-122 sequences differing by one nucleotide (Table 1). Each ssDNA-122 was mixed in a solution containing the abasic PNA probe and a mixture with all four biotinylated SMART-Nucleobases. The product was then analysed by MALDI-TOF, which revealed two main peaks in the spectra: one peak corresponding to the unreacted abasic PNA probe and a second peak corresponding to the abasic PNA probe plus the biotinylated SMART-Nucleobase. The difference between these peaks corresponds to the molecular weight of the incorporated SMART-Nucleobase. The results showed that only the complementary SMART-Nucleobase was successfully incorporated into the abasic position, with no cross-reactivity observed (Figure 4C). See Supporting Information 5 for detailed data. We also performed further MALDI-TOF analyses to verify the detection of SMART-T-Biotin, due to its molecular weight being close to that of SMART-C-Biotin, as detailed in Supporting Information 5.1. In addition, we also tested cross-reactivity using four templates of ssRNA-122 that differ in just one nucleotide (5'UGGAGUGU-G/A/C/U-ACAAUGGUGUUUG3'), and obtained similar results when the template was ssRNA-122. These results are presented in Supporting Information 5.2. All results presented in this section confirm that the dual nanosystem using FACSVerse detects miR-122 in a biological matrix with specificity and robustness, and demonstrates its ability to discriminate with high accuracy between four miR-122 sequences that differ by only one nucleotide.

2.4. Analysis of hsa-miR-122-5p expression in tumour cell lines

Next, we investigated the expression of miR-122 in different tumour cell lines using the dual nanosystem and compared the results with miR-122 expression using a TaqMan assay, a well-established method for studying miRNA expression in cell lines,

commercially available from Thermo Scientific (USA). In this assay, we combined the dual nanosystem with qPCR, where the RNA is reverse transcribed into complementary DNA (cDNA) and then amplified, producing a DNA template (instead of RNA) for the DCL reaction. This approach has the advantage of increased stability and longer sample storage times. Therefore, in the previous section 2.3, we mainly characterised the dual nanosystem using ssDNA-122 instead of ssRNA-122. We first compared the two methods by generating a calibration curve using the full sequence of ssRNA-122 (5' UGGAGUGUGACAAUGGUGUUUG 3') as the starting target. We performed a series of dilutions in triplicate, using amounts of ssRNA-122 ranging from 1 ng to 10⁻⁸ ng. corresponding to 8×10^{10} to 8×10^2 copies of ssRNA-122. The RNA was then reverse transcribed into cDNA and subjected to RT-qPCR using TaqMan probes. The result of plotting these quantities against the cycle threshold (Ct) demonstrated a linear regression $(R^2=0.995)$ with coefficients of variation ranging from 0.25% to 7% (Figure 5A, left). The same PCR products were then subjected to the dual nanosystem and analysed by FACSVerse. In this case, the result of plotting these quantities against the number of Cy5+/Cy3+ events yielded a sigmoidal regression curve (R²=0.968) with coefficients of variation ranging from 1.25% to 25% (Figure 5A, right). The LoD was then determined for both methods. For the TaqMan assay, the LoD was calculated as 3.29 times the standard deviation of the negative control divided by the slope of the calibration curve. The LoD was quantified as 5 copies in a final reaction volume of 20 µL, corresponding to 8.30×10^{-24} moles (8.3 ymoles) of miR-122. The LoD of the dual nanosystem was then calculated using the 4PL model described in section 3.3. The LoD was quantified as 750 copies in a final volume of 50 μ L, corresponding to 1.3×10^{-21} moles (1.3 zmoles) of miR-122.



Figure 5. Analysis of miR-122 expression in tumour cell lines using TaqMan probes and the dual nanosystem. A. Calibration curves of both methods in RT-qPCR products of ssRNA-122. On the left, the TaqMan probes show a linear regression curve. On the right, the dual nanosystem shows a sigmoidal

regression curve. B. Analysis of hsa-miR-122 expression in tumour cell lines. On the left, the TaqMan assay showed high hsa-miR-122 expression in HuH-7. Similarly, on the right, the dual nanosystem showed high hsa-miR-122 expression in HuH-7, followed by a lower expression in HepG2 and little to no expression in A549 or SKBR3.

Then, we analysed hsa-miR-122 expression in tumour cell lines. Since hsa-miR-122 is specific for liver tissue, we chose two human hepatocellular carcinoma cell lines: HuH-7, which has been reported in the literature to have high levels of miR-122 expression, and HepG2, which has been reported to have a lower miR-122 expression ^{36,37}. We also selected two additional cancer cell lines of clinical interest for studying miR-122: A549, derived from lung cancer, which according to the literature has little or no expression of miR-122³⁸, and SKBR3, derived from breast cancer, which, according to the literature, have low intracellular expression of miR-122³⁹. We cultured the cell lines to confluence and extracted total miRNA from one million cell pellets in triplicate. Then, we performed reverse transcription of miR-122, followed by qPCR amplification using TaqMan probes using RNU44 as a normalizer. Then, we analysed the same amplicons using the dual nanosystem via FACSVerse. Using both methods, we found high miR-122 expression in the HuH-7 cell line, followed by lower expression in HepG2, reduced expression in SKBR-3 and little to no expression in A549 (Figure 5B). Extrapolating from the calibration curve, in the TaqMan assay, we found an expression of 4.51×10^6 copies of miR-122 in HuH-7 and 3.47×10^3 copies in HepG2. Meanwhile, with the dual nanosystem, we found 3.69×10^6 copies in HuH-7 and 3.22×10^4 copies in HepG2. These results demonstrate the analytical capability of the dual nanosystem to analyse hsa-miR-122 expression in tumour cell lines, identifying up to 750 copies (1.3 zmol) in 50 µL (26 attomolar) volume when combined with PCR. Although the calibration curve showed higher variability at top values compared to the TaqMan assay, we attribute this to the fact that the flow cytometer may interpret a cluster of nanoparticles as a single event. However, this did not affect the accuracy of the miR-122 expression analysis of the cell lines. Remarkably, the dual nanosystem results highly correlated with the TaqMan assay. This highlights the effectiveness of the dual nanosystem in performing miR-122 expression analysis, while maintaining methodological robustness, compatibility with standard flow cytometers as a readily accessible platform, and the ability to analyse SNVs and truncated miRNA sequences.

3. Conclusions

In this study, we present a click chemistry driven dual nanosystem designed for single base specific miR-122 detection using a standard flow cytometer as the reading platform. Using the dual nanosystem, we analysed miR-122 expression in different tumour cell lines with high performance and specificity, showing a high correlation with results obtained from a TaqMan assay and in a sensitive manner. We also detected miR-122 using a serum matrix and identified four single SNVs at a specific position within the miR-122 sequence with robustness. The dual nanosystem demonstrated a direct limit of detection (LoD) of 2.329 pmol in a 50 μ L solution in a human serum matrix. In addition, when combined with RT-qPCR, the dual nanosystem achieved a LoD of 1.3 zmol in 50

 μ L (26 attomolar). The dual nanosystem proved effective in analysing the expression of hsa-miR-122, showing high expression in the HuH-7 cell line, lower expression in HepG2 and reduced to no expression in SKBR3 and A549, in line with the literature. This dual nanosystem involves a fully bioorthogonal strategy that includes signal amplification using two types of different nanoparticles, polystyrene and silica, together with the high affinity of PNA probes. These nanoparticles are able to bind when capturing miR-122 in a dual structure that can be easily monitored using a flow cytometer. The chemical methods used here to synthesise nanoparticles and perform click chemistry reactions, together with the DCL method for miRNA detection, show great flexibility and provide a basic toolbox that could be further extended with many types of bioorthogonal reactions, and the incorporation of click chemistry into the system allows for the speed, efficiency and compatibility of this reaction with nucleic acids. In summary, the chemistry used in this dual nanosystem offers remarkable versatility and provides a promising opportunity to pioneer enzyme-free nanoparticle-based strategies based on click chemistry and bioorthogonality for miRNA detection and isomiR studies and thus, contributing to the advancement of molecular diagnostic applications.

4. Methodology

4.1. General

Chemicals and solvents were purchased from Sigma Aldrich. Fmoc-Gly-OH was purchased from Sigma Aldrich, and Fmoc-PEG₃-COOH and Fmoc-Lys (Dde)-OH were synthesised as described previously²⁴. N-[((1R,8S,9s)-bicyclo[6.1.0]non-4-yn-9yl)methyloxycarbonyloxy]succinimide carbonate (BCN-succinimidyl ester) was purchased from Sigma Aldrich, sulfo-Cy5-NHS ester was purchased from Lumiprobe (USA) and streptavidin was purchased from Promega (USA). The size distribution, determined by DLS, and the zeta potential of the nanoparticles were measured using a BeNano 180 Zeta Pro instrument from Bettersize Instruments (China). The bioconjugation efficiency of the fluorophore and streptavidin was measured using the NanoQuant Plate[™] from Tecan (Switzerland). Microscopic images were acquired using a TALOS F200C G2 transmission electron microscope. The number of nanoparticles per volume was determined using a previously described spectrophotometric method⁴⁰. Flow cytometry data were acquired using a FACSVerse, BD Biosciences (USA). Acquisition was performed using lasers emitting at 488 nm and 633 nm as excitation sources, while fluorescence emissions were detected with filters at 585/42 nm for the phycoerythrin (PE) channel and 660/20 nm for the allophycocyanin (APC) channel. FACS data were analysed based on the total number of events within the APC/PE subset (representing the Cy5/Cy3 subset), using a mean flow rate for reading and recording of 10,000 events.

4.2. Design and Synthesis of Abasic PNA Probes, SMART-Nucleobases, Single-Stranded DNA and RNA Oligonucleotides

The abasic PNA probe and SMART-Nucleobases were both provided by DESTINA Genomica SL. (Spain). The synthesis of the abasic PNA probe followed standard polymer-supported solid-phase synthesis techniques in Tentagel resin from

Polymer (UK) using an Intavis Bioanalytical MultiPrep CF synthesiser from Intavis AG GmbH (Germany). The SMART-Nucleobases used were SMART-Cytosine-REX-PEG₁₂-Biotin (referred to as SMART-C-Biotin), SMART-Adenine-deaza-enol-PEG₁₂-Biotin (SMART-A-Biotin), SMART-Guanine-deaza-enol-PEG₁₂-Biotin (SMART-A-Biotin), SMART-Guanine-deaza-enol-PEG₁₂-Biotin (SMART-G-Biotin) and SMART-Thymine-REX-PEG₁₂-Biotin (SMART-T-Biotin). The structure of the abasic PNA and SMART-Nucleobases is detailed in *Supporting Information 1*. All single-stranded DNA (ssDNA) or RNA (ssRNA) oligonucleotides used in this study were purchased from Microsynth (Switzerland) or IDT (USA). The sequences of all ssDNA and ssRNA oligonucleotides and the abasic PNAs used in this study are provided in *Supporting Information 2*.

4.3 Synthesis of PS-NPs (1), BCN-Cy5-NPs (12) and BCN-NPs (14)

PS-NPs (1) with a size of 500 nm and an amine group loading of 0.0014 mmol/mL (corresponding to 1 mEq) were synthesised using a dispersion polymerisation process as previously reported²⁴. The complete synthesis procedure of PS-NPs (1) is described in detail in Supporting Information 3.1. The synthesis of BCN-Cy5 NPs (12) was performed by solid phase peptide synthesis techniques as previously described²⁴. All reactions were performed in a thermoshaker (1,200-1,400 rpm, 25°C). Coupling reactions were performed using ethyl cyanohydroxyiminoacetate (Oxyma) (50 equiv, 140 mM) and N,N'-diisopropylcarbodiimide (DIC) (50 equiv, 140 mM) as coupling agents with 50 equiv of Fmoc-protected amino acids at 140 mM concentration, unless otherwise stated. After the coupling reaction, Fmoc was deprotected with 20% piperidine before proceeding to the next coupling. Fmoc-Gly-OH, Fmoc-PEG-OH and Fmoc-Lys(Dde)-OH were coupled to PS-NP (1) in this order to give Fmoc-PEG(Dde)-NPs (8)⁴¹. The Dde group was then selectively deprotected with an NH2OH-HCl/imidazole in 1-methyl-2pyrrolidinone as described elsewhere⁴². The activated sulfo-Cy5 NHS ester (0.321 μ M) in DMF was then used to conjugate the dye to this side chain using N,Ndiisopropylethylamine (DIPEA) in 250 µL anhydrous DMF. After coupling of the dye, the Fmoc group was removed to give Cy5-NPs (11). The coupling between the free amine of the NPs (11) and the activated BCN succinimidyl ester (20 equiv, 27.5 mM) and 0.2 µL DIPEA was performed in 250 µL anhydrous DMF to obtain bifunctionalised BCN-Cy5-NPs (12). Finally, the BCN-Cy5-NPs (12) were washed and stored in water. The complete synthesis procedure of BCN-Cy5-NPs (12) is described in detail in Supporting Information 3.2. In addition, to test for the absence of non-specific binding of nucleic acids to the nanoparticle surface, unlabelled nanoparticles with BCN, termed BCN-NPs (14), were used. The synthesis procedure and structure of BCN-NPs (14) are described in detail in Supporting Information 3.3.

4.4. Synthesis of Strep-LINARDA (L3) detection NPs

LINARDA nanoparticles were supplied by GENOTIX Biotechnologies (USA). LINARDA nanoparticles are also 500 nm in size, exhibit yellow-green fluorescence (Cy3-like) and are carboxyl functionalised. These nanoparticles were conjugated to streptavidin using 1-ethyl-3-carbodiimide (EDC) and N-hydroxysulfosuccinimide (Sulfo-NHS). The process started with centrifugation of 50 μ L stock COOH-LINARDA (L1) (1.5×10⁸ NPs/ μ L) at 13,400 rpm for 3 min to remove the supernatant. Nanoparticles were then conditioned twice with 100 µL of 50 mM 2-morpholinoethanesulfonic acid (MES) buffer at pH 5.5, followed by centrifugation at 13,400 rpm for 3 min. The pellet was resuspended in 80 μ L 50 mM MES pH 5.5 and 10 μ L EDC (50 mg/mL) and 10 μ L Sulfo-NHS (50 mg/mL), both freshly prepared in 50 mM MES pH 5.5, were added to the mixture. After incubation for 20 min at 1,200 rpm and 25°C, LINARDA (L2) nanoparticles were centrifuged at 13,400 rpm for 3 min, washed twice with 100 µL 50 mM MES pH 5.5, conditioned with 100 µL 50 mM MES pH 6 and centrifuged at 13,400 rpm for 3 min. After removal of the supernatant, 100 µL streptavidin at 150 µg/mL in 50mM MES pH 6 was added to the LINARDA (L2) nanoparticles. This mixture was incubated for 2 hours at 1,200 rpm and 25°C. Finally, the conjugated LINARDA (L3) nanoparticles were centrifuged at 13,400 rpm for 3 minutes, washed with 200 µL LINARDA Wash Buffer, centrifuged again under the same conditions and incubated with LINARDA Quenching Buffer for 1 hour at RT. After quenching, Strep-LINARDA (L3) was washed twice with 250 µL LINARDA Wash Buffer and stored in 2 mL Super Assay Buffer (Genotix Biotechnologies, USA). Throughout the protocol, sonication and vortexing were used to avoid aggregates and ensure a good conjugation yield.

4.5. DCL reaction and miR-122 detection with single-base specificity by FACS

DCL reactions were performed in a hybridisation buffer containing $2 \times$ sodium citrate (SSC) with 0.1% Tween 20, with pH carefully adjusted to 6.0 in a final volume of 50 µL. The reaction mixture contained 1 µM abasic PNA probe, 1 µM either ssDNA-122 (5'TGGAGTGT<u>G</u>ACAATGGTG3'), ssRNA-122

(5'UGGAGUGU<u>G</u>ACAAUGGUGUUUG3') or water for negative control, 5 μ M biotinylated SMART-Nucleobase and 1 mM reducing agent sodium cyanoborohydride (NaBH₃CN). The DCL reaction was incubated for 1 hour at 40°C and 1,400 rpm. Then 1 μ L containing 1.46×10⁹ BCN-Cy5 NPs (12) was added and incubated for 1 hour at 25°C with shaking at 1,400 rpm. After incubation, the solution was centrifuged at 13,400 rpm for 5 minutes and the pellet was washed twice with 200 μ L of 1×PBS with 0.1% Tween 20 to remove any excess of biotinylated SMART-Nucleobase. After washing, the supernatant was discarded and 50 μ L Strep-LINARDA (L3) at 25,000 NPs/ μ L was added in Super Assay Buffer. This mixture was incubated for 30 min at 30°C and 1,200 rpm. Finally, 150 μ L of Super Assay Buffer was added and the sample was analysed on the FACSVerse.

4.6. Detection of miR-122 in a serum matrix, calibration curve and evaluation of single base specificity

The serum samples used were obtained from healthy donors from the Biobank of the Andalusian Public Health System (agreement number S1900507). In this case, DCL reactions were performed in Stablitech buffer from DESTINA Genomica (Spain) with a final serum concentration of 10% and a pH carefully adjusted to 6. For the calibration curve, different concentrations of ssDNA-122 were added to the serum (50 pmol, 37.5 pmol, 25 pmol, 12.5 pmol, 5 pmol and 0.5 pmol) in triplicates in a final volume of 50 μ L. The following steps were performed as described in the previous *section 2.6*. To specifically detect the target nucleobase of interest in the ssDNA-122 sequence, four

independent assays were performed in stablitech buffer containing 10% serum using four ssDNA-122 sequences at 1 μ M. Each ssDNA-122 sequence carries a different SNV (5'TGGAGTGT-<u>G/T/C/A</u>-ACAATGGTG-3'). Each ssDNA-122 was then incubated with one of the biotinylated SMART-Nucleobases (SMART-C-biotin, SMART-T-biotin, SMART-G-biotin and SMART-A-biotin) at a concentration of 5 μ M. Samples were then analysed as described in *section 2.6*.

4.7. MALDI-TOF analysis to assess cross-reactivity of SMART-Nucleobases

MALDI-TOF analyses were performed in 2× SSC buffer with 0.1% Tween 20 at pH 6. The abasic PNA probe concentration was 1 µM and was hybridised to four ssDNA templates representing four SNVs as described above, also at a concentration of 1 µM. Then, a mixture containing all four biotinylated SMART-Nucleobases (each at a final concentration of 20 µM) and the reducing agent NaBH₃CN (1 mM final concentration) was added to a final volume of 50 µL. The sample was incubated for two hours at 40°C and 13,400 rpm. Then 5 µL of pre-treated Q-Sepharose® Fast Flow (GE Healthcare, USA) was added. The pre-treatment of Q-Sepharose® Fast Flow consisted of centrifuging 100 µL of resin, discarding the supernatant and washing with 1 mL H₂O, followed by two washes with 10 mM phosphate buffer at pH 7 (1 mL each) by centrifugation at 13,400 rpm. The resin was then resuspended in 200 µL of 10 mM phosphate buffer at pH 7. The samples with the pre-treated Q-sepharose® Fast Flow were then incubated at 25 °C for 20 min with agitation at 1,400 rpm. After incubation, the reaction tube was centrifuged, the supernatant removed and the resin was washed three times with 3% aqueous acetonitrile by centrifugation at 13,400 rpm. Finally, the Qsepharose® resin was resuspended in 10 µL MALDI matrix (1:1 water:acetonitrile mixture) for MALDI-TOF analysis. Mass spectra were recorded on a Bruker Autoflex MALDI-TOF MS and acquired in positive ionisation reflector mode with a delay of 330 ns, 20 kV acceleration voltage and 200 shots.

4.8. Cell culture

The HuH-7 (hepatocellular carcinoma) (JCRB0403), HepG2 (hepatocellular carcinoma) (ATCC HB-8065), SKBR3 (breast adenocarcinoma) (ATCC HTB-30) and A549 (lung epithelial carcinoma) (ATCC CRM-CCL-185) cell lines were obtained from the cell bank of the Centre for Scientific Instrumentation, University of Granada. HuH-7, SKBR3 and A549 were grown in DMEM medium (Gibco, Paisley, UK), while HepG2 was grown in RPMI medium (Gibco, Paisley, UK). Both media were supplemented with 10% fetal bovine serum (Gibco, Paisley, UK), 100 U/mL penicillin/streptomycin (Gibco, Paisley, UK), 1× L-glutamine (Gibco, Paisley, UK) and 1 mM sodium pyruvate (Sigma Aldrich). Cell lines were grown at 37°C in a 5% CO₂ humidified incubator in T75 flasks to 80% confluence and trypsinised (1× trypsin-EDTA solution, Sigma Aldrich) at 37°C for 5 minutes. Then 10^6 cells were collected, centrifuged at 1500 rpm for 5 min and stored at -80°C prior to RNA extraction.

4.9. Analysis of miR-122 expression in tumour cell lines using the dual nanosystem and TaqMan probes by RT-qPCR

First, a calibration curve was generated using ssRNA-122, which represents the mature sequence of hsa-miR-122-5p, to compare miR-122 expression using both the dual nanosystem and the TaqMan assay (Thermo Scientific Inc., USA). We performed a series of dilutions in triplicate using amounts of ssRNA-122 of 1 ng, 0.1 ng, 0.01 ng, 0.001 ng, 10⁻⁴ ng, 10⁻⁵ ng, 10⁻⁶ ng, 10⁻⁷ ng and 10⁻⁸ ng, corresponding to 8×10¹⁰, 8×10⁹, 8×10⁸, 8×10^7 , 8×10^6 , 8×10^5 , 8×10^4 , 8×10^3 and 8×10^2 copies of ssRNA-122. RNA was then reverse transcribed using the TaqMan MicroRNA Reverse Transcription Kit (Thermo Scientific Inc., USA). Triplicate miRNA expression analyses were performed using the TaqMan Fast Advanced Master Mix (Thermo Scientific Inc., USA) according to the manufacturer's recommendations on a QuantStudio 6 Flex Real-Time PCR System (Applied Biosystems, UK). The TaqMan probe used was hsa-miR-122 (ID 002245) (Thermo Scientific Inc., USA). The curves were generated by plotting the log10 number of miR-122 copies as input against the cycle threshold (Ct) for RT-qPCR and against the number of Cy5+/Cy3+ events recorded in FACSVerse for the dual nanosystem. After establishing both calibration curves, the analysis of miR-122 expression was performed by extracting RNA from triplicate cell pellets containing 10⁶ cells each from the HuH-7, HepG2, SKBR3 and A549 tumour cell lines using the miRNeasy Mini Kit (Qiagen Inc., USA). The extracted RNA was then reverse transcribed using the TaqMan MicroRNA Reverse Transcription Kit. Triplicate miRNA expression analyses were performed using TaqMan Fast Advanced Master Mix according to the manufacturer's the recommendations on a QuantStudio 6 Flex Real-Time PCR System (Thermo Scientific). The TaqMan probes used were hsa-miR-122 (ID 002245) with RNU44 as the normalisation gene (ID 001094) (Thermo Scientific Inc., USA). Next, 20 µL of RT-qPCR product was denatured at 94°C for 10 minutes and then cooled on ice for two minutes to allow the strands to remain unbound. The product was then subjected to the dual nanosystem in a final volume of 100 µL in 2× SSC buffer containing 0.1% Tween 20 and analysed by FACSVerse under the conditions described in section 2.6.

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Author contribution

ARR: Conceptualization, methodology, investigation, formal analysis, data curation, writing – original draft of the paper.

IMJ: Conceptualization, methodology, investigation, formal analysis, data curation, review & editing MT: Conceptualization, methodology, investigation

AAG: Methodology, investigation

JALR: Methodology, investigation

MVCC: Methodology (protocols for PS-NPs synthesis)

FJLD: Methodology (synthesis and characterisation of SMART-Nucleobases and modified PNA monomers)

JJGM: Methodology (synthesis and characterisation of abasic PNA probe)

SP: Methodology (design of abasic PNA probes)

JJDM: Conceptualization, writing - review & editing, supervision, project administration, funding **RMSM**: Supervision, project administration, funding

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