

1 Ice templating water-stable macroporous  
2 polysaccharide hydrogels to mimic plant stems

3

4 *Katsuya KOMIYAMA*<sup>1</sup>, *Maya ALLARD*<sup>1</sup>, *Corentin ESCHENBRENNER*<sup>1</sup>, *Clémence SICARD*<sup>2,3</sup>,

5 *Ahmed HAMRAOUI*<sup>1,4</sup>, *Francisco M. FERNANDES*<sup>1\*</sup>

6

7 <sup>1</sup> Sorbonne Université, UMR 7574, Laboratoire de Chimie de la Matière Condensée de Paris, 75005,

8 Paris, France

9 <sup>2</sup> Université de Versailles Saint-Quentin-en Yvelines, UMR 8180, L'Institut Lavoisier de Versailles,

10 78035, Versailles, France

11 <sup>3</sup> Institut Universitaire de France, Paris

12 <sup>4</sup> Université Paris Cité, CNRS, UMR8003, Saints Pères Paris Institute for the Neurosciences, 45, rue

13 des Saints-Pères, 75006 Paris, France

14

15 **Keywords;** alginate, cellulose nanocrystals (CNC), macroporous hydrogel, ice-  
16 templating, capillary liquid transport

17 **Abstract**

18 Water-stable macroporous hydrogels, inspired by the structural and chemical  
19 characteristics of plant stems are expected to open a wide range of possibilities in soft  
20 materials for passive liquid transport. However, obtaining efficient materials for these  
21 applications still poses a major challenge due to the complexity of shaping hydrogels at  
22 the relevant scale-length. Here, water-stable macroporous hydrogels were fabricated  
23 using alginate and TEMPO-oxidized cellulose via a new approach involving ice

24 templating and topotactic ion-crosslinking with  $\text{Ca}^{2+}$ . This approach allows to fully avoid  
25 the energy-intensive lyophilization process and results in composite hydrogels with pore  
26 sizes akin to those found in celery xylem, a model we chose for plant stems. Importantly,  
27 the pore size could be tailored by adjusting both the ice-growth velocities and the ratios  
28 of alginate to oxidized cellulose. The resulting hydrogels displayed remarkable water  
29 stability along with viscoelastic properties and wettability that depend on the alginate and  
30 oxidized cellulose ratios. Mechanical properties, such as compression stress and  
31 toughness, consistently increased with higher alginate contents. In addition, liquid  
32 transport measurements on crosslinked hydrogels with varying compositions and ice  
33 growth velocities revealed comparable rising speeds to those observed in celery,  
34 confirming the ability of polysaccharide-based hydrogels obtained by ice templating and  
35 topotactic crosslinking as relevant materials to mimic the function of plant stems.

36

## 37 **1. Introduction**

38 In Nature, porous structures play a central role in large array of living organisms [1–4].  
39 Some of the most striking examples come from plant stems, which feature highly  
40 sophisticated porous architectures with a high degree of co-alignment. These porous  
41 structures constitute the plants' vascular systems—the xylem and the phloem—that are  
42 responsible for the capillary liquid transport of water and sap, respectively. Beyond the  
43 fundamental understanding of liquid transport in natural materials, plants' vascular  
44 systems are a major source of inspiration for a myriad of technological applications. In  
45 particular, because of the role of the xylem network in plants, the capacity to mimic its  
46 structure, its composition and its function is of technological interest in applications  
47 where water transport regulation is required. In the literature, mimicking the xylem

48 network of plants has led to hydrogels with oriented porosity relevant in a broad range of  
49 fields such as tissue engineering [5,6] and drug delivery [7,8]. Numerous fabrication  
50 approaches such as micropatterning [9,10], 3D printing [11,12], oriented shear flow  
51 [13,14], gravity-induced flow [15], electric field [16], and magnetic field [17] have been  
52 proposed to obtain porous anisotropic hydrogels, but these rely on expensive equipment  
53 and are applicable only to specific hydrogel compositions.

54 Recently, ice-templating (also known as freeze-casting or directional freezing) has gained  
55 traction for its ability to create hydrogels with hierarchically aligned well-defined pores  
56 in a straightforward and inexpensive process [18]. The technique relies on imposing a  
57 controlled temperature gradient on a solution or suspension to induce solvent freezing  
58 along a specific direction. Solutes, because they are mostly insoluble in ice [19,20], are  
59 excluded from the ice fraction and accumulate together with any particle in suspension in  
60 the interstitial space formed in between ice crystals. Upon removal of the ice crystals, the  
61 process enables the formation of oriented porous materials whose characteristic size can  
62 be adjusted by controlling the ice growth velocity. Here, we have implemented this  
63 technique to elaborate materials featuring macroporous anisotropic features that mimic  
64 the xylem network in plant stems.

65 Polysaccharides, mainly cellulose and hemicellulose, dominate the chemical composition  
66 of plants and are of great interest due to their low toxicity, high biocompatibility, low cost  
67 and high abundance. In this regard, mimicking plant structures using polysaccharides  
68 exclusively would be an important step to design hydrogels that go beyond the structural  
69 features of plant stems. However, only few reports have described the formation of water-  
70 stable polysaccharide-based materials with ordered macroporous structure [21–23]. Such  
71 limited examples are due to the abundant hydroxyl groups on the backbone of

72 polysaccharide chains. Most polysaccharides are either soluble in water (*eg.* chitosan,  
73 alginate, starch, among others) or readily dispersible in aqueous environment (*eg.*  
74 cellulose). This affinity towards water has dramatically reduced their potential use in the  
75 context of materials for healthcare or environmental applications, where humid  
76 environments prevail. To prevent these shortcomings, we have focused on two  
77 polysaccharides that can be stabilized using a similar crosslinking strategy; alginate and  
78 oxidized cellulose. Alginate is extracted from a family of brown algae. It is a linear,  
79 unbranched polysaccharide consisting of 1,4-linked  $\beta$ -D-mannuronic acid and an  $\alpha$ -L-  
80 guluronic acid. In presence of multivalent cations such as calcium—among others—ionic  
81 crosslinking occurs, resulting in the formation of a hydrogel stabilized by “egg-box”  
82 structures (Figure S1) [24]. Cellulose is composed of  $\beta$ -1-4-linked D-anhydroglucose  
83 units and is commonly extracted from wood, hemp, cotton, etc. The reaction between  
84 cellulose and 2,2,6,6-tetramethylpiperidine-1-oxyl radical (TEMPO) results in the  
85 selective oxidation of the hydroxyl groups at the C<sub>6</sub> position on the cellulose surface and  
86 induces the formation of carboxylate groups [25] (Figure S2). As with alginate,  
87 interaction of the carboxylate groups of cellulose and cations results in stable hydrogels  
88 [26,27]. These interactions stand as a key advantage to stabilize multicomponent  
89 hydrogels in a single step, leading to increases stability in comparison to single  
90 component hydrogels, due to reinforcement effects [28–30]. However, to date this  
91 crosslinking method has never been applied for the design of water-stable ice-templated  
92 polysaccharide-based hydrogels without an intermediate step requiring the energy-  
93 intensive process of lyophilization. The main challenge lies in the need to remove the ice  
94 while promoting the stabilization of the freeze concentrated phase. Traditionally this is  
95 obtained by lyophilization—the sublimation of ice crystals to obtain a dry foam of solutes.

96 However, this approach fails in the case where the solutes are water-soluble. To  
97 circumvent this limitation—and thus the loss of the macroporous structure, herein, we  
98 replaced lyophilization by topotactic stabilization [36]. A strategy our team developed for  
99 compositions containing type I collagen, that allows transforming frozen monoliths of  
100 biopolymer solutions into macroporous hydrogels without a drying step.

101 We applied this strategy to dispersions of cellulose nanocrystals (CNC) in alginate  
102 solution, to mimic part of the complex architecture and composition of plants' stems. The  
103 materials generated by this approach were water-stable and could be designed with pores  
104 (50-100  $\mu\text{m}$  in diameter) that exhibit dimensional similarity to the xylem of celery (*Apium*  
105 *graveolens*). The performance of the alginate-CNC ice templated hydrogel as water  
106 transport devices were compared with decellularized celery. To untangle the impact of  
107 the polysaccharide composition on the morphology, mechanical and water transport  
108 properties, the ratio between alginate and oxidized cellulose in the precursor  
109 solution/suspension was varied to its widest range. Finally, we demonstrate that the  
110 capillary transport properties of alginate-oxidized cellulose hydrogels are mainly  
111 dominated by the pore size, suggesting their potential utility in biomedical and  
112 environmental applications with an easily tuned macroporosity.

113

## 114 **2. Material and Methods**

### 115 **2.1. Materials**

116 Sodium alginate and  $\text{CaCl}_2 \cdot 2\text{H}_2\text{O}$  were purchased from Sigma-Aldrich and used without  
117 further purification. Cellulose nanocrystals (CNC) were purchased from CelluForce  
118 (Canada) and oxidized through TEMPO (2,2,6,6-tetramethylpiperidine-1-oxy radical)-  
119 mediated oxidation to obtain oxidized cellulose [31]. Briefly, cellulose nanocrystals (10

120 g) were suspended in water (1 L) containing TEMPO (0.156 g) and NaBr (2.572 g). A  
121 solution of NaClO (12 wt%) was added to the suspension under stirring and the mixture  
122 was kept at pH = 10 by adding 0.5 M NaOH. The reaction was quenched by adding  
123 ethanol (1 mL) and the pH of the mixture was lowered to 7 by adding 0.1 M HCl solution.  
124 The mixture was dialyzed for 7 days (Spectra/Por<sup>®</sup> 4, SpectrumLabs). Finally, the  
125 suspension was lyophilized to obtain dry oxidized cellulose powder. The carboxylate  
126 content of oxidized cellulose was 1.01 mmol/g based on electrical conductivity titration.

## 127 **2.2. Plant stem decellularization**

128 Celery (*Apium graveolens*) were purchased at a local supermarket (Paris, France).  
129 Decellularization of the celery stem was conducted according to the method reported by  
130 Esmaeili et al. [32] (Figure S3). The stem was cut into 1 cm thick transversal sections,  
131 immersed in 10% SDS solution, and placed in an orbital shaker at 180 rpm at 25 °C for 5  
132 days. After decellularization, samples were washed with distilled water several times and  
133 immersed in the solution containing 5 w/v% NaOCl and 3 w/v% NaOH at 25 °C for 1  
134 day. Finally, samples were washed with distilled water several times and stored at 4°C  
135 until further use.

## 136 **2.3. Fabrication of ion-crosslinked anisotropic hydrogels**

137 Macroporous hydrogels consisting of alginate and oxidized cellulose were prepared by  
138 unidirectional ice-templating method followed by crosslinking with Ca<sup>2+</sup> (Scheme 1).  
139 The ice-templating setup was composed of a cold finger—a heat conductive aluminum  
140 rod partially immersed in liquid nitrogen. Temperature profiles at the top of the cold  
141 finger were controlled via a heating resistance controlled by a Proportional–integral–  
142 derivative (PID) programmed to ensure a linear progression of the ice front [33].  
143 Alginate-oxidized cellulose relative concentration were set to 7 different ratios with a

144 fixed total solute concentration of 40 g/L (A:C=8:0, 7:1, 6:2, 4:4, 2:6, 1:7 and 0:8, where  
145 A and C stand for alginate and oxidized cellulose, respectively) The ratios are shown in  
146 Table 1.

147

148 **Table 1.** Composition of the macroporous polysaccharide samples.

<b>Alginate:Oxidized Cellulose (A:C)</b>	<b>Alginate / g L<sup>-1</sup></b>	<b>Oxidized Cellulose / g L<sup>-1</sup></b>
8:0	40	0
7:1	35	5
6:2	30	10
4:4	20	20
2:6	10	30
1:7	5	35
0:8	0	40

149

150 For each sample, 2 mL of the suspension were poured inside 12 mm diameter cylindrical  
151 molds, placed at the top of the aluminum rod. The bottom of the suspension in the mold  
152 was then cooled down from 20 to -80 °C. To explore the impact of the composition on  
153 the properties of the obtained hydrogels we have fixed the ice front velocity at 25 μm/s.  
154 Conversely, to assess the impact of the ice front velocity on the properties of the hydrogels,  
155 we fixed the alginate/oxidized cellulose ratio (A:C=4:4) and applied three different ice-  
156 front velocities (10 μm/s, 25 μm/s and 50 μm/s) (Figure S4).

157 After ice templating, all obtained suspensions were crosslinked in 1 M CaCl<sub>2</sub> solution for  
158 24 hours. To ensure that topotactic crosslinking (melting of the ice crystals with  
159 preservation of the porous structure) took place, samples were placed at -3 °C, above the

160 melting point of CaCl<sub>2</sub> solution but below the melting point of pure ice, resulting in self-  
161 supported crosslinked hydrogels that do not disperse in the CaCl<sub>2</sub> solution [34].

#### 162 **2.4. Morphology of the hydrogels**

163 The hydrogels and the stem of the celery were observed using SEM (S-3400N, Hitachi,  
164 Japan) at an accelerating voltage of 10 kV. All samples were coated with a 10 nm layer  
165 of gold before observation. After the Ca<sup>2+</sup> crosslinking, the hydrogels were dehydrated in  
166 successive ethanol baths (30, 50, 70, 80, 90, 95 and 100%) followed by supercritical CO<sub>2</sub>  
167 drying. When plunged into the ethanol bath, sample A:C=0:8 was rapidly dispersed,  
168 preventing its observation by SEM. Images acquired using SEM for the rest of the  
169 samples were analyzed with the MorpholibJ plugin [35] in FIJI software [36] to  
170 investigate the pore size and distribution. Over 100 pores were counted per SEM image  
171 to provide statistically representative values for the pore cross-section areas.

#### 172 **2.5. Rheological characterization**

173 The viscosity of the precursor suspensions with different alginate/oxidized cellulose  
174 ratios before crosslinking were determined using a rheometer (MCR 302, Anton Paar,  
175 Austria). A 25 mm diameter cone-plate geometry with 1° angle was used. The viscosity  
176 measurement was conducted by applying a growing shear-rate from 1 to 500 s<sup>-1</sup> at 25 °C.  
177 The rheological measurements of the different precursor suspensions were carried out  
178 after crosslinking with Ca<sup>2+</sup> ions, using a MCR302 rheometer under a parallel-plate  
179 configuration (diameter of 25 mm). The suspensions (1 mL) were introduced onto the  
180 bottom plate and crosslinked with 1 mL of 1 M CaCl<sub>2</sub> solution 5 minutes before loading  
181 the top plate. The frequency sweep was performed from 0.1 to 10 Hz with 1% amplitude  
182 at 25 °C.



183 **2.6. Water stability test of ion-crosslinked hydrogels**

184 Water stability tests were carried out on all Ca<sup>2+</sup>-crosslinked hydrogels, from pure  
185 alginate to pure oxidized cellulose. Each hydrogel was immersed in 20 mL of distilled  
186 water and stored for 30 days at room temperature. The stability was assessed visually by  
187 the sample deformation after this period.

188 **2.7. Mechanical properties of hydrogels**

189 Compression tests of the crosslinked hydrogels were carried out using a rheometer in  
190 compression mode (MCR 302, Anton Paar, Austria). The compression speed was set to  
191 1 mm/min and samples were compressed until 60% strain. Samples' dimensions were  
192 about 12 mm in diameter and 10 mm in height. A total of 5 replicates were averaged for  
193 each sample. Young's modulus was defined from the maximum slope in the low strain  
194 regime (0 to 10%). Toughness was determined by the area under the stress-strain curves  
195 until 60% stain.

196 **2.8. Wettability**

197 To characterize the wettability of the different crosslinked hydrogels, films with different  
198 ratios of alginate and oxidized cellulose were prepared by casting the suspensions on  
199 optical microscopy glass slides, with fixed height of 2 mm, using a doctor blade knife.  
200 Subsequently, cast suspensions were crosslinked by dipping the slides into 1 M CaCl<sub>2</sub>  
201 solution at room temperature. The deposited films were peeled off the glass slides with  
202 the exception of A:C=1:7 and 0:8 samples, which adhered strongly to the surface of the  
203 glass slides and could not be removed. The contact angle formed between the film and  
204 water was determined by assessing the interfacial force using the Wilhelmy plate method  
205 [34]. During the measurement, a film was suspended from the sample holder, which was  
206 connected to an automated microbalance, and partially immersed in distilled water

207 (Figure S5a). Samples were then vertically pulled from, and then pushed into the water at  
208 room temperature at a constant speed rate of 0.05 mm/s (Figure S5b) which results in  
209 both receding and advancing contact angles, respectively. The dimensions of the films  
210 were  $10 \times 5 \times 0.05 \text{ mm}^3$ . The contact angles were determined in degrees using the following  
211 relation:

$$212 \quad \theta = \cos^{-1} \frac{F_w}{L\sigma} \quad (1)$$

213 where  $\sigma$  is the surface tension of water ( $\text{mN} \cdot \text{m}^{-1}$ ),  $F_w$  is the wetting force (mN),  $L$  is the  
214 length of the triple phase line (defined by the film, the air and the water around the sample  
215 section) (m) and  $\theta$  is the contact angle ( $^\circ$ ).

## 216 **2.9. Liquid transport**

217 Crosslinked hydrogels with different compositions/ice-growth velocities were used for  
218 the liquid transport measurements. Samples were fixed with 2 needles onto a home-built  
219 sample holder brought to contact with a 200 ppm methylene blue (MB) solution (lifted  
220 progressively by a lab jack until the liquid surface reached the bottom of the sample)  
221 (Figure S6a). The progression of the methylene blue in the hydrogels was recorded with  
222 video camera (Q-scope QS.20200-P) for 1 hour (Figure S6b) at 16 frames per second.  
223 The obtained video footage was analyzed with FIJI software. The surface tension of the  
224 methylene blue solution used here was  $65 \text{ mN/m}$  [37]. A control experiment was  
225 performed using single hydrogel walls (prepared as described above by doctor blade  
226 casting followed by crosslinking for three different compositions, 2:6, 4:4 and 6:2 A:C).  
227 The movement of the dye was monitored as outlined earlier.

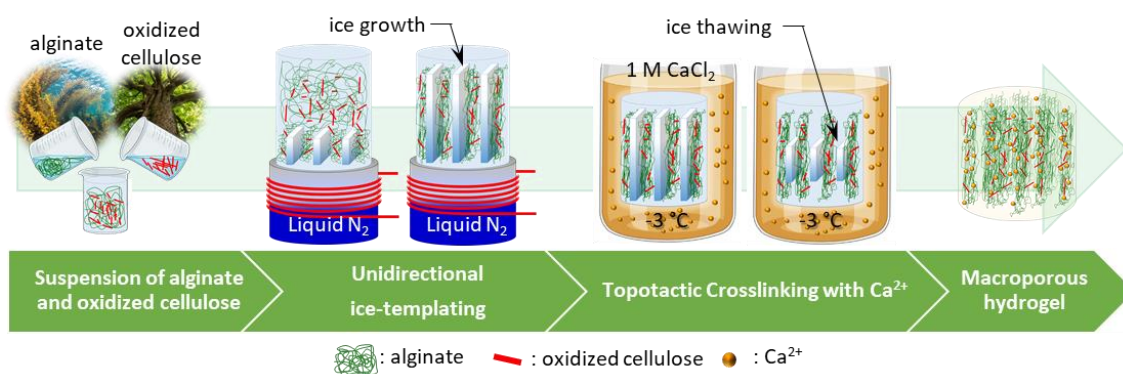
## 228 **3. Results and discussion**

### 229 **3.1. Macroporous alginate-CNC gels obtained by ice templating and topotactic**

230 **crosslinking**

231 Ice templating exploits the poor solubility of most solutes in ice, resulting in the formation  
232 of two different phases during freezing. One phase is composed of pure ice, and the  
233 second corresponds to freeze-concentrated solutes in between the ice crystals. To remove  
234 the ice without altering the macroporous structure, we implemented a topotactic  
235 stabilization strategy [38]. This technique relies on the concomitant occurrence of ice  
236 thawing and polymer crosslinking. Here, we have selected  $\text{CaCl}_2$  at a concentration of 1  
237 M to induce crosslinking of the alginate-CNC system (Scheme 1).

238



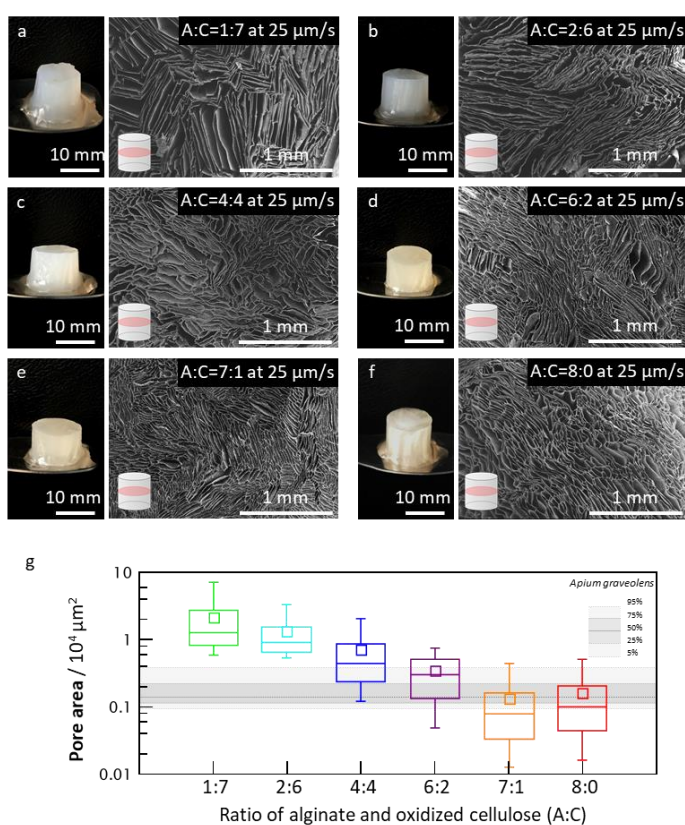
239

240 **Scheme 1.** Schematic illustration of the fabrication process of macroporous anisotropic hydrogels  
241 consisting of alginate and oxidized cellulose.

242

243 Alginate and oxidized cellulose are crosslinked when exposed to  $\text{Ca}^{2+}$  ions, leading to the  
244 formation of gels. In addition, the presence of  $\text{CaCl}_2$  at this concentration induces a strong  
245 cryoscopic depression (*ca.*  $-5^\circ\text{C}$ ). Together, these conditions ensure that, when a frozen  
246 monolith is placed in a  $\text{CaCl}_2$  solution, at a temperature between  $0$  and  $-5^\circ\text{C}$ , the sample  
247 can be progressively transformed into an unfrozen crosslinked hydrogel. We have applied  
248 this strategy to the elaboration of macroporous alginate-CNC materials ranging from pure  
249 alginate to pure CNC. Regardless of the composition, the resulting materials are fully

250 self-supported, as can be seen in the left hand side images in Figure 1a-f. The longitudinal  
251 sections of the samples, depicted in Figure S7 confirm the pores run parallel to the  
252 temperature gradient applied during freezing, regardless of the studied compositions.  
253 Notably, pure CNC hydrogel (A:C 0:8) was found unstable in ethanol solution impeding  
254 its observation under SEM. While the changes in composition do not affect the  
255 macroscopic stability nor the orientation of pores of the obtained hydrogels, SEM  
256 observations of the transversal sections of these samples (Figure 1a-f) indicate that the  
257 polysaccharide composition does play a major role in determining the pores' dimensions  
258 and morphology.  
259



260

261 **Figure 1.** Pictures and SEM images of  $\text{Ca}^{2+}$ -crosslinked macroporous hydrogels prepared  
262 at  $25 \mu\text{m/s}$  (ice growth velocity) using different ratios of alginate and oxidized cellulose.  
263 (a) A:C=8:0, (b) A:C=7:1, (c) A:C=6:2, (d) A:C=4:4, (e) A:C=2:6 and (f) A:C=1:7. (g)

264 Summary of the pore area distribution of alginate and oxidized cellulose macroporous  
265 hydrogels at different compositions for 25  $\mu\text{m/s}$  (ice growth velocity). Moustaches delimit  
266 the 5 and 95 percentiles of the distribution and box limits represent the 1<sup>st</sup> and 3<sup>rd</sup> quartiles.  
267 The rectangles and horizontal lines in the boxes represent mean and median values,  
268 respectively. Gray horizontal bars depict the pore area distribution of *A. graveolens* xylem  
269 vascular system.

270

271

272 Figure 1g depicts the pore area distribution (taken from the area of the pore in the  
273 transversal cross-section). Samples exclusively composed of alginate (A:C=8:0) display  
274 anisotropic pore section that tend to pack together producing co-alignment (Figure 1a).  
275 Increasing the oxidized cellulose content produces larger pores (Figure 1g). The increase  
276 in pore dimensions, resulting from increasing CNC content, also results in wider pore size  
277 distribution (Figure S8a). In other words, alginate favors smaller and more homogeneous  
278 pores with narrower size distribution, whereas CNC promotes bigger, more polydisperse  
279 pores.

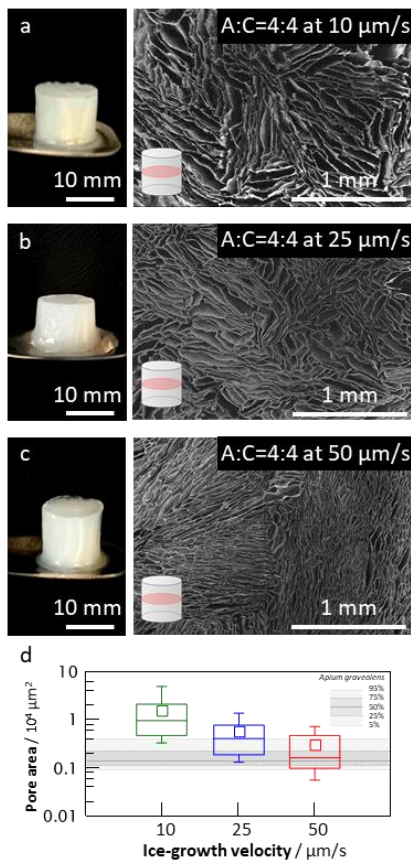
280 One of the key factors affecting the growth of ice crystals during ice-templating (and thus  
281 determining the final dimensions of the pores in the final materials) is the viscosity of the  
282 precursor solution/suspension. We investigated the viscosity of the different compositions  
283 of alginate and oxidized cellulose to ascertain their impact on the pore size of mixed  
284 polysaccharide hydrogels (Figure S9). The viscosity of the suspensions progressively  
285 increased with the ratio of alginate, regardless of the shear rate. This could be associated  
286 with the intrinsically low viscosity of oxidized cellulose nanocrystal rods and the  
287 relatively high viscosity of entangled alginate chains. In addition, the viscosity of all  
288 suspensions showed shear-thinning behavior, which was more pronounced for higher  
289 ratios of alginate. This effect could be ascribed to the disentanglement of alginate chain

290 coils under shear [39], even if strong shear thinning effects have equally been reported  
291 for CNCs [40].

292 The viscosity values determined for the different aqueous suspensions of polysaccharides  
293 display an inverse relationship with the pore size. This observation confirms the strong  
294 dependence between porosity and viscosity widely discussed in the literature for other  
295 compositions [41]. Here, high alginate fractions impose higher viscosity to the  
296 polysaccharide solutions/suspension, resulting in restricted lateral growth of ice crystals  
297 and consequently smaller and more uniform pore size for the same ice front velocity [42].  
298 However, ascribing the differences in pore size exclusively to the viscosity implies that  
299 the different polysaccharides do not have specific interactions with ice during the freezing  
300 events.

301 SEM images in the transversal section of the hydrogels prepared at 4:4 ratio of alginate  
302 and oxidized cellulose with different ice-growth velocities (including 10, 25, and 50  
303  $\mu\text{m/s}$ ) are shown in Figure 2a to 2c (Figure S10 shows the longitudinal section of those  
304 hydrogels). Faster ice-growth velocities induced the formation of smaller pores as  
305 reported earlier for other polysaccharides [43]. At 50  $\mu\text{m/s}$ , the ice front velocity yielded  
306 pore surface areas of approximately  $2.5 \times 10^3 \mu\text{m}^2$  (Figure 2c), 16% of the value found for  
307 10  $\mu\text{m/s}$  ( $\approx 1.6 \times 10^4 \mu\text{m}^2$ , Figure 2a). This effect is due to the creation of more ice  
308 nucleation sites on the bottom of the samples as the ice growth velocity increased, leading  
309 to smaller macropores [44]. Overall, we found out that the pore size and their respective  
310 distributions can be tuned by modulating the alginate/oxidized cellulose relative  
311 composition (Figure 1g and Figure S8a), but also by the ice-growth velocities (Figure 2d  
312 and Figure S8b). These values (especially those of A:C=6:2 at 25  $\mu\text{m/s}$  and A:C=4:4 at  
313 50  $\mu\text{m/s}$ ) are comparable to those measured for the xylem of native celery stems

314 ( $\approx 1.9 \times 10^3 \mu\text{m}^2$ ). In other words, hydrogels reported here, prepared by ice-templating  
315 followed by ion-crosslinking, mimic the unidirectional orientation found in plant stems  
316 as well as their characteristic dimensions. It is important to note that the biomimetic  
317 features of these materials concern not only their structural features, but also their  
318 composition, a mixture of polysaccharides close to those found in native plant tissues  
319 [45–47].  
320



321  
322 **Figure 2.** Pictures and SEM images of  $\text{Ca}^{2+}$ -crosslinked hydrogels prepared at 4:4 ratio  
323 of alginate and oxidized cellulose at different ice front velocities. (a) 10  $\mu\text{m/s}$ , (b) 25  $\mu\text{m/s}$   
324 and (c) 50  $\mu\text{m/s}$ . (d) Summary of the pore area distribution of alginate and oxidized  
325 cellulose macroporous hydrogels at different ice front velocities. Moustaches delimit the  
326 5 and 95 percentiles of the distribution and box limits represent the 1st and 3rd quartiles.  
327 The rectangles and horizontal lines in the boxes represent mean and median values,  
328 respectively. Gray horizontal bars depict the pore area distribution of *A. graveolens* xylem



329 vascular system.

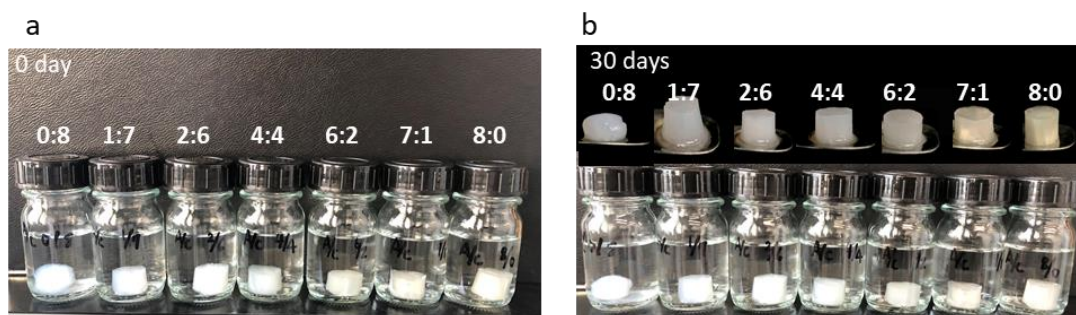
330

### 331 **3.2. Characterization of topotactic crosslinked hydrogels**

332 *Water stability.* The water stability of hydrogels is one of the most significant features for  
333 a variety of applications, including biomedical scaffolds, oil extraction/separation, and  
334 water purification/desalination [48,49]. To evaluate the contribution of the proportions of  
335 alginate and oxidized cellulose on the water stability, topotactic crosslinked hydrogels  
336 with 7 different compositions (prepared with an ice-front velocity of 25  $\mu\text{m/s}$ ) were  
337 immersed in distilled water (Figure 3a) and kept for 30 days at room temperature in static  
338 conditions (Figure 3b). At day 30, hydrogels A:C=0:8 were partially dispersed and  
339 swollen. On the contrary, all hydrogels containing alginate showed good water stability,  
340 suggesting higher alginate contents allow for a more stable crosslinking by calcium ions.  
341 These results correlate positively with the higher theoretical crosslinking density for  
342 sodium alginate (according to the supplier the carboxyl groups density equals to 5.05  
343  $\text{mmol g}^{-1}$  with a M/G ratio of 1.56, which amounts to *c.a.* 2.0  $\text{mmol g}^{-1}$  of G units) in  
344 comparison with that of oxidized cellulose (carboxyl groups density equal to 1.01  $\text{mmol}$   
345  $\text{g}^{-1}$ ). In general, polysaccharide materials prepared by ice templating redisperse readily in  
346 water unless cryogelation occurs [50] or postprocessing steps are added, such as photo-  
347 crosslinking or photo-polymerization. [51–56]. Here, we demonstrate that self-supported  
348 hydrogels with long term water stability can be achieved via ice-templating followed by  
349 ion crosslinking during thawing, without further stabilization by photo-polymerization or  
350 photo-crosslinking. Moreover, the components commonly used for the photo-induced  
351 gelation rely on particularly harmful components for the environment and are especially  
352 difficult to implement in complex, 3D geometries. Ice templating coupled to topotactic



353 stabilization eliminates these bottlenecks in a straightforward and non-toxic process.



354  
355 **Figure 3.** Photos of water stability tests of ion-crosslinked samples with the different ratio  
356 of alginate and oxidized cellulose (prepared with an ice growth velocity of 25  $\mu\text{m/s}$ ); (a)  
357 immediately after the immersion in the water, (b) 30 days after the immersion.

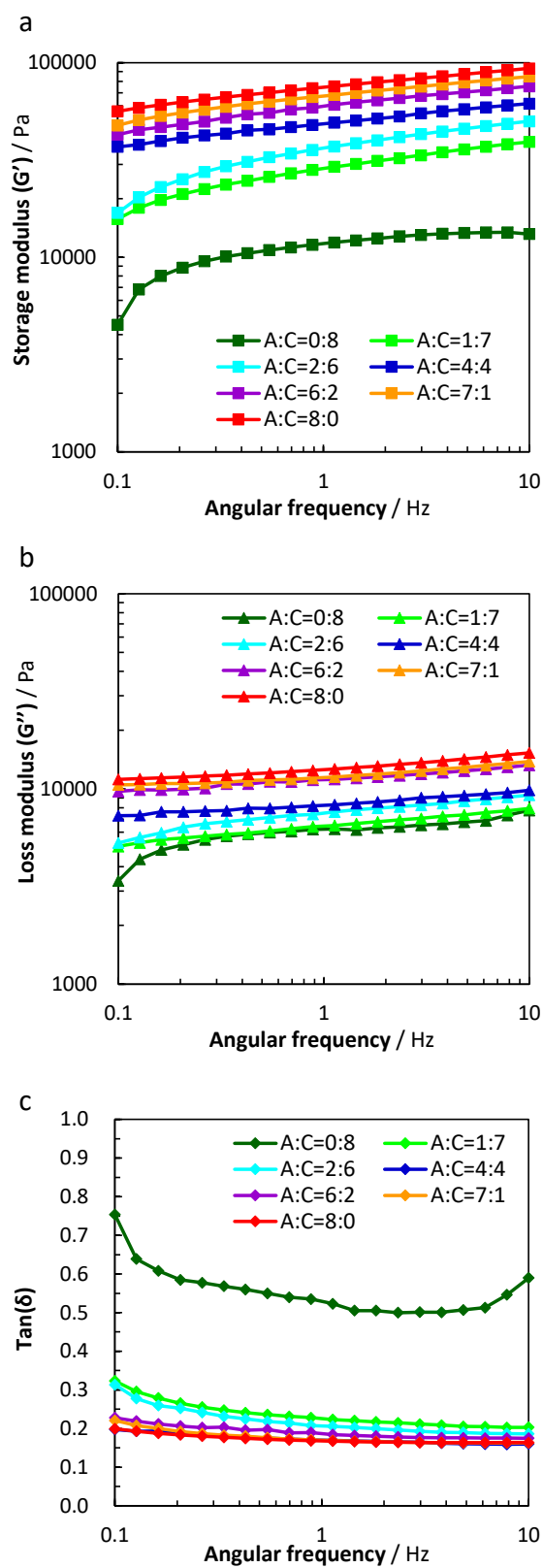
358

359 *Viscoelastic properties* . The viscoelastic properties of hydrogels determine, to a large  
360 extent, their applicability for a wide range of uses. To ascertain the viscoelastic properties  
361 of the macroporous hydrogels, frequency sweep measurements were carried out on  
362 crosslinked suspensions obtained through  $\text{Ca}^{2+}$ -crosslinking at different alginate/oxidized  
363 cellulose components. The storage modulus ( $G'$ ), loss modulus ( $G''$ ), and damping factor  
364 ( $\tan(\delta) = G''/G'$ ) as functions of frequency are shown in Figure 4a, b, and c. All the  
365 compositions of alginate/oxidized cellulose showed a gel-like behavior ( $G' > G''$ ) over  
366 the entire angular frequency range. The decrease of  $\tan(\delta)$  with alginate content suggests  
367 that in presence of  $\text{Ca}^{2+}$  ions, this polysaccharide promotes a more solid-like and stiffer  
368 internal network to the hydrogels, as previously seen for the water swelling experiments.

369 These observations are equally confirmed by the absolute values of  $G'$  and  $G''$ . Both  
370 values increase with the fraction of alginate, and in both, the values are mostly  
371 independent from the angular frequency.

372 The ratio between the two polysaccharides provides a tool to tailor the characteristic pore  
373 size and to modulate the crosslinking density inside the hydrogel and, as a consequence,

374 a lever to tune their viscoelastic properties.



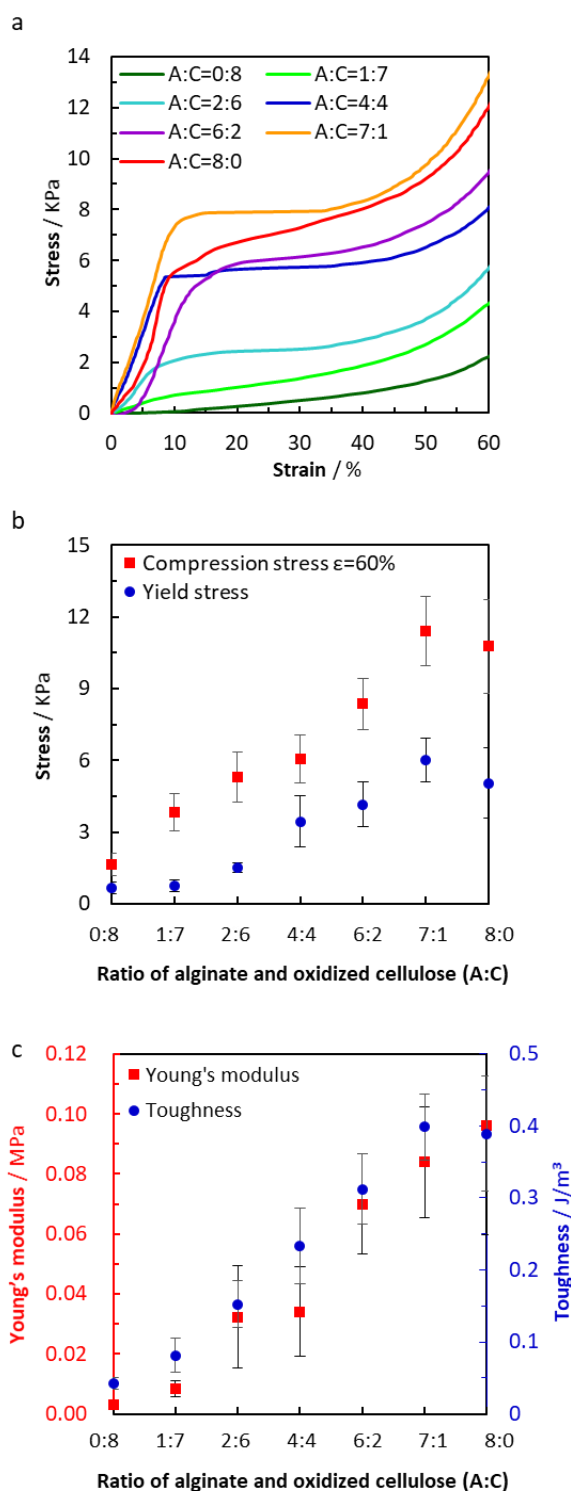
375

376 **Figure 4.** Viscoelastic properties of crosslinked gels with different compositions of  
377 alginate and oxidized cellulose (prepared with an ice growth velocity of 25  $\mu\text{m/s}$ ) (a)  
378 storage modulus, (b) loss modulus, and (c) damping factor.

379

380 *Mechanical properties.* To investigate the effects of the composition of alginate and  
381 cellulose on the hydrogels, compression tests were performed uniaxially along the  
382 freezing direction on macroporous hydrogels prepared from different ratios of  
383 alginate/oxidized cellulose with a constant ice growth velocity of 25  $\mu\text{m/s}$ . The resulting  
384 stress-strain curves are shown in Figure 5a, and their mechanical properties are described  
385 in Table S1. All stress-strain curves present an equivalent behavior, with an initial slope  
386 corresponding to an elastic deformation regime, followed by a yield point and a plateau,  
387 which evolves to reach a densification regime. The compression stress at 60% strain and  
388 the yield stress are summarized in Figure 5b, and the Young's modulus and toughness of  
389 the hydrogels are summed up in Figure 5c. All measured properties increased with  
390 increasing ratio of alginate, with exception for the A:C = 8:0 sample. The A:C=7:1 sample  
391 resulted in the highest compression stress, yield stress, and toughness. This optimum  
392 value is ascribed to the reinforcement of the alginate hydrogel matrix by low volume  
393 fractions of oxidized cellulose, which is likely to favor even dispersion of the filler. At  
394 higher volume fractions oxidized cellulose is expected to aggregate and entangle,  
395 providing a less effective reinforcement effect. At A:C=7:1 ratio, hydrogels featured an  
396 improvement in compression and yield stress up to 107% and 119%, respectively, in  
397 comparison to A:C=8:0. Taking into account that this material (A:C=7:1) has the smallest  
398 pore area distribution (Figure S8a), it is impossible to ascribe the enhancement of the  
399 mechanical properties exclusively to the composite nature of the hydrogels or the  
400 rheology of the suspensions, and the size and morphology of the pores should equally be

401 considered.



402

403 **Figure 5.** Compression test results of crosslinked hydrogels prepared with an ice growth

404 velocity of 25  $\mu\text{m/s}$  with the different ratios of alginate and oxidized cellulose. (a)

405 Compression strain-stress curves, (b) compression stress at 60% of strain and yield stress,

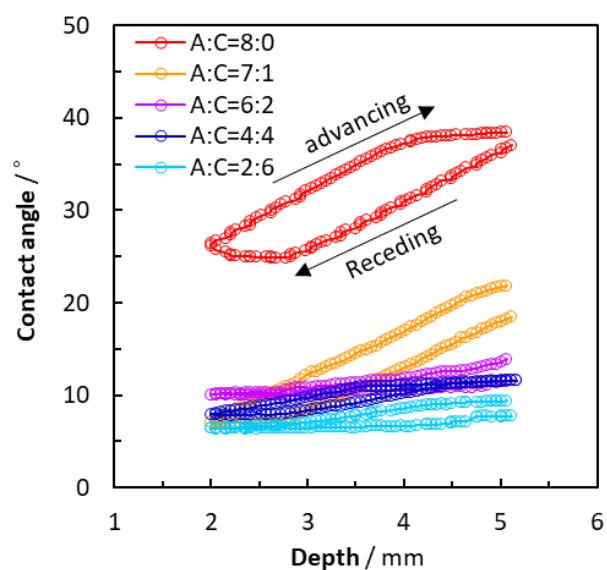
406 (c) Young's modulus and toughness.

407

### 408 3.3. Dynamic contact angle measurement

409 To assess the wettability dynamics of various hydrogel compositions, we measured the  
410 contact angles at the triphase line formed by the films deposited on glass slides, water,  
411 and air during dipping and retraction stages (Figure 6). At 38°, A:C=8:0 featured the  
412 highest advancing contact angle and it scaled monotonically with the oxidized cellulose  
413 contents, reaching 9° for A:C=2:6. This trend is in good agreement with the observations  
414 of Montrezor *et al.*, who measured the contact angle for non-crosslinked alginate and  
415 oxidized cellulose samples [57]. Although the geometric aspects of these films may differ  
416 from the walls inside the hydrogels prepared by ice-templating, their surface chemistry  
417 should be strictly comparable. In this sense, the values measured here provide valuable  
418 information to describe the wettability of hydrogels of different polysaccharide  
419 composition.

420



421

422 **Figure 6.** Hysteresis of the dynamic contact angle measurement with deposited films with

423 different ratios of alginate/oxidized cellulose.

424

#### 425 **3.4. Liquid transport measurement**

426 The previous sections have shown that it is possible to control pore size inside the  
427 macroporous polysaccharide hydrogels by tuning the ice-growth velocities or the  
428 alginate/oxidized cellulose ratio. Furthermore, the wettability measurements demonstrate  
429 the influence of composition on the water contact angle. Given the significant roles of  
430 pore size and wettability in water transport within biological structures, we have  
431 conducted measurements of this property in macroporous polysaccharide hydrogels  
432 fabricated through ice templating and topotactic crosslinking. Water transport within  
433 cross-linked hydrogels obtained at different ice-growth velocities (10, 25, and 50  $\mu\text{m/s}$ )  
434 and different ratios of alginate/oxidized cellulose was measured and compared to the  
435 water transport properties found for decellularized stem of celery. To ensure that the  
436 experimental setup accurately measured the transport of liquid within the pores, rather  
437 than the diffusion of dye through the pore walls, a control experiment was conducted.  
438 This involved exposing single polysaccharide walls to the dye (methylene blue, MB)  
439 under the same conditions (Figure S11). As no measurable diffusion of the dye in the pore  
440 walls was detected within the relevant time frame (60 minutes), we confirmed that all  
441 observations of dye progression in the hydrogels corresponded to liquid transport inside  
442 the pores.

443 Compositions A:C=6:2, 4:4, and 2:6 were chosen as they reproduce more accurately the  
444 global fraction of cellulose in plant stems (approximately 30-80% cellulose) [58,59].  
445 Images of liquid transport inside hydrogels—prepared at different ice-growth  
446 velocities—up to 60 minutes are shown in Figure 7a and b, respectively. Plotting the

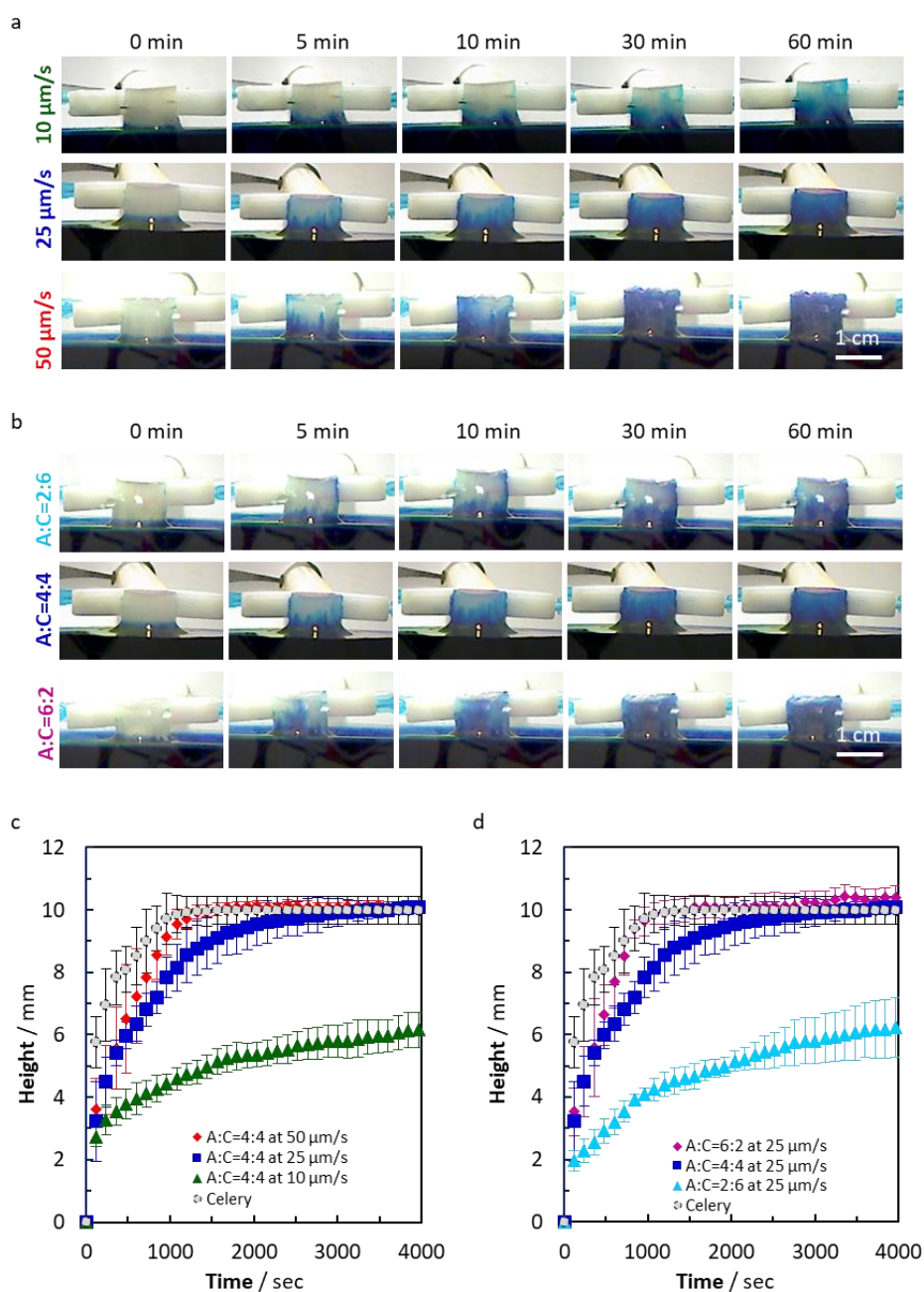
447 curves of rising height of liquid versus time (Figure 7c and d for different ice-growth  
448 velocities and ratios, respectively) shows that the ascending speed through anisotropic  
449 hydrogels is faster in the initial stages followed by a slower regime. For a given  
450 composition, the rising speed of liquid within the hydrogels prepared at 50  $\mu\text{m/s}$  was the  
451 highest and it decreased consistently for samples prepared at slower ice-growth velocities.  
452 This observation underscores the significant influence of ice front velocity, and  
453 consequently pore size variation, on regulating the liquid transport velocities of the  
454 resultant hydrogels, despite their identical compositions.

455 For hydrogels with different ratios of alginate/oxidized cellulose, the elapsed time before  
456 the liquid reached the top of the sample (height = 10 mm) varied with the composition.  
457 For sample A:C=6:2 the elapsed time was around 1440 s whereas for sample A:C=4:4  
458 the required time was as high as 3240 s. In addition, in contact with sample A:C=2:6, the  
459 liquid did not reach the top of the hydrogel within 60 mins. Although these findings align  
460 with the hydrogels' composition and, consequently, the samples' wettability. It is  
461 important to highlight that the characteristic contact angles fall within a narrow range,  
462 spanning from 9 to 14°. This limited variation hardly accounts for the significant  
463 differences observed in transport properties. On the contrary, the pore distribution in the  
464 same samples ranges from approximately  $3\text{-}16 \times 10^3 \mu\text{m}^2$ , suggesting this parameter plays  
465 a predominant role in liquid transport properties. Lower contact angle should translate to  
466 a higher capillary coefficient—and thus faster capillary water transport according to  
467 Lucas-Washburn equation [60,61]. However, our observations contradict this trend,  
468 reinforcing the predominant role of the pores' dimensions and the arrangement of pores  
469 in relation to each other in controlling the capillary transport within the macroporous  
470 hydrogels reported here.

471 Celery was used as a native plant tissue reference for comparing the capillary rising  
472 behavior of the prepared hydrogels. The decellularized and bleached celery allowed for  
473 the visualization of dye rising from the bottom to the top of the celery stem sample (Figure  
474 S12a). In living vascular plants, leaves facilitate transpiration. The resulting evaporation  
475 generates a vapor pressure depression which promotes capillary liquid transport through  
476 the plant stem. However, in this study, liquid was transported up the celery stem without  
477 leaves, reaching the top after around 1000 seconds (Figure 7c, d and Figure S12b).  
478 Although the celery's initial rising speed was much faster than the prepared hydrogels, it  
479 became comparable to hydrogels, especially for A:C=6:2 at 25  $\mu\text{m/s}$  and A:C=4:4 at 50  
480  $\mu\text{m/s}$ . In other words, the hydrogels prepared with alginate and oxidized cellulose via ice-  
481 templating in this study successfully mimic both the structural features of plant stems and  
482 their liquid transport behavior.

483 In summary, we successfully created bioinspired hydrogels through ice-templating/ion-  
484 crosslinking of alginate and oxidized cellulose suspensions. By adjusting precursor  
485 compositions and ice growth velocities, we could control mechanical, surface properties,  
486 and morphologies. The resulting hydrogels exhibit capillary water transport behavior  
487 primarily dependent on pore size and the alignment of pores in relation to each other.  
488 These findings and insights are valuable for developing bioinspired materials resembling  
489 native biological tissues, with aligned mechanical properties, for potential biomedical and  
490 environmental applications.





491

492 **Figure 7.** Liquid transport experiment with hydrogels prepared with different  
 493 compositions of alginate/oxidized cellulose and with different ice-growth velocities, as  
 494 comparison with celery. Optical photos showing capillary action behavior with the  
 495 hydrogel prepared at (a) different ice growth velocities (A:C = 4:4) and (b) with different  
 496 compositions of alginate and oxidized cellulose (ice growth velocity 25  $\mu\text{m/s}$ ). (c) Time-  
 497 liquid height curves with A:C = 4:4 at different ice-growth velocity. (d) Time-liquid height  
 498 curves with hydrogels obtained by different compositions of alginate and oxidized  
 499 cellulose with ice growth velocity of 25  $\mu\text{m/s}$ .

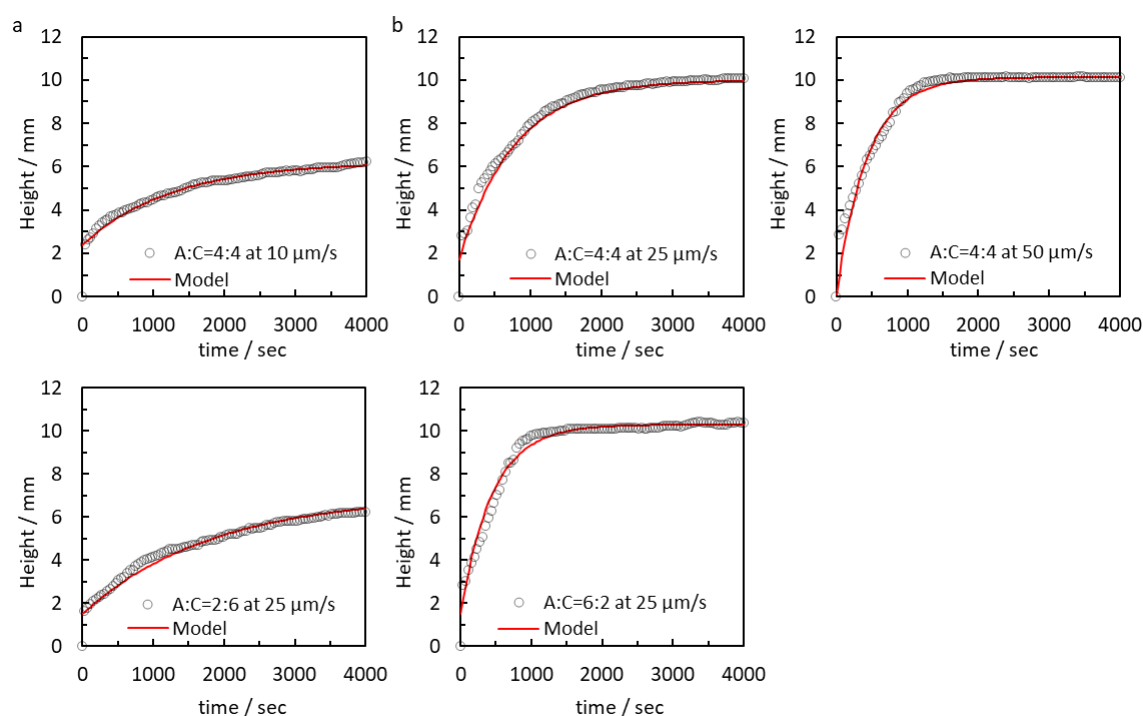
500

501 In general, porous media can be characterized by studying the kinetics of liquid rise within  
502 the pore spaces. Although porous media generally have a complex structure, they can be  
503 modeled as a single, vertical capillary or as an assembly of such capillaries. The main  
504 difficulties lie in separately estimating the effective mean radius of the capillaries and the  
505 contact angle between the liquid and the pore. In the characterization of porous media by  
506 capillary rise, the dynamic properties of the liquid front and any meniscus deformation or  
507 dynamic contact angle effects will have important consequences. Specifically, we  
508 consider that the contact angle between the liquid meniscus and the inner surface of the  
509 capillary becomes a dynamic contact angle when the liquid front is in movement as shown  
510 in the hysteresis study of the contact angle (Figure 6). It has previously been demonstrated  
511 that the resulting time dependence is due to frictional dissipation at the moving wetting  
512 front. In modeling the conducted experiments, we employ an analytical expression for  
513 height versus time, facilitating the determination of the retardation coefficient. This  
514 coefficient encompasses both diffusion and friction contributions to dissipation [56]. Here,  
515 we utilize the analytical equation established by Hamraoui *et al.* [57].

$$516 \quad h(t) = h_e + (h(0) - h_e) \exp \left[ -\frac{\gamma \cos(\theta_0)}{\beta_1 h_e} t \right], \quad (\text{E1})$$

517 where  $\beta_1$  is the slowdown coefficient,  $\theta_0$  is the equilibrium contact angle,  $\gamma$  surface  
518 tension of the used liquid,  $h(t = 0)$  and  $h_e = h(t \rightarrow \infty)$  are respectively the initial  
519 and the equilibrium heights. In this scenario, the fitting process required only  $\beta_1$  as a  
520 parameter, with the pore radius implicitly incorporated into  $h_e$ , which is determined  
521 experimentally. The experimental curve fits, presented in Figure 8, were carried out using  
522 the analytical expression given in equation (E1). Across all experimental curves,  
523 including sample prepared with different composition (A:C=2:6-6:2) of polysaccharide

524 and with different ice-growth velocities (at 10-50  $\mu\text{m/s}$ ), a consistent match with fitting  
525 model curves is observed. Table 2 gathers the retardation coefficients calculated for each  
526 sample. The retardation coefficients in sample A:C=2:6 at 25  $\mu\text{m/s}$  and A:C=4:4 at 10  
527  $\mu\text{m/s}$  are relatively lower ( $\beta_1 \approx 13$  and 17 for A:C=2:6 at 25  $\mu\text{m/s}$  and A:C=4:4 at 10  
528  $\mu\text{m/s}$  respectively), while those for A:C=6:2 at 25  $\mu\text{m/s}$  and A:C=4:4 at 50  $\mu\text{m/s}$  exhibited  
529 higher values ( $\beta_1 \approx 2.8$ ). This observation aligns well with the experimental data of the  
530 liquid height profile, emphasizing the pivotal role of pore size in the liquid transport  
531 behavior within the macroporous hydrogels.



532

533 **Figure 8.** The graphs illustrate the capillary water transport behavior within hydrogels,  
534 which were prepared with varying ice-growth velocities (a-c) and distinct compositions  
535 of alginate and oxidized cellulose (d and e), along with the theoretical fitting curves as  
536 defined by E1.

537

538 In the liquid transport behavior within the macroporous hydrogels, diffusion plays a  
539 crucial role in governing the initial stages of the liquid transport. This stage is guided by

540 the pressure gradients generated by the impulsive force, such as the wetting stress. Figure  
 541 S13a-e displays fitting curves on the experimental  $h(t)$  profiles at short times by using  
 542 diffusion equation  $h(t)^2 = 6Dt$ , where  $D$  denotes diffusion coefficient, and  $t$  denotes  
 543 time. The revealed values of diffusion coefficient highlight a trend where the hydrogels  
 544 with smaller pore size, such as A:C=4:4 at 10  $\mu\text{m/s}$  and A:C=6:2 at 25  $\mu\text{m/s}$ , yielded  
 545 higher diffusion coefficients. Figure S13f illustrates the findings, indicating an inverse  
 546 correlation between the diffusion coefficient and the retardant coefficients. Notably,  
 547 hydrogels with smaller pore sizes displayed lower retardation coefficients. These  
 548 variations in the diffusion coefficients among samples indicate that the contribution of  
 549 the friction at the triple phase line—defined by polysaccharide walls, air, and water—is  
 550 relatively equivalent for sample A:C=4:4 at 10  $\mu\text{m/s}$  and A:C=2:6 at 25  $\mu\text{m/s}$  but  
 551 considerably lower than that along a three-phase line of sample A:C=6:2 at 25  $\mu\text{m/s}$  and  
 552 A:C=4:4 at 50  $\mu\text{m/s}$ .

553 In summary, this study demonstrates the impact of the intricate correlation between pore  
 554 size, diffusion coefficients, and retardation coefficients on liquid transport within  
 555 macroporous hydrogels. It also highlights the central roles of diffusion as the driving force  
 556 for liquid movement within the pores and friction at the triphase line responsible for the  
 557 dynamic nature of the contact angle.

558

559 **Table 2.** Retardation coefficients and diffusion coefficients ( $D$ ) of samples prepared  
 560 with different ice-growth velocities/compositions of alginate and oxidized cellulose.

Sample	Retardation coefficient	$D$ ( $\text{mm}^2 \text{s}^{-2}$ )
A:C=4:4 at 10 $\mu\text{m/s}$	12.85	0.00072
A:C=4:4 at 25 $\mu\text{m/s}$	4.91	0.00600

A:C=4:4 at 50 $\mu\text{m/s}$	2.76	0.01457
A:C=2:6 at 25 $\mu\text{m/s}$	16.60	0.00103
A:C=6:2 at 25 $\mu\text{m/s}$	2.78	0.01630

---

561

## 562 **4. Conclusions**

563 Anisotropic macroporous hydrogels, inspired by the structural features of plant stems,  
564 were successfully fabricated using alginate and oxidized cellulose through ice-templating  
565 followed by topotactic ion-crosslinking with  $\text{Ca}^{2+}$ , a strategy previously developed in our  
566 team to stabilize protein-based biomaterials. The resulting ionic crosslinking rendered the  
567 hydrogels insoluble in water. By adjusting the overall amounts of alginate and oxidized  
568 cellulose, tunable viscoelastic properties and wettability were achieved, aligning with the  
569 respective compositions of alginate and oxidized cellulose. Remarkably, introducing a  
570 minimal quantity of oxidized cellulose in the crosslinked hydrogels effectively reinforced  
571 the alginate matrix, leading to the highest mechanical properties. Moreover, the  
572 morphological characteristics of the hydrogels were tunable, influenced not only by the  
573 ice growth speed but also by the composition. These levers allowed to obtain pore sizes  
574 comparable with those found in the xylem of celery and, more importantly, to reproduce  
575 the plant stems' liquid transport behavior. In fact, capillary liquid transport experiments  
576 demonstrated that crosslinked anisotropic hydrogels with smaller pore sizes exhibited  
577 faster liquid rising speeds, comparable to those observed in celery. These findings  
578 highlight the potential applications of these hydrogels as biomimetic scaffolds in  
579 biomedical fields or water purification systems, capitalizing on their anisotropic  
580 architecture and their biocompatible composition.

581

## 582 **5. Acknowledgement**

583 This work was supported by both the Paris Ile-de France Region - DIM Respire, The  
584 French Embassy in Tokyo through Bourses France Excellence and by French state funds  
585 managed by the National Research Agency (ANR) through the CellsInFoams project,  
586 grant n. ANR-17-CE08-0009

## 587 **6. Declaration of Competing Interest**

588 The authors declare that they have no known competing financial interests or personal  
589 relationships that could have appeared to influence the work reported in this paper.

## 590 **7. CRediT author statement**

591 Katsuya KOMIYAMA: Investigation, Writing - Original Draft. Maya ALLARD:  
592 Investigation. Corentin ESCHENBRENNER: Investigation. Ahmed HAMRAOUI:  
593 Investigation. Clémence SICARD: Writing - Review & Editing, Supervision, Funding  
594 acquisition. Francisco M. FERNANDES: Conceptualization, Writing - Review & Editing,  
595 Supervision, Funding acquisition.

## 596 **8. References**

- 597 [1] T.I. Baskin, Anisotropic expansion of the plant cell wall, *Annu Rev Cell Dev*  
598 *Biol* 21 (2005) 203–222.  
599 <https://doi.org/10.1146/annurev.cellbio.20.082503.103053>.
- 600 [2] W. Kong, C. Wang, C. Jia, Y. Kuang, G. Pastel, C. Chen, G. Chen, S. He, H. Huang,  
601 J. Zhang, S. Wang, L. Hu, Muscle-Inspired Highly Anisotropic, Strong, Ion-  
602 Conductive Hydrogels, *Advanced Materials* 30 (2018) 1–7.  
603 <https://doi.org/10.1002/adma.201801934>.
- 604 [3] P. Calvert, Hydrogels for soft machines, *Advanced Materials* 21 (2009) 743–756.  
605 <https://doi.org/10.1002/adma.200800534>.
- 606 [4] M.J. Hancock, K. Sekeroglu, M.C. Demirel, Bioinspired directional surfaces for  
607 adhesion, wetting, and transport, *Adv Funct Mater* 22 (2012) 2223–2234.  
608 <https://doi.org/10.1002/adfm.201103017>.

- 609 [5] J. Radhakrishnan, A. Subramanian, U.M. Krishnan, S. Sethuraman, Injectable and  
610 3D Bioprinted Polysaccharide Hydrogels: From Cartilage to Osteochondral Tissue  
611 Engineering, *Biomacromolecules* 18 (2017) 1–26.  
612 <https://doi.org/10.1021/acs.biomac.6b01619>.
- 613 [6] P. Datta, V. Vyas, S. Dhara, A.R. Chowdhury, A. Barui, Anisotropy Properties of  
614 Tissues: A Basis for Fabrication of Biomimetic Anisotropic Scaffolds for Tissue  
615 Engineering, *J Bionic Eng* 16 (2019) 842–868. [https://doi.org/10.1007/s42235-](https://doi.org/10.1007/s42235-019-0101-9)  
616 [019-0101-9](https://doi.org/10.1007/s42235-019-0101-9).
- 617 [7] S. Murdan, Electro-responsive drug delivery from hydrogels, 92 (2003) 1–17.
- 618 [8] M.H. Cai, X.Y. Chen, L.Q. Fu, W.L. Du, X. Yang, X.Z. Mou, P.Y. Hu, Design  
619 and Development of Hybrid Hydrogels for Biomedical Applications: Recent  
620 Trends in Anticancer Drug Delivery and Tissue Engineering, *Front Bioeng*  
621 *Biotechnol* 9 (2021) 1–18. <https://doi.org/10.3389/fbioe.2021.630943>.
- 622 [9] N. Annabi, K. Tsang, S.M. Mithieux, M. Nikkhah, A. Ameri, A. Khademhosseini,  
623 A.S. Weiss, Highly elastic micropatterned hydrogel for engineering functional  
624 cardiac tissue, *Adv Funct Mater* 23 (2013) 4950–4959.  
625 <https://doi.org/10.1002/adfm.201300570>.
- 626 [10] M. Nikkhah, N. Eshak, P. Zorlutuna, N. Annabi, M. Castello, K. Kim, A.  
627 Dolatshahi-Pirouz, F. Edalat, H. Bae, Y. Yang, A. Khademhosseini, Directed  
628 endothelial cell morphogenesis in micropatterned gelatin methacrylate hydrogels,  
629 *Biomaterials* 33 (2012) 9009–9018.  
630 <https://doi.org/10.1016/j.biomaterials.2012.08.068>.
- 631 [11] Z. Chen, D. Zhao, B. Liu, G. Nian, X. Li, J. Yin, S. Qu, W. Yang, 3D Printing of  
632 Multifunctional Hydrogels, *Adv Funct Mater* 29 (2019) 1–8.  
633 <https://doi.org/10.1002/adfm.201900971>.
- 634 [12] T. Distler, A.R. Boccaccini, 3D printing of electrically conductive hydrogels for  
635 tissue engineering and biosensors – A review, *Acta Biomater* 101 (2020) 1–13.  
636 <https://doi.org/10.1016/j.actbio.2019.08.044>.
- 637 [13] M.A. Haque, G. Kamita, T. Kurokawa, K. Tsujii, J.P. Gong, Unidirectional  
638 alignment of lamellar bilayer in hydrogel: One-dimensional swelling, anisotropic  
639 modulus, and stress/strain tunable structural color, *Advanced Materials* 22 (2010)  
640 5110–5114. <https://doi.org/10.1002/adma.201002509>.
- 641 [14] X. Ying Lin, Z. Jian Wang, P. Pan, Z. Liang Wu, Q. Zheng, Monodomain  
642 hydrogels prepared by shear-induced orientation and subsequent gelation, (2016).  
643 <https://doi.org/10.1039/c6ra17103f>.
- 644 [15] J.M. Jang, S.H.T. Tran, S.C. Na, N.L. Jeon, Engineering controllable architecture



- 645 in Matrigel for 3D cell alignment, *ACS Appl Mater Interfaces* 7 (2015) 2183–2188.  
646 <https://doi.org/10.1021/am508292t>.
- 647 [16] Q. Lu, S. Bai, Z. Ding, H. Guo, Z. Shao, H. Zhu, D.L. Kaplan, Hydrogel Assembly  
648 with Hierarchical Alignment by Balancing Electrostatic Forces, *Adv Mater*  
649 *Interfaces* 3 (2016) 1–6. <https://doi.org/10.1002/admi.201500687>.
- 650 [17] W. Shi, J. Huang, R. Fang, M. Liu, Imparting Functionality to the Hydrogel by  
651 Magnetic-Field-Induced Nano-assembly and Macro-response, *ACS Appl Mater*  
652 *Interfaces* 12 (2020) 5177–5194. <https://doi.org/10.1021/acsami.9b16770>.
- 653 [18] K. Qin, C. Parisi, F.M. Fernandes, Recent advances in ice templating: From  
654 biomimetic composites to cell culture scaffolds and tissue engineering, *J Mater*  
655 *Chem B* 9 (2021) 889–907. <https://doi.org/10.1039/d0tb02506b>.
- 656 [19] E. Thibert, F. Dominé, Thermodynamics and Kinetics of the Solid Solution of HCl  
657 in Ice, *J Phys Chem B* 101 (1997) 3554–3565. <https://doi.org/10.1021/jp962115o>.
- 658 [20] E. Thibert, F. Dominé, Thermodynamics and Kinetics of the Solid Solution of  
659 HNO<sub>3</sub> in Ice, *J Phys Chem B* 102 (1998) 4432–4439.  
660 <https://doi.org/10.1021/jp980569a>.
- 661 [21] T. Köhnke, T. Elder, H. Theliander, A.J. Ragauskas, Ice templated and cross-  
662 linked xylan/nanocrystalline cellulose hydrogels, *Carbohydr Polym* 100 (2014)  
663 24–30. <https://doi.org/10.1016/j.carbpol.2013.03.060>.
- 664 [22] K. Yan, F. Xu, S. Li, Y. Li, Y. Chen, D. Wang, Ice-templating of chitosan/agarose  
665 porous composite hydrogel with adjustable water-sensitive shape memory  
666 property and multi-staged degradation performance, *Colloids Surf B Biointerfaces*  
667 190 (2020) 110907. <https://doi.org/10.1016/j.colsurfb.2020.110907>.
- 668 [23] S. Christoph, J. Kwiatoszynski, T. Coradin, F.M. Fernandes, Cellularized Cellular  
669 Solids via Freeze-Casting, *Macromol Biosci* 16 (2016) 182–187.  
670 <https://doi.org/10.1002/mabi.201500319>.
- 671 [24] P. Sikorski, F. Mo, G. Skjåk-Bræk, B.T. Stokke, Evidence for egg-box-compatible  
672 interactions in calcium - Alginate gels from fiber x-ray diffraction,  
673 *Biomacromolecules* 8 (2007) 2098–2103. <https://doi.org/10.1021/bm0701503>.
- 674 [25] A. Isogai, T. Saito, H. Fukuzumi, TEMPO-oxidized cellulose nanofibers,  
675 *Nanoscale* 3 (2011) 71–85. <https://doi.org/10.1039/c0nr00583e>.
- 676 [26] H. Dong, J.F. Snyder, K.S. Williams, J.W. Andzelm, Cation-induced hydrogels of  
677 cellulose nanofibrils with tunable moduli, *Biomacromolecules* 14 (2013) 3338–  
678 3345. <https://doi.org/10.1021/bm400993f>.
- 679 [27] N. Masruchin, B.D. Park, V. Causin, I.C. Um, Characteristics of TEMPO-oxidized  
680 cellulose fibril-based hydrogels induced by cationic ions and their properties,



- 681 Cellulose 22 (2015) 1993–2010. <https://doi.org/10.1007/s10570-015-0624-0>.
- 682 [28] T. Guo, Y. Pei, K. Tang, X. He, J. Huang, F. Wang, Mechanical and drug release  
683 properties of alginate beads reinforced with cellulose, *J Appl Polym Sci* 134 (2017)  
684 44495. <https://doi.org/10.1002/APP.44495>.
- 685 [29] L.F. Wang, S. Shankar, J.W. Rhim, Properties of alginate-based films reinforced  
686 with cellulose fibers and cellulose nanowhiskers isolated from mulberry pulp,  
687 *Food Hydrocoll* 63 (2017) 201–208.  
688 <https://doi.org/10.1016/J.FOODHYD.2016.08.041>.
- 689 [30] T. Huq, S. Salmieri, A. Khan, R.A. Khan, C. Le Tien, B. Riedl, C. Fraschini, J.  
690 Bouchard, J. Uribe-Calderon, M.R. Kamal, M. Lacroix, Nanocrystalline cellulose  
691 (NCC) reinforced alginate based biodegradable nanocomposite film, *Carbohydr*  
692 *Polym* 90 (2012) 1757–1763. <https://doi.org/10.1016/j.carbpol.2012.07.065>.
- 693 [31] T. Saito, A. Isogai, TEMPO-Mediated Oxidation of Native Cellulose. The Effect  
694 of Oxidation Conditions on Chemical and Crystal Structures of the Water-  
695 Insoluble Fractions, *Biomacromolecules* 5 (2004) 1983–1989.  
696 <https://doi.org/10.1021/bm0497769>.
- 697 [32] J. Esmaili, S. Jadbabae, F.M. Far, M.E. Lukolayeh, K.K. Kırboğa, F.S. Rezaei,  
698 A. Barati, Decellularized *Alstroemeria* flower stem modified with chitosan for  
699 tissue engineering purposes: A cellulose/chitosan scaffold, *Int J Biol Macromol*  
700 204 (2022) 321–332. <https://doi.org/10.1016/j.ijbiomac.2022.02.019>.
- 701 [33] C. Stolze, T. Janoschka, U.S. Schubert, F.A. Müller, S. Flauder, Directional  
702 Solidification with Constant Ice Front Velocity in the Ice-Templating Process, *Adv*  
703 *Eng Mater* 18 (2016) 111–120. <https://doi.org/10.1002/adem.201500235>.
- 704 [34] C. Rieu, C. Parisi, G. Mosser, B. Haye, T. Coradin, F.M. Fernandes, L. Trichet,  
705 Topotactic Fibrillogenesis of Freeze-Cast Microridged Collagen Scaffolds for 3D  
706 Cell Culture, *ACS Appl Mater Interfaces* 11 (2019) 14672–14683.  
707 <https://doi.org/10.1021/acsami.9b03219>.
- 708 [35] D. Legland, I. Arganda-Carreras, P. Andrey, MorphoLibJ: Integrated library and  
709 plugins for mathematical morphology with ImageJ, *Bioinformatics* 32 (2016)  
710 3532–3534. <https://doi.org/10.1093/bioinformatics/btw413>.
- 711 [36] J. Schindelin, I. Arganda-Carreras, E. Frise, V. Kaynig, M. Longair, T. Pietzsch,  
712 S. Preibisch, C. Rueden, S. Saalfeld, B. Schmid, J.Y. Tinevez, D.J. White, V.  
713 Hartenstein, K. Eliceiri, P. Tomancak, A. Cardona, Fiji: An open-source platform  
714 for biological-image analysis, *Nat Methods* 9 (2012) 676–682.  
715 <https://doi.org/10.1038/nmeth.2019>.
- 716 [37] S. Ardizzonea, G. Gabriellib, P. Lazzarib, Adsorption of Methylene Blue at

- 717 solid/liquid and water/air interfaces, 1993.
- 718 [38] C. Rieu, C. Parisi, G. Mosser, B. Haye, T. Coradin, F.M. Fernandes, L. Trichet,  
719 Topotactic Fibrillogenesis of Freeze-Cast Microridged Collagen Scaffolds for 3D  
720 Cell Culture, *ACS Appl Mater Interfaces* 11 (2019) 14672–14683.  
721 <https://doi.org/10.1021/acsami.9b03219>.
- 722 [39] C. Rodríguez-Rivero, L. Hilliou, E.M. Martín del Valle, M.A. Galán, Rheological  
723 characterization of commercial highly viscous alginate solutions in shear and  
724 extensional flows, *Rheol Acta* 53 (2014) 559–570.  
725 <https://doi.org/10.1007/S00397-014-0780-4/METRICS>.
- 726 [40] E.A. Pinto, J.L. Dávila, M.A. d'Ávila, Rheological studies on nanocrystalline  
727 cellulose/alginate suspensions, *J Mol Liq* 277 (2019) 418–423.  
728 <https://doi.org/10.1016/j.molliq.2018.12.091>.
- 729 [41] I. Nelson, S.E. Naleway, Intrinsic and extrinsic control of freeze casting, *Journal*  
730 *of Materials Research and Technology* 8 (2019) 2372–2385.  
731 <https://doi.org/10.1016/j.jmrt.2018.11.011>.
- 732 [42] B. Thomas, S. Geng, J. Wei, H. Lycksam, M. Sain, K. Oksman, Ice-Templating of  
733 Lignin and Cellulose Nanofiber-Based Carbon Aerogels: Implications for Energy  
734 Storage Applications, *ACS Appl Nano Mater* (2022).  
735 <https://doi.org/10.1021/ACSANM.2C01033>.
- 736 [43] S. Christoph, P. Barré, B. Haye, T. Coradin, F.M. Fernandes, Environmentally-  
737 stable eco-friendly pectin-silica bio-hybrid foams for soil remediation, *Giant* 12  
738 (2022) 100119. <https://doi.org/10.1016/j.giant.2022.100119>.
- 739 [44] S. Deville, Ice-templating, freeze casting: Beyond materials processing, *J Mater*  
740 *Res* 28 (2013) 2202–2219. <https://doi.org/10.1557/jmr.2013.105>.
- 741 [45] J.U. Hernández-Beltrán, I.O. Hernández-De Lira, M.M. Cruz-Santos, A. Saucedo-  
742 Luevanos, F. Hernández-Terán, N. Balagurusamy, Insight into pretreatment  
743 methods of lignocellulosic biomass to increase biogas yield: Current state,  
744 challenges, and opportunities, *Applied Sciences (Switzerland)* 9 (2019).  
745 <https://doi.org/10.3390/APP9183721>.
- 746 [46] K.A. KHALID, A.A. AHMAD, T.L.-K. YONG, Lignin Extraction from  
747 Lignocellulosic Biomass Using Sub- and Supercritical Fluid Technology as  
748 Precursor for Carbon Fiber Production, *Journal of the Japan Institute of Energy* 96  
749 (2017) 255–260. <https://doi.org/10.3775/JIE.96.255>.
- 750 [47] P. Ghanney, J.X. Kugbe, D.K. Anning, Role of Microbial Biomechanics in  
751 Composting with Special Reference to Lignocellulose Biomass Digestion, *Asian J*  
752 *Biotechnol Bioresour Technol* (2021) 30–46.

- 753 <https://doi.org/10.9734/AJB2T/2021/V7I130093>.
- 754 [48] E.M. Ahmed, Hydrogel: Preparation, characterization, and applications: A review,  
755 J Adv Res 6 (2015) 105–121. <https://doi.org/10.1016/j.jare.2013.07.006>.
- 756 [49] X. Zhou, Y. Guo, F. Zhao, G. Yu, Hydrogels as an Emerging Material Platform  
757 for Solar Water Purification, Acc Chem Res 52 (2019) 3244–3253.  
758 <https://doi.org/10.1021/acs.accounts.9b00455>.
- 759 [50] V.I. Lozinsky, O. Okay, Basic Principles of Cryotropic Gelation, Advances in  
760 Polymer Science 263 (2014) 49–101. [https://doi.org/10.1007/978-3-319-05846-](https://doi.org/10.1007/978-3-319-05846-7_2)  
761 [7\\_2](https://doi.org/10.1007/978-3-319-05846-7_2).
- 762 [51] H. Bai, A. Polini, B. Delattre, A.P. Tomsia, Thermoresponsive composite  
763 hydrogels with aligned macroporous structure by ice-templated assembly,  
764 Chemistry of Materials 25 (2013) 4551–4556. <https://doi.org/10.1021/cm4025827>.
- 765 [52] M. Barrow, H. Zhang, Aligned porous stimuli-responsive hydrogels via directional  
766 freezing and frozen UV initiated polymerization, Soft Matter 9 (2013) 2723–2729.  
767 <https://doi.org/10.1039/c2sm27722k>.
- 768 [53] J. Wu, Q. Zhao, J. Sun, Q. Zhou, Preparation of poly(ethylene glycol) aligned  
769 porous cryogels using a unidirectional freezing technique, Soft Matter 8 (2012)  
770 3620–3626. <https://doi.org/10.1039/c2sm07411g>.
- 771 [54] J. Wu, Y. Lin, J. Sun, Anisotropic volume change of poly(N-isopropylacrylamide)-  
772 based hydrogels with an aligned dual-network microstructure, J Mater Chem 22  
773 (2012) 17449–17451. <https://doi.org/10.1039/c2jm34010k>.
- 774 [55] M. Barrow, A. Eltmimi, A. Ahmed, P. Myers, H. Zhang, Frozen polymerization  
775 for aligned porous structures with enhanced mechanical stability, conductivity, and  
776 as stationary phase for HPLC, J Mater Chem 22 (2012) 11615–11620.  
777 <https://doi.org/10.1039/c2jm31425h>.
- 778 [56] M. Chen, J. Zhu, G. Qi, C. He, H. Wang, Anisotropic hydrogels fabricated with  
779 directional freezing and radiation-induced polymerization and crosslinking method,  
780 Mater Lett 89 (2012) 104–107. <https://doi.org/10.1016/j.matlet.2012.08.087>.
- 781 [57] L.H. Montezor, L.G.D. Benevenuto, B.F. Antunes, A.C. Amaral, L.P. Novo, A.J.F.  
782 Carvalho, E. Trovatti, The influence of chitosan, cellulose and alginate chemical  
783 nature on mineral matrix formation, International Journal of Polymeric Materials  
784 and Polymeric Biomaterials 71 (2022) 875–885.  
785 <https://doi.org/10.1080/00914037.2021.1919669>.
- 786 [58] E.M. Fernandes, R.A. Pires, J.F. Mano, R.L. Reis, Bionanocomposites from  
787 lignocellulosic resources: Properties, applications and future trends for their use in  
788 the biomedical field, Prog Polym Sci 38 (2013) 1415–1441.

- 789 <https://doi.org/10.1016/j.progpolymsci.2013.05.013>.
- 790 [59] I.K. Susheel Kalia, B. S. Kaith, Cellulose Fibers: Bio- and Nano-Polymer  
791 Composites, Springer Berlin Heidelberg, 2011. [https://doi.org/10.1007/978-3-642-](https://doi.org/10.1007/978-3-642-17370-7)  
792 [17370-7](https://doi.org/10.1007/978-3-642-17370-7).
- 793 [60] R. Lucas, Ueber das Zeitgesetz des kapillaren Aufstiegs von Flüssigkeiten,  
794 Kolloid-Zeitschrift 23 (1918) 15–22. <https://doi.org/10.1007/BF01461107>.
- 795 [61] W. Gardner, Note on the dynamics of capillary flow, Physical Review 18 (1921)  
796 206–209. <https://doi.org/10.1103/PhysRev.18.206>.
- 797
- 798

## Supporting information

799

800

801 Ice templating water-stable macroporous polysaccharide hydrogels  
802 to mimic plant stems

803

804 *Katsuya KOMIYAMA*<sup>1</sup>, *Maya ALLARD*<sup>1</sup>, *Corentin ESCHENBRENNER*<sup>1</sup>, *Clémence*  
805 *SICARD*<sup>2,3</sup>, *Ahmed HAMRAOUI*<sup>1,4</sup> *Francisco M. FERNANDES*<sup>1\*</sup>

806

807 <sup>1</sup> Sorbonne Université, UMR 7574, Laboratoire de Chimie de la Matière Condensée de  
808 Paris,

809 75005, Paris, France

810 <sup>2</sup> Université de Versailles Saint-Quentin-en Yvelines, UMR 8180, L'Institut Lavoisier de  
811 Versailles, 78035, Versailles, France

812 <sup>3</sup> Institut Universitaire de France

813 <sup>4</sup> Université Paris Cité, CNRS, UMR8003, Saints Pères Paris Institute for the  
814 Neurosciences, 45, rue des Saints-Pères, 75006 Paris, France

815

816 \* Corresponding author. E-mail: francisco.fernandes@sorbonne-universite.fr; Tel: +33 1  
817 44 27 62 45

818

819

820

821

822

823

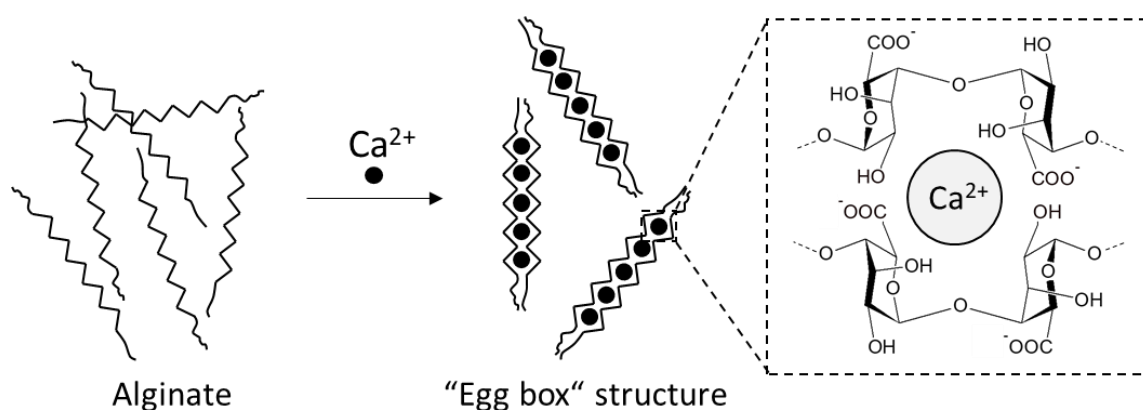
824

825

826

827

828



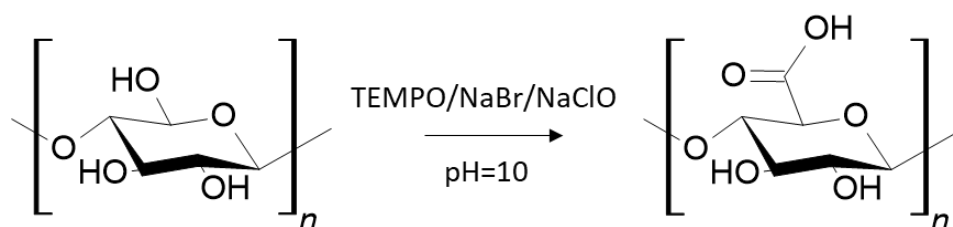
829

830 **Figure S1.** Egg-box structure of alginate gel in the presence of Ca<sup>2+</sup>.

831

832

833



834

835 **Figure S2.** Scheme of TEMPO oxidation of cellulose.

836

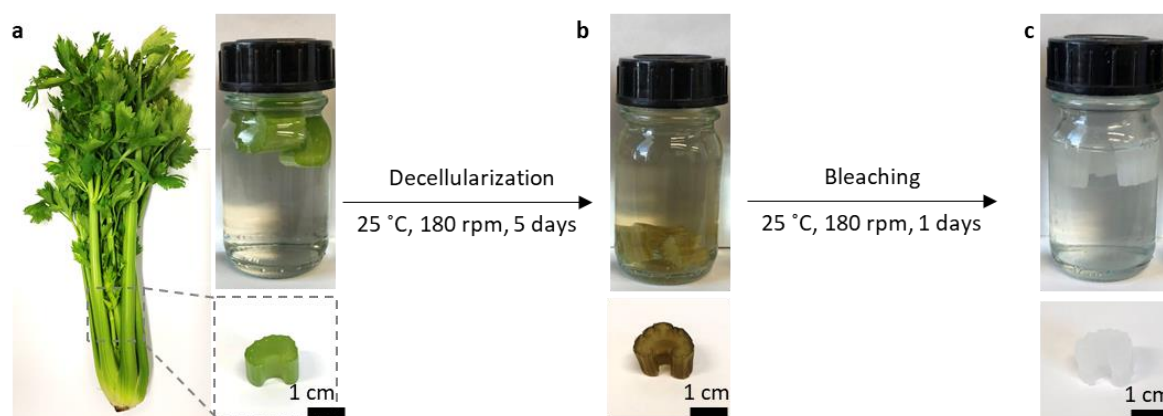
837

838

839

840

841

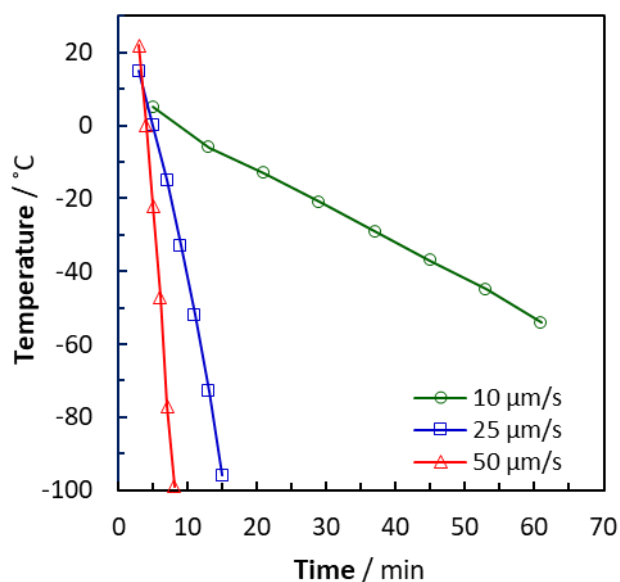


842 **Figure S3.** The scheme of the decellularization and bleaching for the celery (*Apium*  
843 *graveolens*), (a) The stem of the celery was cut into 1 cm and then (b) cut samples was

844 immersed in 10 % SDS solution for 5 days. (c) After 5 days decellularization, samples  
845 are immersed in NaClO solution for 1 day for bleaching.

846

847



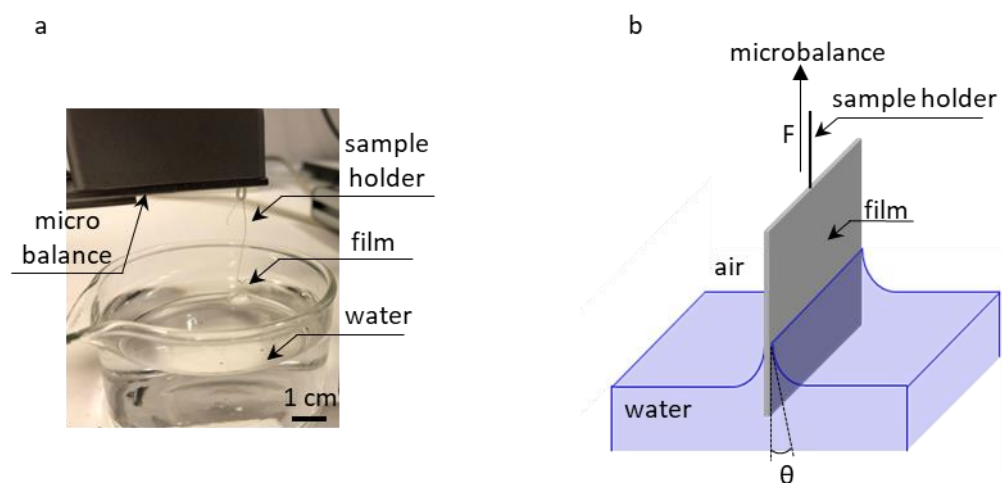
848

849 **Figure S4.3** cooling temperature profiles applied in this study for the unidirectional ice-  
850 templating, resulting in constant ice-front velocity of 10, 25 and 50 μm/s.

851

852

853



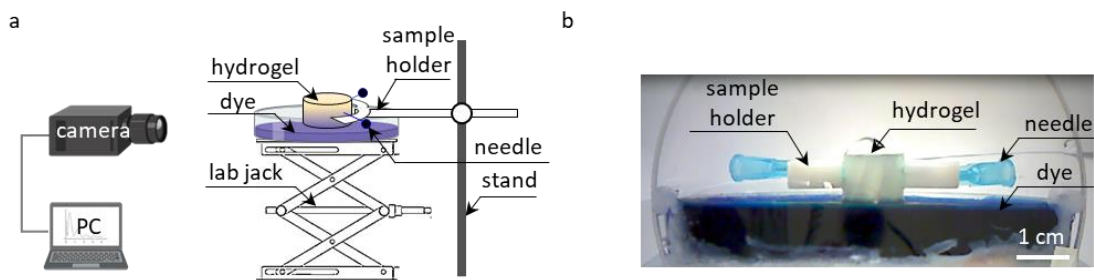
854

855 **Figure S5.** (a) The photo and (b) schematic illustration of the dynamic contact angle  
856 measurement with tensiometer.

857



858



859

860

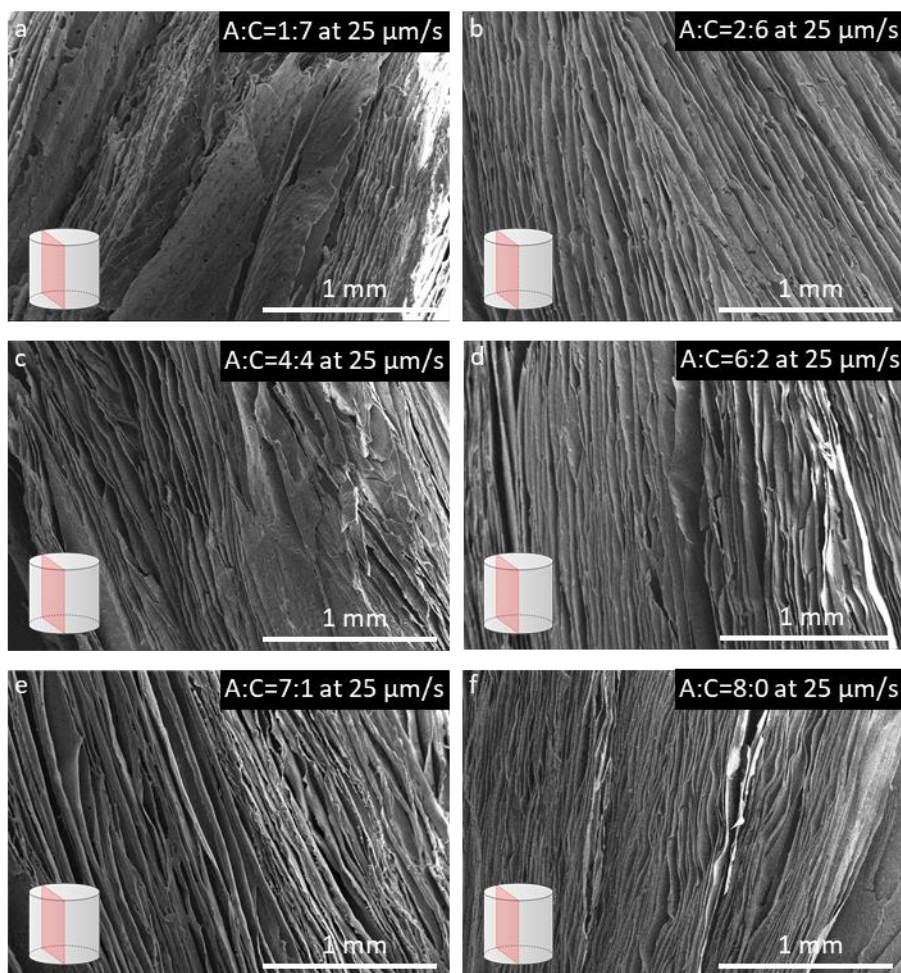
861

862

863

864

**Figure S6.** Liquid transport experiment with different composition of alginate and oxidized cellulose and with different ice-growth velocity. (a) Schematic illustration of the liquid transport experimental setup, (b) the photo through the lens of the camera during liquid transport experiment.



865

866

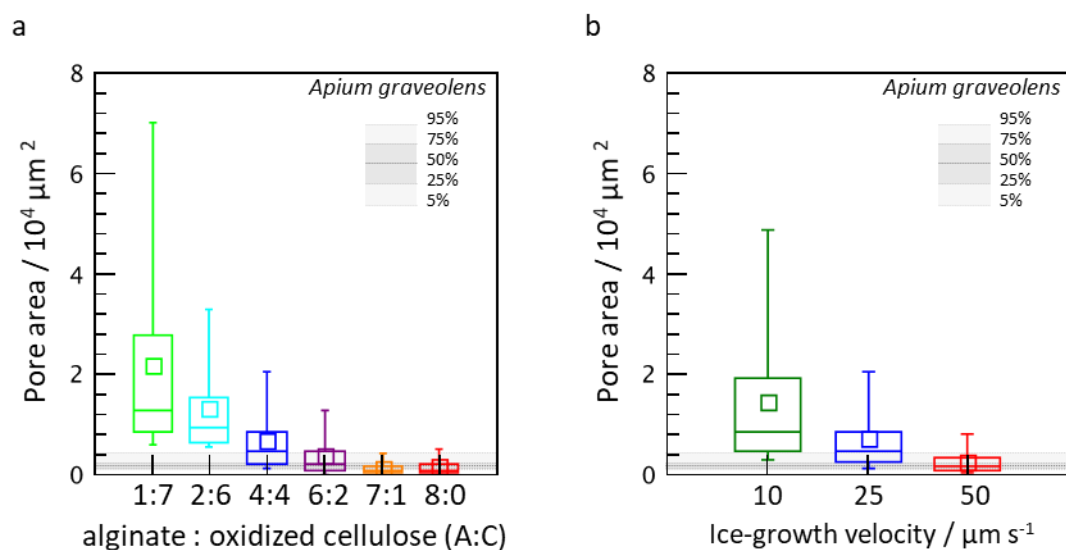
867

868

**Figure S7.** SEM images in longitudinal section of Ca-crosslinked hydrogels with the different ratio of alginate and oxidized cellulose prepared at constant ice growth velocity ( $25 \mu\text{m/s}$ ). (a) A:C=8:0, (b) A:C=7:1, (c) A:C=6:2, (d) A:C=4:4, (e) A:C=2:6, and (f)



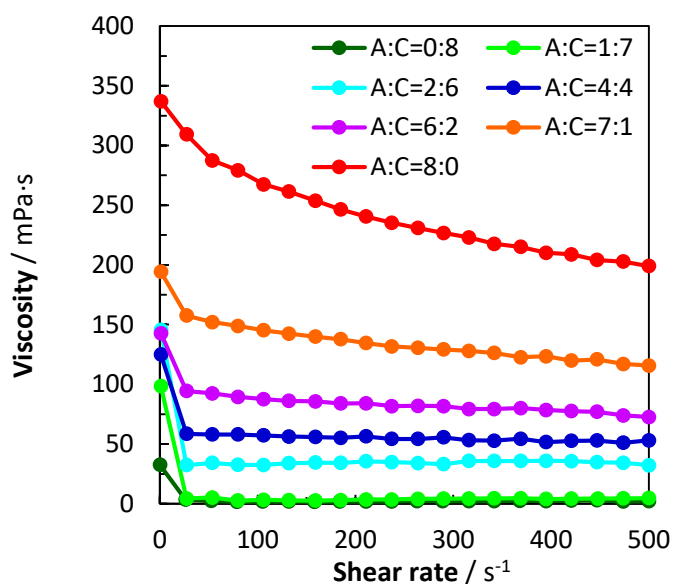
869 A:C=1:7.



870

871 **Figure S8.** Normal scale pore distribution. (a) Summary of the pore area distribution of  
872 alginate and oxidized cellulose macroporous hydrogels at different compositions for 25  
873  $\mu\text{m/s}$  (ice growth velocity). (b) Summary of the pore area distribution of alginate and  
874 oxidized cellulose macroporous hydrogels (A:C=4:4) at different ice front velocities.  
875 Moustaches delimit the 5 and 95 percentiles of the distribution and box limits represent  
876 the 1st and 3rd quartiles. Gray horizontal bars depict the pore size distribution of *A.*  
877 *graveolens* xylem vascular system.

878



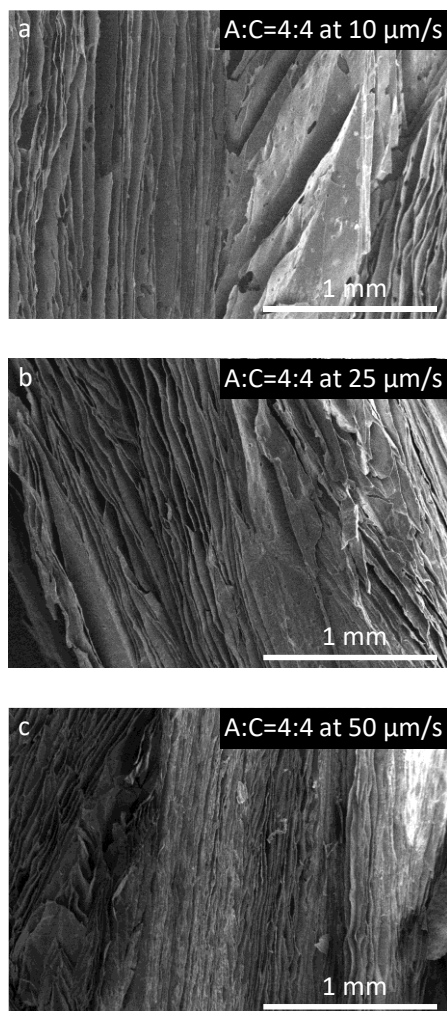
879

880 **Figure S9.** Viscosity profile of the suspensions with different ratio of alginate and

881 oxidized cellulose.

882

883



884

885 **Figure S10.** SEM images in longitudinal section of Ca-crosslinked hydrogels prepared at  
886 different ice growth velocity (10, 25, and 50  $\mu\text{m/s}$ ) at constant ratio of alginate and  
887 oxidized cellulose (4:4). (a)  $v = 10 \mu\text{m/s}$ , (b)  $v = 25 \mu\text{m/s}$ , and (c)  $v = 50 \mu\text{m/s}$ .

888

889

890

891

892

893

894

895

896

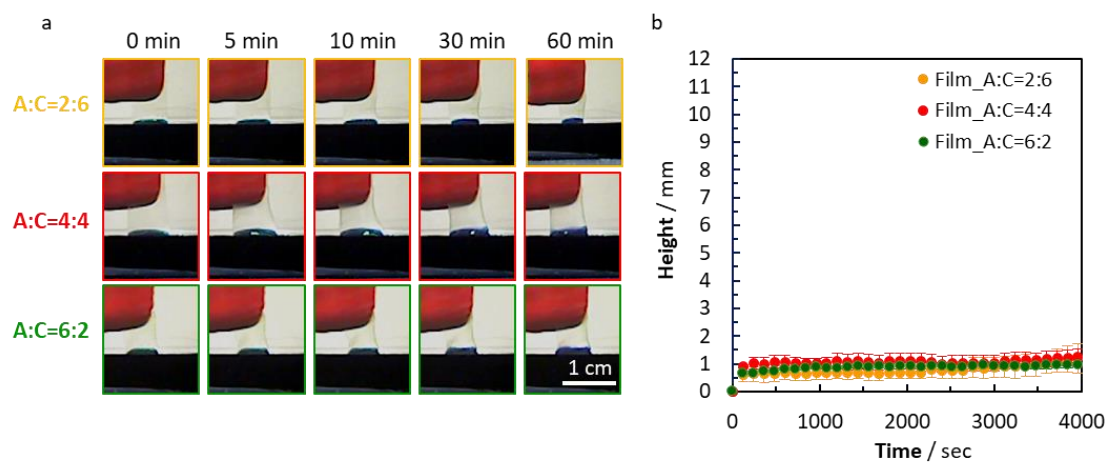
897 **Table S1.** Mechanical properties of hydrogels with an ice growth velocity of 25  $\mu\text{m/s}$   
 898 with different compositions of alginate/oxidized cellulose (A:C) after ion-crosslinking.

	Young's modulus / MPa	Toughness / $\text{J/m}^3$	Yield stress / KPa	Compression stress $\epsilon=20\%$ / KPa	Compression stress $\epsilon=40\%$ / KPa	Compression stress $\epsilon=60\%$ / KPa
0:8	$0.003 \pm 0.001$	$0.04 \pm 0.01$	$0.7 \pm 0.2$	$0.3 \pm 0.1$	$0.8 \pm 0.2$	$1.6 \pm 0.5$
1:7	$0.008 \pm 0.003$	$0.08 \pm 0.02$	$0.8 \pm 0.3$	$1.0 \pm 0.1$	$1.8 \pm 0.2$	$3.8 \pm 0.8$
2:6	$0.032 \pm 0.017$	$0.15 \pm 0.03$	$1.5 \pm 0.2$	$2.1 \pm 0.4$	$2.7 \pm 0.5$	$5.3 \pm 1.1$
4:4	$0.034 \pm 0.015$	$0.23 \pm 0.05$	$3.4 \pm 1.1$	$3.9 \pm 0.9$	$4.4 \pm 0.8$	$6.1 \pm 1$
6:2	$0.070 \pm 0.017$	$0.31 \pm 0.05$	$4.1 \pm 0.9$	$5.1 \pm 1$	$5.8 \pm 0.9$	$8.4 \pm 1.1$
7:1	$0.084 \pm 0.019$	$0.40 \pm 0.05$	$6.0 \pm 0.9$	$6.5 \pm 0.9$	$7.3 \pm 0.6$	$11.4 \pm 1.5$
8:0	$0.096 \pm 0.036$	$0.39 \pm 0.08$	$5.0 \pm 1.5$	$5.8 \pm 1.3$	$7.5 \pm 1.3$	$10.8 \pm 1.9$

899

900

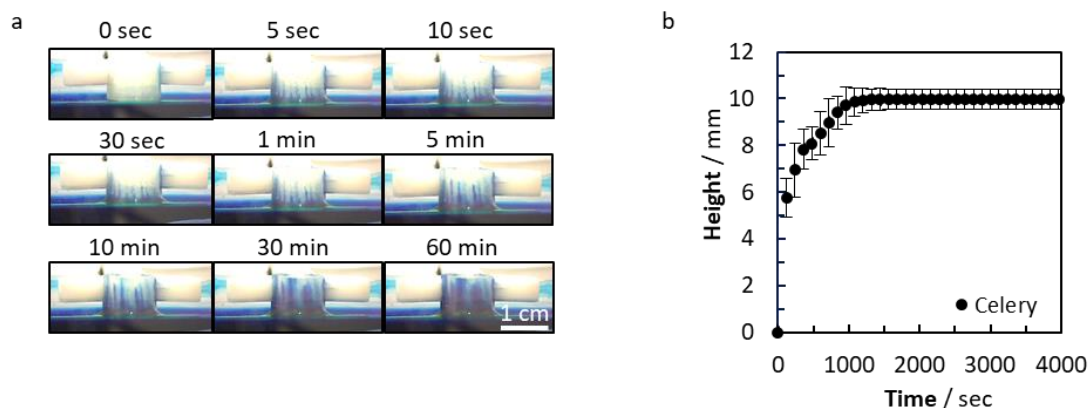
901



902

903 **Figure S11.** Liquid transport experiment using the films with different compositions of  
 904 alginate and oxidized cellulose. (a) Optical photos showing capillary action behavior. (b)  
 905 Time-liquid height curves.

906



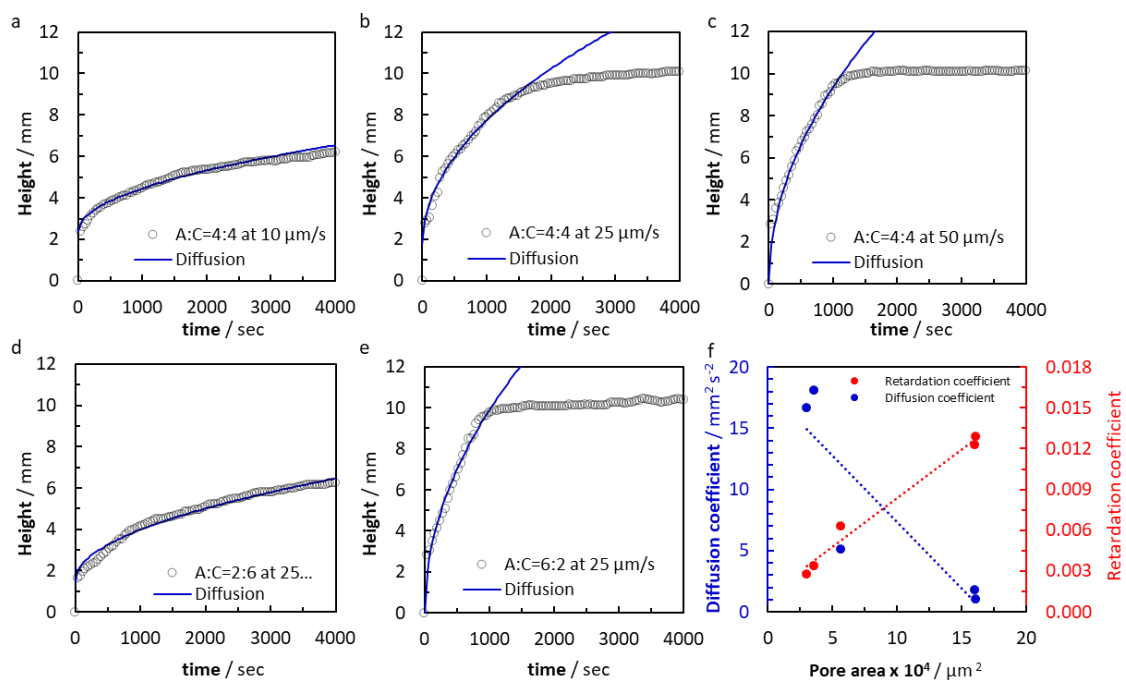
907

908 **Figure S12.** Liquid transport experiment with celery. (a) Optical photos showing capillary  
 909 action behavior. (b) Time-liquid height curves and rising speeds of celery.

910

911

912



913

914 **Figure S13.** Capillary water transport behavior of hydrogels prepared with different ice-  
 915 growth velocities (a-c) and different compositions of alginate and oxidized cellulose (d  
 916 and e) and those theoretical curves fitting to the equation of mean square displacement  
 917 (i.e.  $h(t)^2=6Dt$ ), (f) trends among pore area, diffusion coefficients, and retardation  
 918 coefficients. Dashed lines are a guide to the eye.

919