# Multicomponent delivery system based on biologically produced gold nanoparticles for targeted therapy of breast cancer *in vivo*

Parastoo Pourali<sup>1</sup><sup>†</sup>, Eva Neuhöferová<sup>1</sup><sup>†</sup>, Volha Dzmitruk<sup>2</sup>, Milan Svoboda<sup>3</sup>, Eva Stodůlková<sup>1</sup>, Miroslav Flieger<sup>1</sup>, Behrooz Yahyaei<sup>4, 5</sup> & Veronika Benson<sup>1\*</sup>

<sup>1</sup>Institute of Microbiology, Czech Academy of Sciences, Czech Republic

<sup>2</sup>Center of Molecular Structure, Institute of Biotechnology, Czech Academy of Sciences, Czech Republic

<sup>3</sup>Institute of Analytical Chemistry, Czech Academy of Sciences, Brno, 602 00, Czech Republic;

<sup>4</sup>Department of Medical Sciences, Shahrood Branch, Islamic Azad University, Shahrood, Iran;

<sup>5</sup>Department of Medical Sciences, Biological Nanoparticles in Medicine Research Center, Shahrood Branch, Islamic Azad University, Shahrood, Iran;

<sup>†</sup>Both with the same contributions and preferably as first authors.

\*Email: benson@biomed.cas.cz

### Abstract

This study recognized biologically produced gold nanoparticles (AuNP) as multiple cargo carriers with a perspective of drugs delivery into specialized tumor cells *in vivo*. Paclitaxel (PTX), transferrin, and antimiR-135b were conjugated with AuNPs and their uptake by mouse tumor cells in an induced breast cancer model was investigated. Each of the above-mentioned molecules was conjugated to the AuNPs separately as well as simultaneously, loading efficiency of each cargo was assessed, and performance of the final product (FP) was assessed. After tumor induction in BALB/c mice, sub-IC<sub>50</sub> doses of FP as well as control AuNPs, PTX, and PBS were administered *in vivo*. Round AuNPs were prepared using *Fusarium oxysporum* and exhibited size of  $13 \pm 1.3$  nm and zeta potential of  $-35.8 \pm 1.3$  mV. The cytotoxicity of individual conjugates and FP were tested by MTT assay in breast tumor cells 4T1 and non-tumor fibroblasts NIH/3T3 cells. The conjugation of the individual molecules with AuNPs was confirmed and FP (size of  $54 \pm 14$  nm and zeta potential of  $-31.9 \pm 2.08$  mV) showed higher 4T1-specific toxicity *in vitro* when compared to control conjugates. After *in vivo* application of the FP, TEM analyses proved presence of AuNPs in the tumor cells. Hematoxylin and eosin

staining of the tumor tissue revealed that the FP group exhibited the highest amounts of inflammatory, necrotic, and apoptotic cells in contrast to control groups. Finally, qPCR results showed that FP could transfect and suppress miR-135b expression *in vivo*, confirming the tumor-targeting properties of FP. The capacity of biologically produced gold nanoparticles to conjugate with multiple decorative molecules while remaining their stability and effective intracellular uptake makes them promising alternative strategy superior to current drug carriers.

**Key words:** Multicomponent drug delivery system; Biologically produced gold nanoparticles; Paclitaxel; Transferrin; AntimiR-135b; miRNA knock-down.

### Introduction

Breast cancer (BC) is one of the most common cancers in women [1] as there were 2.3 million of new BC cases (with 685,000 deaths) reported worldwide in 2020 [2]. There are several different strategies to combat BC depending on the subtype and stage of the cancer [1, 3]. Surgical resection, chemotherapy, and radiation therapy are the three main therapies used to treat BC, and each has its own advantages and disadvantages. For example, radiation therapy affects the surrounding normal tissue. Both chemotherapy and radiation therapy cause DNA damage. Although chemotherapy drugs target fast-growing cells and suppress the proliferation of cancer cells, in some cases resistance to the anticancer drugs occurs. Therefore, there is a need for a new approach that allows to overcome these issues [4].

Through many efforts in these decades, the characteristics and pathways of different subtypes of BC have been identified, which has helped to better target a specific subtype of BC [3, 5]. Recently, new strategies of BC treatment focus on targeted therapies. Goal of the targeted therapy is to deliver anticancer drug into selective cancer cells without affecting the non-cancerous environment. For example, trastuzumab therapy (Herceptin, an IgG1 monoclonal humanized mouse antibody) binds to the ECD of the HER2 transmembrane receptor. Blockade of the receptor inhibits the downstream signal transduction pathway and induces apoptosis [5]. A newer strategy is receptor-targeted therapy [6]. In this method, the specific chemotherapeutic agent is bound to the specific ligand of the cancer cell and the drug can enter the cells by binding the ligand to its receptor. After receptor-mediated endocytosis, the drug is delivered into the cancer cells [6]. For example, ado-trastuzumab emtansine conjugate consisting of a fungal toxin emtansine (DM1) and trastuzumab. In this approach, trastuzumab possessing affinity to HER2, mediates conjugate internalization and delivery of DM1 into tumor cells, resulting in microtubules blockage [5]. Application of receptor-targeted therapy allows to decrease dosage of the chemotherapeutic drugs, their cumulative toxicity, and side effects for patients.

Although this technique has its own advantages, tumor resistance has been reported in some cases. One type of resistance is called acquired resistance [7]. In tumors, there are heterogeneous populations of both types, target-positive and target-negative cancer cells. The administration of a targeted therapy triggers a selection pressure that leads to the selection of target-negative tumor cells that do not respond to the therapy. This is the main reason of acquired cancer resistance development [7, 8]. To overcome or prevent this problem can be challenged by multiple targets strategies with a synergistic anti-tumor effect aiming at different subtypes of cancer cells [7]. Using multiple targets strategies prior to the development of acquired tumor resistance may prevent treatment complications caused by regrowth of drug resistant tumor.

These days, molecules used for the multiple targeting strategy include specific cancer cell ligands (such as monoclonal antibodies, hormones, or small protein molecules), ribonucleic acid interference (RNAi) molecules, and chemotherapeutic agents [9]. The use of RNAi molecules to inhibit gene expression in cancer cells is straightforward, but one of the drawbacks of this technique is the short half-life of the interfering RNA. It has been reported that the association of these molecules with some types of nanoparticles (NPs) increases their plasma circulation time and payload to the cancer cells without affecting the non-cancer cells [10]. In this strategy, the NPs protect the RNAs from RNases and deliver the RNA usually combined with a cytostatic directly into the cytoplasm of the cancer cells without the need for an additional transfection reagent. Among the various NPs used for this objective, gold nanoparticles (AuNPs) are attracting more attention due to their biocompatibility and ability to bind to various molecules.

There are three different techniques for producing AuNPs, which are divided into biological, physical, and chemical techniques. The disadvantages of the chemical method for producing AuNPs are the persistence of some toxic elements on the surfaces of the produced AuNPs and their environmental toxicity [11]. The disadvantages of the physical technique are its time-consuming preparation and a polydisperse product. The production of AuNPs by biological systems is safe, simple, fast, inexpensive, and environmentally friendly [11]. Different types of microbial strains such as bacteria and fungi are capable of producing high yields of AuNPs. In principle, the microorganisms reduce the gold ions to AuNPs to reduce their toxicity. This reduction occurs intracellularly or extracellularly and via non-enzymatic or enzymatic pathways [12, 13]. After reduction of gold ions, molecules (like proteins) secreted by the microorganisms, naturally cover the surface of newly formed AuNPs. These molecules are called capping agent and they prevent AuNPs from agglomerating, even when the produced

AuNPs are in a close contact [14, 15]. Therefore, the obtained AuNPs are always monodisperse and uniform in size. These capping agents are responsible for the direct conjugation of the AuNPs with other molecules through electrostatic or ionic interactions due to the charged amino acids on their surface [16] which eliminates the need for additional linkers [17-19]. AuNPs produced by the biological method possibly evade the immune system [20] and there are some reports on their nonimmunogenic nature [21].

In this study, the AuNPs were prepared using a biological method. They were then conjugated with different molecules to produce a synergistic effect for multifunctional targeted drug delivery. Paclitaxel (PTX, as the BC chemotherapeutic drug), antimiR-135b (for targeting microRNA-135b), and human transferrin (Tf, as a ligand for its receptor overexpressed on BC cells) were conjugated to AuNPs. MicroRNA-135b (miR-135b) was chosen following our past research [22]. The miR-135b is overproduced in BC cells acting as an oncogene and regulator of BC cell proliferation, migration, and invasion [23]. Down-regulation of miR-135b was shown to be a possible therapeutic strategy for an adjuvant treatment of BC [24]. After conjugation of the individual components with biologically produced AuNPs, we tested performance of the different AuNP conjugates *in vitro*. Subsequently we followed with administration of the multi-component AuNP conjugate as well as control AuNPs and PTX into tumor-bearing animals *in vivo*. We found perspective performance of the multi-component AuNP conjugate as well as control AuNPs and PTX into tumor-bearing animals *in vivo*. We found perspective performance of the multi-component AuNP conjugate as well as control AuNPs and PTX into tumor-bearing animals *in vivo*. We found perspective performance of the multi-component AuNP conjugate as well as control AuNPs and PTX into tumor-bearing animals *in vivo*. We found perspective performance of the multi-component AuNP conjugate regarding tumor cells internalization, miR-135b knock-down, and tumor cells death.

#### Materials and methods

### Cultivation of fungi and production of AuNPs

*Fusarium oxysporum* (CCF 3732) was cultured in Sabouraud Dextrose Broth (SDB, Sigma Aldrich, Prague, Czech Republic) at 30 °C under shaking conditions for approximately 1 week. The biomass was separated from the culture medium by centrifugation at 8000 rpm for 15 min, and the supernatant was used to prepare extracellular AuNPs [16]. For this purpose, HAuCl<sub>4</sub>.3H<sub>2</sub>O (Sigma Aldrich, Prague, Czech Republic) was added to the supernatant at a final concentration of 1 mmol, and the pH was adjusted to 7.5. The dispersion was heated directly at 80 °C for 5 min and the color change indicated the formation of AuNPs. The negative control flask containing sterile SDB and a final concentration of 1 mmol HAuCl<sub>4</sub>.3H<sub>2</sub>O was heated in the same condition.

### **Characterization of the AuNPs**

Prior to any test, the obtained color-changed AuNPs dispersions were washed three times with ddH<sub>2</sub>O. During washing process, the AuNPs were collected by centrifugation at 15000 rpm for 30 min [11]. AuNPs were characterized using spectrophotometry, transmission electron microscopy (TEM), energy dispersive X-ray spectroscopy (EDS), zetasizer, and Fourier-transform infrared spectroscopy (FTIR); and the methodologies were described previously [14, 15]. Au concentration was determined by graphite furnace atomic absorption spectroscopy (GF-AAS) as described in our previous study [14].

### Conjugation and loading efficiency tests

Different molecules (Tf, antimiR-135b, and PTX) were used for conjugation with AuNPs. First, a standard curve was constructed based on the known amounts of each molecule, then each molecule at different amounts was conjugated separately. The best conjugate with the highest loading but still stable (according to the color change of AuNPs and spectrophotometry analysis) was selected and its loading efficiency on AuNPs was measured. Using the equation from each curve and an online tool (available at www.wolframalpha.com), the amount of bound molecule was determined. Finally, AuNPs-Tf- antimiR-135b-PTX (i.e., FP) was prepared and the amount of each molecule was determined. All conjugation experiments were performed in triplicate.

### Conjugation of AuNPs to Tf and Tf-load assessment

Eight  $\mu$ L of Tf-labelled Texas Red (5 mg/mL, Life Technologies, Prague, Czech Republic) stock solution was diluted with 192  $\mu$ L of RNase free ddH<sub>2</sub>O. To generate a Tf standard curve, <sup>1</sup>/<sub>2</sub> serial dilutions of Tf were prepared in a 96-well microtiter plate using RNase free ddH<sub>2</sub>O and the fluorescence intensity of the wells was determined at excitation/emission wavelengths of 580/609 nm using Tecan spectrophotometer (Thermo Fisher Scientific, Prague, Czech Republic).

For the conjugation study, 32  $\mu$ L of Tf (5 mg/mL) was added to 1184  $\mu$ L of AuNPs and 384  $\mu$ L of ddH<sub>2</sub>O. This ratio was the best one that showed no AuNPs spectra distortion after adding to the AuNPs (optimization data are not presented). The dispersion was incubated in a thermomixer (Eppendorf, Hamburg, Germany) at 1000 rpm and 4 °C overnight [19, 25]. The dispersion was then centrifuged at 15000 g for 30 min, and the supernatant was examined at the indicated excitation/emission wavelengths to determine the amounts of unbound Tf. The pellet was washed three times with RNase-free ddH<sub>2</sub>O and used for detection and cytotoxicity analyses.

### Conjugation of AuNPs to antimiR-135b and antimir-load assessment

AntimiR-135b was designed during our previous research to specifically inhibit mammalian microRNA-135b. The RNA sequence used was 5' rUrCrA rCrArU rArGrG rArArU rGrArA rArArG rCrCrA rUrA - 3' labelled at 5' with Alexa Fluor 488 [22]. The stock solution of 100  $\mu$ mol antimiR-135b was diluted to 0.03125  $\mu$ mol and then ½ serial dilutions were performed in a 96-well microtiter plate. The excitation/emission wavelengths were 488/520 nm, and the fluorescence intensity was determined in each well. The assay was performed three times and the standard curve was generated. To conjugate the AuNPs with antimiR-135b, different amounts of AuNPs were conjugated with different amounts of antimiR-135b (50 µL AuNPs + 50 µL RNA (50 mmol), 60 µL AuNPs + 40 µL RNA (40 mmol), 70 µL AuNPs + 30 µL RNA (30 mmol), and 80 µL AuNPs + 20 µL RNA (20 mmol). Finally, 118 µL of antimiR-135b at a concentration of 100 µmol was added to 1184 µL of the AuNPs and 282 µL of ddH<sub>2</sub>O dispersion. This amount was the best one that showed no AuNPs spectra distortion after adding to the AuNPs (optimization data are not presented). The dispersion was incubated overnight in a thermomixer at 1000 rpm at 4 °C [19, 25]. The dispersion was then centrifuged at 15000 g for 30 min. Because of the high fluorescence intensity of conjugated fluorophore, the supernatant was first diluted and then examined at 488/520 nm wavelengths to determine the amounts of unbound antimiR-135b. The pellet was washed three times with RNase-free ddH<sub>2</sub>O and used for detection and cytotoxicity analyses.

### Conjugation of AuNPs to PTX and PTX-load assessment

The standard curve of PTX (1 mg/mL, Sigma Aldrich, Prague, Czech Republic) stock solution was constructed by using  $\frac{1}{2}$  serial dilutions of the drug in a 96-well plate (the first well contained 1 mg/mL PTX). The absorbance of the different concentrations of the drug was determined by spectrophotometry at a wavelength of 230 nm [26]. To conjugate the AuNPs with PTX, 160 µL of PTX (1 mg/mL) was added to 1184 µL of AuNPs and 240 µL of ddH<sub>2</sub>O and incubated overnight in a thermomixer at 1000 rpm at 4 °C. This amount was the best one that showed no AuNPs spectra distortion after adding to the AuNPs (optimization data are not presented). The dispersion was then centrifuged at 15000 g for 30 minutes, and the supernatant was examined at the same wavelength (i.e., 230 nm) to detect amounts of unbound PTX. The pellet was washed three times with RNase-free ddH<sub>2</sub>O and used for detection and cytotoxicity analyses [18].

# Conjugation of AuNPs to PTX, antimiR-135b, and Tf (FP formation) and load assessments

After establishing the standard curve and demonstrating conjugation of each molecule with the AuNPs, PTX, antimiR-135b, and Tf were added to the AuNPs. For this purpose, 32  $\mu$ L of Tf stock solution (5 mg/mL), 1184  $\mu$ L AuNPs, 118  $\mu$ L antimiR-135b (100  $\mu$ mol), 160  $\mu$ L PTX stock solution (1 mg/mL) and 90  $\mu$ L of ddH<sub>2</sub>O were combined and incubated overnight in a thermomixer at 1000 rpm at 4 °C. The dispersion was centrifuged at 15000 g for 30 minutes and the supernatant, after dilution, was analyzed for fluorescence intensity (for Tf and antimiR-135b) and optical density (for PTX) at the above wavelengths to estimate the amounts of individual unbound molecules in the supernatant and subsequently the amounts of molecules attached to the AuNPs surface. FP was washed three times with RNase-free ddH<sub>2</sub>O and used for detection and cytotoxicity analyses.

### **Proof of conjugation**

To demonstrate that the final AuNP conjugate consisted of AuNPs, Tf, PTX, and antimiR-135b, the FP samples were analyzed using spectrophotometry, zetasizer, and FTIR techniques as mentioned earlier.

Data from the size and zeta potential analyzes were compared using analysis of variance (ANOVA) in SPSS software as an online tool (available at https://astatsa.com/OneWay\_Anova\_with\_TukeyHSD). p-values of  $\leq 0.05$  and  $\leq 0.01$  were considered as significant.

To confirm Tf conjugation to AuNPs, the conjugates (both AuNPs-Tf and FP) were analyzed using a liquid chromatography-mass spectrometry system (LC-MS) (Agilent 1200 series, Agilent Technologies, USA) operated in positive data-dependent mode and connected to a timsToF Pro PASEF mass spectrometer with CaptiveSpray (Bruker Daltonics, USA). A C18 trap column (UHPLC Fully Porous Polar C18 2.1mm ID, Phenomenex) and a C18 column (Luna Omega 3  $\mu$ m Polar C18 100 Å, 150  $\times$  0.3 mm, Phenomenex) were used in this experiment. Results were analyzed using PEAKS Studio 10.0 software (Bioinformatics Solutions, Canada) and the UniProt database (all taxa. 11/2021) [27]. To confirm PTX conjugation to AuNPs, the supernatants of the conjugates (both AuNPs-PTX and FP) were analyzed using high performance liquid chromatography (HPLC). For the analysis of PTX, the same HPLC instrument was used as previously published [28]. The mobile phases, which contained water, were filtered through a 0.22 mM GS filter (Millipore, Billerica, MA, USA) and degassed in an ultrasonic bath for 10 min before use. The mobile phase consisted of water (A) and methanol (B), to each of which 0.01% acetic acid was added. A Kinetex 5m C18 column (250 x 4.6 mm, Phenomenex) with a guard column was used for analysis. Gradient elution started at 30% B (0 min) and increased linearly to 100% B within 15 min at a flow rate of 1 mL/min. UV detection was performed at 227 nm. The amount of PTX was quantified using a calibration curve. A standard solution (1mg/mL PTX in DMSO) was further diluted in methanol to final concentrations of 20, 10, 2, 0.2 and 0.1 mg. mL<sup>-1</sup>. The calibration plot was constructed by plotting the integrated peak areas of PTX against concentration. The following linear regression equation and correlation coefficient were obtained: y = 12574x - 11860,  $R^2 = 0.9998$ .

To confirm conjugation of antimiR-135b with AuNPs, the pellets of the conjugates (both AuNPs-antimiR-135b and FP) were analyzed by agarose gel electrophoresis. The migration delay of the conjugates compared with the control as a sign of successful conjugation was evaluated [29, 30].

### Cytotoxicity assay

To analyze the activity of the conjugates in cell culture, an MTT assay was performed for FP and controls including AuNP and PTX alone. For this purpose, a 96-well tissue culture plate (JETBiofil, Guangzhou, China) was used, and  $2 \times 10^{-3}$  cells/mL of a 4T1 cell line (cell line derived from mammary adenocarcinoma of BALB/c mouse strain, ATCC CRL -2539) were added to 4 rows of the plate. The other 4 rows were filled with the same amounts of NIH/3T3 (cell line of immortalized fibroblasts derived from NIH/Swiss mouse strain, ATCC CRL -1658) cells. The culture medium for 4T1 cell line was Roswell Park Memorial Institute Medium 1640 (RPMI-1640, Sigma Aldrich, Prague, Czech Republic) supplemented with 10 % fetal bovine serum (FBS, Gibco, Massachusetts, USA), 44 µg/mL gentamicin (Sandoz, Novartis Company, Prague, Czech Republic), and 4.5 g/L glucose (Sigma Aldrich, Prague, Czech Republic). The culture medium for NIH/3T3 cells was Dulbecco's Modified Eagle Medium (DMEM, Sigma Aldrich, Prague, Czech Republic) supplemented with 10 % FBS and 50 mg/L gentamicin. After incubation of the plate in 37°C and 5 % CO<sub>2</sub> overnight (reaching confluency 60 %), cells in each row of the plate were challenged with 1/2 concentration of the FP obtained by titration (the pellet of the conjugate was dissolved into 250 µL of appropriate media). Control wells were loaded separately with AuNPs and PTX. For PTX as a control, a concentration equal to the determined amount of PTX in the FP was used. Six wells served as untreated controls and contained only the cells.

After overnight incubation, 100  $\mu$ L of appropriate media with 20  $\mu$ L of 5 mg/mL of 3-(4,5-Dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT, EMD Millipore, CA, USA) in phosphate buffered saline (PBS) were added into all the experimental wells and cells were incubated for another 4 h. Formazan crystals were dissolved in dimethyl sulfoxide (DMSO, Sigma Aldrich, Prague, Czech Republic) and absorbance at 570 nm was analyzed in each well using a Tecan spectrophotometer at a reference wavelength of 630 nm. The Cell survival rate (%) and therefore the percentage of half-maximal inhibitory concentration (IC<sub>50</sub>) was calculated by this formula: Cell survival rate (%) = (a-c)/(b-c) × 100 (a = absorbance of each well containing conjugate or drug, b = absorbance of the control well without any conjugate or drug, and c = absorbance of the blank) [31].

#### In vivo experiment

The in vivo study was performed with respect to the Czech Law on Animal Protection Act no 246/1992 and was approved by ethical committee of the Czech Academy of Sciences with the number 14-2022-P. Twenty Balb/c mice (female, six weeks old) were used in the study. The mice were randomly housed in cages with 5 animals/cage and received food and water ad *libitum*. To induce mammary tumors, a suspension of 10<sup>6</sup> freshly prepared 4T1 cells in PBS was injected subcutaneously into the fourth left mammary fat pad. The mice were kept for tumor development for 14 days and observed every two days. After the developed tumor reached a diameter of approximately 5 mm, treatment was started. Each cage was considered as a group and treated separately with PBS, AuNPs, PTX and FP. The administration dose was 50 µL sub-IC<sub>50</sub> concentration of each sample (i.e., AuNPs, PTX, and FP) determined by MTT assay, and the injection was performed on three consecutive days into four regions of peripheral tumor tissue. Tumor size was measured before the start of treatment and after the last treatment. Under deep anesthesia (using ketamine/xylazine), one animal from each group was sacrificed one hour after the third dose by cervical dislocation, and the tumor tissue was harvested [22]. These animals are referred here as the group I. The remaining mice were sacrificed in the same manner five days after administration of the last dose. The diameter of each tumor outside the body was measured quickly and the tumor volume was calculated according to the formula:  $(A \times B \times C)/2$ [32]. These animals are referred here as the group II.

Each tumor sample was divided into three parts immediately after size measurement, one part was placed in the cold and fresh fixator and stored in the 4 °C for TEM, second part was placed in the fresh formaldehyde 4 % and stored at 4 °C for hematoxylin and eosin staining (H & E

staining), and the third part was homogenized and retrieved cells were kept in about 65 % ethanol at -20 °C for GF-AAS, flow cytometry, and qPCR (described below).

### **TEM and EDS analysis**

The samples from group I were cut into small cubes (1 mm<sup>3</sup>) and were fixed immediately in the fixator contained 3% formaldehyde, 1 % glutaraldehyde in 0.1 M sodium cacodylate buffer (pH 7.4) and preserved at 4°C. Next day, the sections were then washed in sodium cacodylate buffer and post fixed with 1 % OsO4 in sodium cacodylate buffer. After washing steps with the same buffer and water, different concentrations of acetone in water were used and embedded in Epon-Araldite resin. After polymerization the resin, the sections were prepared using a microtome. Jeol JEM-F200 TEM operated at 200 kV equipped by TVIPS XF 416 CMOS camera was used for imaging. JED 2300 X-ray spectrometer was applied for obtaining EDS spectra from the specific detected AuNPs and the raw spectra were analyzed using standardless Zeta factor method in Jeol AnalysisStation software.

### H & E staining

The tumor samples from group II were fixed and embedded in the paraffin blocks. Using microtome, sample slices of 5  $\mu$ m thickness were prepared and stained by H & E method [33]. Differences in parameters such as neoplastic, necrotic, apoptotic, and inflammatory cells as well as the amount of blood accumulation were analyzed and compared in the different groups under the light microscope.

### Homogenization of the tumor samples and internalization of AuNPs analysis

To separate the cells, tumors from group II were homogenized in PBS, centrifuged at 1500 rpm for 5 min, and resuspended in PBS / 70 % ethanol (1:9). In this stage, cells were stored at -20 °C till further processing. To evaluate cellular internalization of FP and AuNP samples, 1 mL of each sample was analyzed with GF-AAS and the amounts of Au present in the tumor derived cells were calculated.

### qPCR

qPCR analysis was employed in order to assess the inhibitory effect of the antimiR-135b on its target (i.e., miR-135b) in FP group. The control samples (i.e., AuNPs, PTX, and PBS groups) were analyzed as well and used as controls. All the samples were from the group II. The microRNA was isolated Using High Pure miRNA isolation Kit (Roche, Prague, Czech Republic) [22] and its amount was determined using Invitrogen Qubit RNA high sensitivity Kit

(Thermo Fisher Scientific, Prague, Czech Republic). High-Capacity cDNA Reverse Transcription Kit (Thermo Fisher Scientific, Prague, Czech Republic) was applied for cDNA synthesis. The miR-specific reverse transcription primers were miR-16 (assay 000391, Thermo Fisher Scientific, Prague, Czech Republic) and miR-135b (assay 002261). miR-specific RT-PCR primers and TaqMan Universal PCR Master Mix (No AmpErase) were used for amplification and each sample was tested in triplicate. The amplification and the data analysis employed an iQ5 Real Time PCR Detection System (BioRad, Prague, Czech Republic) and an iQ5 Optical System Software 2.1 (BioRad, Prague, Czech Republic), respectively. The miR-135b expression was normalized to the miR-16 internal control [22].

### **Results and discussion**

### Cultivation of fungi and production of AuNPs

The results showed that the color of the supernatant containing HAuCl<sub>4</sub>.3H<sub>2</sub>O changed from yellow to crimson after incubation, indicating the formation of AuNPs (Figure 1. A). Color of the non-challenged control flask remained unchanged (Figure 1. B).

# Characterization of the AuNPs

### Spectrophotometry

Spectrophotometry showed that AuNPs exhibited a maximum absorption peak at 528 nm, confirming the presence of AuNPs in the dispersion (Figure 1. C).



Figure 1. Preparation of AuNPs by challenging supernatant from microbial culture with Au<sup>+</sup> ions. A) color-changed supernatant after formation of AuNPs, B) control supernatant, and C) spectrophotometry of the AuNPs dispersion showing the maximum absorption peak at 528 nm.

### **TEM and EDS**

The results from TEM confirm the presence of AuNPs in the samples with polygonal shape and average size of 15 nm. EDS confirmed the presence of elemental Au in the sample. Figure 2 shows the obtained results.



Figure 2. Representative TEM and EDS analyses of the biologically produced AuNPs. A) TEM (scale bar = 50 nm) and B) Location of areas that were analyzed by EDS (scale bar = 100 nm), the spot 009 represents background and the spot 010 represents AuNPs rich area. C) EDS analysis of AuNPs (in blue) and background (in red).

The Au peaks in Figure 2 C confirm the presence of elemental Au in the sample. There are several other peaks, such as Cu peaks belonging to the copper grid, and C peak, which confirms the presence of organic matter present on the AuNPs surface.

### **Zetasizer analysis**

The hydrodynamic diameters (sizes estimated by DLS) and surface zeta potentials of the AuNPs as well as subsequent conjugates are listed in Table 1. The average hydrodynamic diameter of the original AuNPs was about  $13 \pm 1$  nm and they possessed negative zeta potential about -35 mV (Table 1).

### **GF-AAS**

The GF-AAS showed that totally  $2.24 \pm 0.10$  mg of Au was found in the 1184  $\mu$ L AuNPs in ddH<sub>2</sub>O sample.

# Conjugation and loading efficiency tests

As shown in Supplementary image 1 A, the color of the dispersions was constant after conjugation of the AuNPs with individual components - PTX, antimiR-135b, and Tf as well as with their mixture (FP). The conjugates were resuspended in sera-supplemented culture media (DMEM with 10 % FBS and gentamycin), proving that the AuNP conjugates remain stable and the presence of sera and the incubation of AuNPs with the cargoes did not affect the nature of the AuNPs in respect to agglomeration.

# Determination of the loading amounts of each molecule in AuNPs-Tf, AuNPs-antimiR-135b, AuNPs-PTX and the prepared FP

Standard curves of Tf, antimiR-135b, and PTX were determined (Supplementary image 1B, C, and D) in order to estimate the load of the individual components within AuNP conjugates. The estimated amount of each molecule in AuNPs-conjugate was determined using equation based on the fluorescence intensity of the supernatants (in the case of Tf and antimiR-135b) or absorbance at 230 nm of the the supernatant containing PTX.

Considering the standard curves, we estimated that in average AuNP conjugates contained 0.041 mg/mL of Tf (in the AuNPs-Tf conjugate) or 0.66  $\mu$ mol of antimiR-135b (in the AuNPs-antimiR-135b conjugate) per 1 mg of the present AuNPs. In the case of the AuNPs-PTX conjugate as well as the FP all (0.16 mg) the added PTX was present within the conjugate (containing in average 2.24 mg of AuNPs). Next to PTX, the FP consisted of 0.83  $\mu$ mol of antimiR-135b and 0.037 mg/mL of Tf per 1 mg of AuNPs.

### **Proof of conjugation**

### Spectrophotometry

The maximum absorbance peak of each conjugate compared to original AuNPs as control was determined using Nanodrop and representative spectra are shown in Figure 3.

The maximum absorption peak of default AuNPs (528 nm) shifted based on conjugation with particular molecule: AuNPs-Tf (529 nm), AuNPs-antimiR-135b (527 nm), AuNPs-PTX (539 nm), and the FP (529 nm). The shift in the maximum absorption peak point to successful conjugation.

The FP remained stable, and as shown in Figure 3 D, the slope of the peak was well maintained. Although the spectra slope of the AuNPs-PTX was blunt compared to the default AuNPs, the FP samples exhibited sharp slope of the spectrum, indicating that the AuNPs were uniform in size.



Figure 3. Representative spectra distribution exhibited by individual AuNP conjugates (blue) and their comparison to default AuNPs (red). A) AuNPs-Tf, B) AuNPs-antimiR, C) AuNPs-PTX, and D) the FP.

# Hydrodynamic diameter and zeta potential of the conjugates

Hydrodynamic diameter shows size of the nanoparticle core together with the surface molecules. Such size evaluation might differ from estimates based on solely AuNP core. After conjugation of different cargoes with AuNPs, the AuNPs exhibited size below 100 nm. All the conjugates also carried remarkable negative zeta potential supporting our previous statements regarding retained stability of AuNPs after any conjugation (Table 1).

Table 1. Statistical analyses of differences in hydrodynamic diameter (Size) and zeta potential (Charge) of default AuNPs and AuNPs conjugated with different cargoes. P-values are based on five individual measurements detailed in Supplementary table 1. Significant p-values are in bold, the p-values of  $\leq 0.01$  are marked with \*\*, and the p-values of  $\leq 0.05$  are marked with \*.

Charge	AuNPs	AuNPs-Tf	AuNPs-PTX	AuNPs-antimiR	FP
AuNPs	N/A	0.89	0.001**	0.08	0.02*
AuNPs-Tf	0.001**	N/A	0.002**	0.03*	0.052
AuNPs-PTX	0.001**	0.89	N/A	0.001**	0.56
AuNPs-antimiR	0.02*	0.001**	0.001**	N/A	0.001**
FP	0.001**	0.27	0.18	0.003**	N/A

Significant differences in size and surface charge were evaluated by ANOVA Analysis and the post-hoc Tukey HSD test.

As expected, all the conjugates were significantly larger (showed larger hydrodynamic diameter) in comparison to the default AuNPs. Furthermore, there were no significant differences in size among AuNPs-Tf, AuNPs-PTX, and FP conjugates but all these conjugates were significantly larger than AuNPs-antimiR.

Regarding the surface charge, we found no significant difference between default AuNPs and AuNPs-Tf or AuNPs-antimiR conjugates. On the other hand, conjugation of PTX resulted in significant change of zeta potential in comparison to other conjugates as well as default AuNPs. While there was no difference in surface charge between AuNPs-PTX and FP, we speculate, the PTX component plays a key role in determining the final surface charge of the FP.

### Proof of the cargo conjugation to AuNPs by FTIR

The FTIR spectra of FP and the individual components, i.e. AuNPs, Tf, and PTX were analyzed. Representative spectra of the FP conjugate compared to the individual components as controls is shown in Figure 4.



Figure 4. FTIR spectra of FP compared to control spectra of individual components AuNP, PTX, and Tf. A) Full range IR spectra from 3500 to 900 cm<sup>-1</sup>, B) detailed IR spectra from 3500 to 2500 cm<sup>-1</sup>, C) detailed IR spectra from 1800 to 900 cm<sup>-1</sup>.

As presented in Figure 4 A and B, FP spectrum has overlapped multiple peaks of N-H and O-H stretching vibration spreading from about 3480 to 3280 cm<sup>-1</sup>, while the AuNP as well as Tf have a broad peak centered at 3290 cm<sup>-1</sup> and PTX has a broad peak centered at about 3450 to 3400 cm<sup>-1</sup>. The overlapped peak of FP likely sums signals originated from PTX with AuNP and/or Tf. Similar to Tf spectra, the C-H vibration region of FP exhibits two peaks at 2960 cm<sup>-1</sup> and 2935 cm<sup>-1</sup>, which corresponds to - C(sp<sup>3</sup>)-H vibrations of CH2/CH3 groups present in protein side chains; and two peaks of =C(sp<sup>2</sup>)-H stretching vibrations which are originated from

PTX. Further, the peak at about 1450 cm<sup>-1</sup> represents the  $CH_2$  scissoring mode and it is present in each compound (Figure 4 C).

In the fingerprint IR absorption region (Figure 4 C) of FP spectrum, majority of peaks possess the same positions as PTX spectrum clearly indicating presence of PTX. The PTX strong sharp peaks at 1733 cm<sup>-1</sup> and 1701 cm<sup>-1</sup> are shifted in FP spectrum towards 1733 cm<sup>-1</sup> and 1702 cm<sup>-1</sup> and correspond to C=O stretching and C=C stretching, which also is supported with peaks of C=C bending of PTX at 905 cm<sup>-1</sup> and 983 cm<sup>-1</sup> for both compounds. As all tested components contain amides, they all have an amide I and amide II peaks at about 1650 cm<sup>-1</sup> and 1540 cm<sup>-1</sup>, and so does the FP. There are also common peaks at 1250 cm<sup>-1</sup> denoting C-N stretching and at 1071 to 1081 cm<sup>-1</sup> representing absorption of C-O stretching.

There are two unique weak peaks at FP spectrum that are not present in other samples (at 1017 cm<sup>-1</sup> (shoulder) and 1017 cm<sup>-1</sup>) which may correspond to C-O ribose stretching of nucleic acid. Major IR bands of nucleic acids are at about 1247 cm<sup>-1</sup> and 1085 cm<sup>-1</sup> (-PO4 stretching) and about 1655 cm<sup>-1</sup> or 1700 cm<sup>-1</sup> (C=O stretching) that are present at PTX spectra and may be overlapped (Figure 4 C). We suggest there is small amount of nucleic acids within the FP, but it is arguable since the statement it based only on FTIR data.

### LC-MS

Mass spectrometry analysis of AuNPs-Tf and the FP confirmed the presence of Tf in both samples and the results are consistent with the FTIR results. Table 2 presents adequate output data.

Table 2. LC-MS output set, regarding Tf presence on the surface of AuNPs, from both AuNPs-Tf and FP samples.

Protein	Protein		Coverage		Avg.					
Group	ID	Accession	(%)	Intensity	Mass	Description				
AuNPs-Tf										
						Serotransferrin OS=Homo sapiens				
1	131110	P02787 TRFE_HUMAN	77	1.08E+06	77064	OX=9606 GN=TF PE=1 SV=3				
FP										
						Serotransferrin OS=Homo sapiens				
1	131110	P02787 TRFE_HUMAN	76	6.62E+04	77064	OX=9606 GN=TF PE=1 SV=3				
						Serotransferrin OS=Pan troglodytes				
2	131111	A5A6I6 TRFE_PANTR	70	4.14E+02	77064	OX=9598 GN=TF PE=2 SV=1				

### HPLC

The HPLC analysis (Figure 5) confirmed effective binding of PTX within the FP and AuNPs-PTX conjugates, and obtained data agree with the FTIR analysis. There was no free PTX detected in supernatants originating from the FP and AuNPs-PTX samples. Representative analysis of the FP supernatant is shown in Figure 5. Full chromatogram is available in Supplementary image 2A. The estimated concentration of PTX in tested conjugate was about 107  $\mu$ g/ml. Increasing the PTX concentration to 545  $\mu$ g/ml led to saturation of PTX within the AuNPs-PTX conjugate and traceable amount of PTX could be detected in supernatant (Supplementary image 2B).



Figure 5. Determination of free PTX remaining in supernatant after preparation of FP (starting concentration of PTX 107  $\mu$ g/ml, blue line). Chromatogram of standard solution of PTX (20  $\mu$ g/ml, black line) is given for the comparison.

Based on the HPLC results, we conclude that all the PTX (in concentration used in FP) was fully associated with the AuNPs. Applying approximately five times higher concentration of PTX saturated the AuNPs surface.

### **Electrophoresis**

For final confirmation of the conjugation of different concentrations of antimiR-135b with AuNPs, the pellets of the conjugates were analyzed by agarose gel electrophoresis which all showed oligonucleotide presence and a migration delay of the conjugates compared to the free control antimir-135b (Figure 6).



Figure 6. Confirmation of the antimiR-135b - AuNPs conjugation. Different concentrations of antimir-135b are shown. 1) MassRuler low range DNA ladder, 2) control antimiR-135b (100 mM), 3) AuNPs-50 mM of antimiR-135b, 4) AuNPs-40 mM of antimiR-135b, 5) AuNPs-30 mM of antimiR-135b, 6) AuNPs-20 mM of antimiR-135b, 7) FP.

RNA electrophoresis showed detectable oligonucleotide (antimir-135b) band in AuNPs conjugates as well as visible migration delay of the antimiR when conjugated with AuNPs. These data are in agreement with our previous study [34] where we reported that AuNPs have the ability to directly conjugate with different types of nucleic acids, including short single stranded RNAs such as antimir-135b.

#### Cytotoxicity assay

PTX is a component of the FP that is known for its cytotoxic effect towards cancer cells. To evaluate PTX – mediated toxicity of the conjugates in cancer cells and non-cancerous fibroblasts, we used the equal amount of free PTX that was detected within the FP. We found that although both cell lines were inhibited by the FP, it was more notable in the 4T1 cancer cells than for the NIH/3T3 fibroblasts cells. The sensitivity of both cell lines to free control PTX was the same but the sensitivity of the cancer cells to the PTX within the FP was higher than in the case of fibroblast. We conclude that the FP was more effective to interact with, internalize, and transfect the 4T1 cancer cells because of its tumor targeting properties (e.g. transferrin ligand). Figure 7 shows calculated viability for the FP and PTX treatments in each cell line (averages of nine replicates). The calculated averages of replicates (including appropriate IC50) obtained from the difference between absorbance at 570 nm compared to reference wavenumber (i.e., 630 nm) are listed in a Supplementary table 2.



Figure 7. Logarithmic trendline presenting PTX – mediated toxicity with respect to its free form (PTX) or conjugation within FP. Viability (% of non-treated control) for cancer cell line 4T1 and non-cancerous fibroblasts NIH/3T3 is shown.

### Evaluation of FP conjugate in vivo

In order to test applicability of the FP conjugate *in vivo*, we developed breast tumors in Balb/c mouse model (Figure 8A). Once the tumors reached about 0.5cm, we performed treatment with FP as well as AuNPs and PTX alone, and PBS. The groups treated with AuNPs and PTX alone served as controls for effect judgement of the individual components. The group that obtained PBS represented non-treated control. All groups received treatment or PBS in the same time in three consecutive doses. One hour after administration of the last dose, one animal from each group was sacrificed (here referred to as the group I). Five days after administration of the last dose, remaining animals were sacrificed (here referred to as the group II). Tumors obtained from sacrificed animals were measured and further analyzed. Figure 8B shows tumors excised from group I. In general, these tumors were smaller than those obtained from group II (in group II, the tumors could continue growing). Tumor samples obtained from group I were used solely to check the successful application od nanoparticles and their immediate uptake by tumor tissue. The application sites in the case of AuNPs and FP can be detected visually since the nanoparticles retain their crimson/violet color even after *in vivo* application (Figure 8B). To confirm prompt AuNP infiltration into tumor tissue, TEM analysis was used.

Tumors samples of group II underwent the same visual check of AuNPs application (Figure 8C). The AuNPs were still well visible in tumors that received AuNPs alone as well as FP and the colorful spots especially in AuNPs parallel were larger in comparison to samples from group I. This may point out further penetration of the AuNPs into tumor tissue. Tumors excised from experimental group II were compared regarding to size (Figure 8D). There are three tumors in PBS group in contrast to the other groups because one animal died before the end of experiment.



Figure 8. Tumor growth evaluation *in vivo*. A) developed breast cancer in Balb/c mice, B) tumors excised from experimental group I. C) tumors excised from experimental group II, D) comparison of estimated tumor volume in animals from group II. Red arrows indicate AuNPs.

As presented in Figure 8D, tumor tissue volume (from group II) was not significantly reduced after treatment with FP, AuNPs, or PTX, when compared to PBS group. The ANOVA with post-hoc Tukey HSD test showed there is no significant difference between the test groups (in all groups p-value > 0.05). PTX is a cytostatic drug that leads to tumor death and thus volume reduction. However, in our setup, we used sub IC<sub>50</sub> concentration of the drug to avoid rapid death of tumor cells. That way we could learn about the FP internalization and its subsequent effect on surviving tumor cells. In the FP samples from experimental group II, we performed H

& E staining to evaluate tumor structure and cell types distribution and qPCR to evaluate inhibition of target microRNA-135b in cancer cell cytoplasm.

### AuNPs infiltration into tumor tissue in vivo confirmed by TEM and EDS analyses

Group I tumor tissue was analyzed using TEM. Although mice were sacrificed 1 hour after administration of the last dose (group I) to evaluate early infiltration of AuNPs into tumor mass and likelihood of AuNPs agglomeration. In both experimental groups (I and II), the nanoparticles accumulated in several spots on the outside of tumor (Figure 8B and 8C) and thus their agglomeration could occur.

The AuNPs were able to enter the cells in both treatments' groups (AuNP alone and FP) and were seen in the cytoplasm, endosome, late endosome or lysosome, and even in the mitochondrion and endoplasmic reticulum (ER). Representative images are shown in Figure 9. To prove that the particles seen were AuNP, a simultaneous EDS analysis was performed and Au content was confirmed (Figure 9C and 9F). The AuNPs were observed singly or in clusters in both treatment groups (AuNPs and FP). We found potential agglomeration in the endolysosome, vesicles possessing a low pH. This observation confirmed our previous report regarding agglomeration of the AuNPs in low pH [16]. Since at the same time, the AuNPs were seen also singly in the endolysosome, further analysis is necessary to elucidate that observation (e.g., by assessing the presence of AuNPs in the extracellular vesicles). We hypothesize that releasing the cargo from AuNP core in FP samples in response to low pH, results into exposing the capping agent. Due to low pH, that capping agent (as well as the one in AuNP samples) undergoes via molecules reorganization, shifting surface charge, and partial or complete aggregation.





Figure 9. TEM and EDS analyses showing penetration of AuNPs alone and FP into tumor tissue one hour after completion of treatment (experimental group I). A) Distinguishable AuNPs from the AuNP parallel were seen individually and within the mitochondrion (white arrow, scale bar = 500 nm and insert = 200 nm). B) Selected areas for EDS analysis (scale bar = 500 nm). C) EDS analysis of areas 009 (blue) and 011 (red) from part B. D) Distinguishable AuNPs from the FP parallel were seen individually or in clusters within the endolysosome (white arrows show AuNPs inside the electron dense lysosome, scale bar = 500 nm and insert = 200 nm). E) Selected areas for EDS analysis (scale bar = 500 nm). F) EDS analysis of areas 002 (blue) and 003 (red) from part E. G) AuNPs found within endoplasmic reticulum in AuNP parallel (white arrow, scale bar = 500 nm) and H) clusters but not agglomerated AuNPs seen freely in the cytoplasm of the FP parallel (white arrow, scale bar = 200 nm).

Finally, after examining more than 2000 cell nuclei by TEM, no AuNPs were detected in the cell nuclei. This suggests that AuNPs from both treatment groups (i.e., FP and AuNP parallels) penetrated the plasma membrane but not the nuclear membrane. This observation suggests that the biological AuNPs used in this report do not likely cause genotoxicity. Further analysis is required to confirm this result.

### Histology analysis of the tumor tissues evaluated by the H & E staining

Tumor growth depends on the balance between cell proliferation and cell death [35] and particularly cells undergoing programmed cell death (i.e. apoptosis, necroptosis, ferroptosis, entosis, and pyroptosis) [36] remain in the tumor tissue till their disintegration. Tumor-driven deregulation of apoptosis, which is the most studied programmed cell death, promotes cancer metastasis [37, 38]. PTX, that we used in our study, induces apoptotic cell death in tumor cells and stops the cell cycle by binding to microtubules [39]. To evaluate effect of the FP with respect to induction of cell death including apoptosis, we used sub  $IC_{50}$  doses of PTX in our setup. The applied PTX dose does not trigger excessive necrosis of the tumor tissue as confirmed by minimal changes in tumor size (Figure 8D). The sub  $IC_{50}$  dose was effective though to induce apoptosis in cancer cells as revealed by H & E staining.

Tumors obtained from animals in experimental group II were checked for changes in tissue and cell morphology by histology analysis of stained tumor sections. In the sections from the PBS-treated group of breast tumors (Figure 10 A and B), a large number of neoplastic cells are in the process of proliferation and in different stages of mitosis. Different stages of division can be seen in most of the cells present (green arrows). Tumor cells are polymorphic and undifferentiated and often have irregular and hyperchromatic as well as basophilic nuclei and little cytoplasm (white arrow). The presence of necrotic and apoptotic tissue or cellular areas is low and inconspicuous, but inflammatory cells are seen in low numbers and scattered in some areas of the tumor (yellow arrow).

In the sections from the AuNPs-treated group (Figure 10 C and D), compared to the group treated with PBS, the number of neoplastic cells showing a polymorphic and undifferentiated state (white arrow) and the number of neoplastic cells in the process of mitosis is reduced (green arrow). In some parts of the tumor tissue, necrotic areas can be seen (blue arrow) covered by a rim of inflammatory cells, and around which inflammatory cells are concentrated in medium numbers (yellow arrow). A very small blood accumulation can be seen in the vessels around the necrotic area (red arrow).

In the sections from the PTX-treated group (Figure 10 E and F), scattered necrotic parts are found in most tissue areas (blue arrow). The extent of inflammatory cells and the number of these cells are larger than in the previous groups (i.e., PBS and AuNPs, yellow arrow) and they are more densely arranged around the necrotic area. Neoplastic cells with polymorphism and nuclear compaction are observed less frequently (white arrow) and cells undergoing the process of mitosis are very rare. Some of the cells in the necrotic area have pyknotic nuclei with

karyorrhexis and compact and small cytoplasm, which is a sign of cell apoptosis (black arrow). There is some vasodilatation and blood accumulation around the necrotic area (red arrow).

In the sections from the FP-treated group (Figure 10 G and H), necrotic areas are larger and more numerous than in the previous groups (i.e., PBS, AuNPs and PTX, blue arrow), and the number of inflammatory cells around these areas has also increased (yellow arrow). Neoplastic cells are associated with a decrease in number and polymorphism (white arrow) and a decrease in mitotic process (green arrow). The cells of the necrotic area often have pyknotic nuclei with characteristic karyorrhexis and small and unclear cytoplasm, which is a sign of increased apoptosis in the cells of this area (black arrow) and the presence of severe inflammation in the surrounding area also confirms the increased apoptosis in this area. There is some blood accumulation in various tissue areas (red arrow).





Figure 10. Microscopic images of H & E stained tumor tissue samples from different treatment groups. A & B represent the PBS, C & D the AuNPs, E & F the PTX and G & H the FP groups. The magnification of A, C, E, and G is 100 x and the magnification of B, D, F, and H is 400 x. Arrows mark specific features such as mitosis (green) or bleeding (red) and they are detailed in the text.

In summary, the histology analysis revealed that treatments with PTX alone and FP remarkably decreased the number of proliferating neoplastic cells in contrast to PBS-treated samples. A small decrease in mitotic activity was found also in samples treated with AuNPs alone. On the other hand, the AuNP, PTX, and FP – treated samples exhibited a remarkably higher number of inflammatory cells as well as blood accumulation probably due to vasodilatation. The accumulation of inflammatory cells was situated around the necrotic areas. Treatments with the PTX and the FP were also characterized by presence of apoptotic cells that were localized around the necrotic areas. Since the necrotic areas were present also in samples treated with the AuNPs that did not induce remarkable apoptosis, we suggest that the formation of necrotic areas

was primarily caused by infiltration of inflammatory cells and local inflammation maybe in response to nanoparticle interaction. In the case of the PTX alone, the inflammation was likely in parallel or subsequent to apoptosis induction. The individual actions of the PTX and the AuNP were then potentiated in the FP that combines both the components. The summary of histology evaluation is shown in Table 3. The individual groups are graded with respect to specific criteria such as neoplastic, necrotic & apoptotic, and inflammatory cells and the amount of blood accumulation.

Table 3. Comparison of the groups based on the results of H & E staining according to the different criteria. The observed changes are graded from 0 to 3. Grade 0 means no change, grade 1 means slight change, grade 2 means moderate change, and grade 3 means severe.

Groups treated by	Inflammatory cells & amount of	Necrotic & apoptotic cells	Neoplastic cells		
	blood accumulation				
BPS	0	0	3		
AuNPs	1	1	2		
PTX	2	2	1		
FP	3	3	1		

## Assessment of antimiR-135b activity and reduction of oncogenic miR-135b in tumor cells

AntimiR-135b was designed to specifically bind to oncogenic miR-135b in tumor cells and promote its degradation. To assess the effectivity of antimir-135b cytoplasmic delivery and its ability to bind its target, we compared miR-135b levels in tumors treated with PBS and the AuNPs, PTX, or FP. As a positive control of the qPCR analysis, we used samples treated with antimir-135b delivered into cells using a commercial transfection reagent (HP; X-tremeGENE transfection reagent from Sigma-Aldrich). The levels of miR-135b quantified with a qPCR were normalized to internal control miR-16. Significance of the miR-135b reduction was calculated with ANOVA group comparison with Tukey post hoc test. Since the AuNP carriers were not equally distributed throughout the entire tumor tissue, we analyzed amount of Au in the homogenates with a GF-AAS. The amount of each homogenate used for RNA extraction was then equalized to 49 ng of Au.



Figure 11. MiR-135b levels in tumors treated with FP that comprised inhibitory sequence antimir-135b designed to specifically degrade the miR-135. Samples treated with PBS served as controls without effect on mir-135b levels. HP served as positive control of miR-135b silencing. Values of  $p \le 0.01$  (\*\*) showed significant differences between groups. "ns" marks non-significant change.

Compared to PBS group, a significant decrease of miR-135b was detected in samples treated with FP (p value  $\leq 0.01$ ), AuNPs (p value  $\leq 0.01$ ), and PTX (p  $\leq 0.01$ ). We also checked the differences in miR-135b reduction among the FP and the individual components like AuNPs and PTX. We found significantly stronger reduction of the miR-135b level after FP treatment in comparison to the solely PTX treatment (p value  $\leq 0.01$ ). The difference between tumors treated by solely AuNPs and tumors treated with FP was not significant (p value = 0.107). We suggest that FP entered tumor cells and delivered antimiR-135b to cytoplasm. Since the antimir-135b was able to bind and degrade the miR-135, we expect the antimir-135b to be released from the FP and that its loading and unloading from the AuNP carriers did not affect the structure and function of the antimiR-135b molecule. These results agree with our previous studies on antimir-135b delivery by functionalized nanodiamond carriers. We suspect similar mechanism of nanocarrier entry and cargo released as described by our group [22, 40]. However, this assumption has to be proved since the biologically produced nanoparticles are unique type nanocarrier and their ability to transport effector RNA hasn't been studied yet. The qPCR also confirmed that the FP has higher efficacy in miR-135b reduction than the individual

components (PTX and AuNPs). While the miR-135b reduction by PTX was expected due to its complex anticancer effect, the reduction of miR-135b by solely AuNPs was unexpected. Independently, we observed alteration of cancer-associated proteins as a response of 4T1 tumor cells to biologically produced AuNPs in our subsequent study (data not shown, manuscript in preparation). It seems that AuNPs may induce some anticancer activity in breast cancer cells and the down-regulation of oncogenic miRNA-135b could be one of the effector mechanisms. More exploration in this field is necessary though to understand this phenomenon.

In this study, we prepared AuNPs using the fungal strain and conditions that we developed previously [14, 15]. Many characteristics of the AuNPs (the maximum absorption peak at 528 nm, round shape, average size of 15 nm, and zeta potential of -35 mV), produced in different batches in different time were consistent [12-16, 18, 19, 41]. It confirms the ability of the fungus to reliably produce similar AuNPs and obtain reproducible data.

Presented data showed that the AuNPs were able to bind to PTX, antimiR-135b, and Tf, both individually, and simultaneously. The AuNPs were stable when conjugated with different cargos and their size stayed under 100 nm. The stability of the FP was even higher compared to AuNPs-PTX, which was probably due to presence of other cargoes (i.e. Tf and RNA) contributing to the stabilization of the complex. For example, antimiR-135b with its negative charge improved the stability and overall net charge of FP (-38.84 mV in AuNPs-antimiR *versus* -30.2 mV in AuNPs-PTX, -35.6 mV in AuNPs-Tf, and -31.9 mV in FP).

Using tumor specific ligand – transferrin, Tf - for decoration of the FP led to higher specificity of the FP towards tumor cells as shown in cytotoxicity tests. Here, the 4T1 cells were more inhibited by FP than NIH/3T3 cells, which may be due to the 1) overexpression of Tf receptor on the surface of 4T1 cells [41] and confirming the tumor-targeting properties of FP and 2) higher growth rate of 4T1 compared to NIH/3T3 cells sensitizing the 4T1 cells to the toxic effect of FP.

Final application of the FP *in vivo* using the 4T1 syngeneic tumor model showed important aspects of the AuNPs as drug carriers. To reduce the number of experimental animals according to the 3R strategy, Czech Animal Protection Act no 246/1992, we performed the *in vivo* study with the complex FP conjugate and controls consisting of the main components (AuNPs, PTX). The FP applied peritumorally exhibited good penetration into the tumor tissue followed by inflammatory response, apoptosis, and necrosis in the tissue adjacent to application sites. At the molecular level we observed successful inhibition of target miR-135b in tumor cells. Since the miR-135b is present in cytoplasm, the FP conjugate had to enter the cell and unload the antimir-

135b cargo into cytoplasm. The exact mechanism of internalization and potential release of the AuNP - based conjugate from internalizing vesicles such as endosomes needs to be further revealed. It remains unclear if the FP stayed stable and traveled into cytosol functionalized will all the decorative molecules including antimir-135b or the molecules were at least partially released already in transport vesicles as we found in the case of nanodiamond carriers [40].

Location of AuNPs within the cell was uncovered by TEM. The AuNPs were located in the organelles such as the mitochondrion and ER, but not in the nuclei. This suggests that the mechanism of internalization of the biologically produced AuNPs through the plasma membrane differs from the mechanism of internalization through the nuclear membrane (which is mainly through nuclear pore complexes (NPCs) [42]. The absence of AuNPs in nuclei is favorable because 1) FP must be translocated to the cytosol where target miR-135b is located, and 2) it decreases the possibility of FP-mediated genotoxicity. Regarding mean of internalization, we expect the FP entered cells via the clathrin-mediated endocytosis pathway due to Tf present on its surface [43]. Moreover, the AuNPs (including those within the FP conjugate) were located in endolysosomes as observed by TEM. It is a question if part of the AuNP carriers escaped the endosomes and delivered antimir-135b into cytoplasm or if the short RNA was released from the carrier and transported to cytoplasm during the endosome maturation endolysosomes. The physicochemical properties of nanocarriers, such as size, shape, surface charge and surface coating, as well as the amounts of individual molecules, are important for their fate in cells [44, 45]. For example, clathrin-independent endocytosis was observed in the case of folic acid, whereas clathrin-dependent and -independent endocytosis was observed in the case of folic acid-conjugated NPs [45]. The non-biological AuNPs were reported to be localized in the subcellular vesicles and rarely within the organelles or cytosol [44]. On the other hand, the biologically produced AuNPs with capping agent and multiple functionalization, the FPs, used in this study were observed within organelles and cytosol. Approaches to promote the internalization of nonbiological AuNPs in the cytoplasm were made and involved conjugation of dynein-binding peptides or cell-penetrating peptides (CPPs) to the surface of AuNPs [46, 47] or conjugation of TAT and HA2, two viral proteins, to the surface of AuNPs [48].

Endosomal escape seems like a major limitation in successful drug delivery. The attempts to disrupt and bypass the endosomal pathway involved direct methods such as microinjection, direct translocation, use of bacterial pore-forming toxins or electroporation, and indirect methods such as lysis of the endosome using drugs or osmotic shock [48]. The FP tested in the

current study passed through the endosomal pathway and delivered cargo i.e. PTX and antimiR into the cytoplasm. We are aware that Tf helps the conjugate to find target cells and enter them by endocytosis [49], but whether Tf helped the AuNP conjugates to overcome endosomal barrier by passing the trans-Golgi network (TGN), then ER and finally the cytosol [50, 51] has to be analyzed in the future. We also consider passive diffusion (i.e., direct penetration) [52] of FP into the cytosol.

### Conclusion

In the current study, we prepared and successfully tested a multifunctional drug delivery agent based on biologically produced AuNPs. AuNPs were able to conjugate directly with various cargoes. This is due to their "capping agents", which are likely polypeptides or amino acids that can bind to different types of cargoes due to their polar properties. The high load capacity of biologically produced AuNPs for various molecules makes them a good candidate for transporting drugs and/or genes into target cells. In this study, we showed that the FP containing PTX, Tf, and antimiR-135b could reduce cell survival better than the same concentration of PTX as control *in vitro*. The results confirmed the ability of FP to penetrate the tumor, induce cell death and inflammation, and regulate gene expression *in vivo*. It seems that AuNPs serve as multifunctional carriers for targeted therapy and detailed investigation with respect to internalization of the biologically produced AuNPs is needed and we plan to perform it in our future studies.

### Acknowledgement

This work was supported by MSCA Fellowships CZ (Institute of Microbiology of the CAS, v. v. i.) No. CZ.02.01.01/00/22\_010/0002357. We acknowledge CMS-Biocev ("Biophysical techniques, Crystallization, Diffraction, Structural mass spectrometry") of CIISB, Instruct-CZ Centre. supported MEYS CR (LM2023042) ERDF by and (CZ.02.1.01/0.0/0.0/18 046/0015974). We would like to thank Petr Pompach, a scientist in charge of the mass spectroscopy service, who analyzed our samples by LC MS and Miroslav Kolařík, head of the laboratory fungal genetics and metabolism for help with fungal cultivation. We acknowledge the Electron Microscopy Core Facility, IMG CAS, Prague, Czech Republic, supported by MEYS CR (LM2023050 Czech-BioImaging) and **ERDF** (CZ.02.1.01/0.0/0.0/18 046/0016045) for their support with obtaining TEM data presented in this paper. The authors thank the Core of Cytometry and Microscopy, Institute of Microbiology CAS for their support with microscopy measurements and the Institute of Analytical Chemistry of CAS, v.v.i. supported by Institutional Research Plan RVO: 68081715. We acknowledge the Histology Laboratory, IMG, Prague, Czech Republic for assistance with processing, sectioning, and staining of the tissues presented here.

### References

- [1] A. G. Waks and E. P. Winer, "Breast cancer treatment: a review," *Jama*, vol. 321, no. 3, pp. 288-300, 2019.
- [2] S. Lei *et al.*, "Global patterns of breast cancer incidence and mortality: A population-based cancer registry data analysis from 2000 to 2020," *Cancer Communications*, vol. 41, no. 11, pp. 1183-1194, 2021.
- [3] H.-C. Wu, D.-K. Chang, and C.-T. Huang, "Targeted therapy for cancer," *J Cancer Mol*, vol. 2, no. 2, pp. 57-66, 2006.
- [4] Y. Li, Y. Gao, X. Zhang, H. Guo, and H. Gao, "Nanoparticles in precision medicine for ovarian cancer: From chemotherapy to immunotherapy," *International Journal of Pharmaceutics,* p. 119986, 2020.
- [5] J. Wang and B. Xu, "Targeted therapeutic options and future perspectives for HER2-positive breast cancer," *Signal transduction and targeted therapy*, vol. 4, no. 1, p. 34, 2019.
- [6] H. L. Perez *et al.*, "Antibody–drug conjugates: current status and future directions," *Drug discovery today*, vol. 19, no. 7, pp. 869-881, 2014.
- [7] D. Zardavas, A. Irrthum, C. Swanton, and M. Piccart, "Clinical management of breast cancer heterogeneity," *Nature reviews Clinical oncology*, vol. 12, no. 7, pp. 381-394, 2015.
- [8] K. C. Wood, "Mapping the pathways of resistance to targeted therapies," *Cancer research,* vol. 75, no. 20, pp. 4247-4251, 2015.
- [9] P. S. Huang and A. Oliff, "Drug-targeting strategies in cancer therapy," *Current Opinion in Genetics & Development*, vol. 11, no. 1, pp. 104-110, 2001.
- [10] K. L. Vine, S. Lobov, V. I. Chandran, N. L. E. Harris, and M. Ranson, "Improved pharmacokinetic and biodistribution properties of the selective urokinase inhibitor PAI-2 (SerpinB2) by sitespecific PEGylation: implications for drug delivery," *Pharmaceutical research*, vol. 32, no. 3, pp. 1045-1054, 2015.
- [11] B. Yahyaei, M. Nouri, S. Bakherad, M. Hassani, and P. Pourali, "Effects of biologically produced gold nanoparticles: toxicity assessment in different rat organs after intraperitoneal injection," *AMB Express*, vol. 9, no. 1, pp. 1-12, 2019.
- [12] P. Pourali, S. H. Badiee, S. Manafi, T. Noorani, A. Rezaei, and B. Yahyaei, "Biosynthesis of gold nanoparticles by two bacterial and fungal strains, Bacillus cereus and Fusarium oxysporum, and assessment and comparison of their nanotoxicity in vitro by direct and indirect assays," *Electronic Journal of Biotechnology*, vol. 29, pp. 86-93, 2017.
- [13] P. Pourali, B. Yahyaei, and S. Afsharnezhad, "Bio-Synthesis of Gold Nanoparticles by Fusarium oxysporum and Assessment of Their Conjugation Possibility with Two Types of β-Lactam Antibiotics without Any Additional Linkers," *Microbiology (00262617)*, vol. 87, no. 2, 2018.
- [14] P. Pourali, V. Dzmitruk, M. Pátek, E. Neuhöferová, M. Svoboda, and V. Benson, "Fate of the capping agent of biologically produced gold nanoparticles and adsorption of enzymes onto their surface," *Scientific Reports*, vol. 13, no. 1, p. 4916, 2023/03/25 2023, doi: 10.1038/s41598-023-31792-5.
- [15] P. Pourali, E. Neuhöferová, V. Dzmitruk, and V. Benson, "Investigation of Protein Corona Formed around Biologically Produced Gold Nanoparticles," *Materials*, vol. 15, no. 13, p. 4615, 2022.
- [16] P. Pourali, O. Benada, M. Pátek, E. Neuhöferová, V. Dzmitruk, and V. Benson, "Response of Biological Gold Nanoparticles to Different pH Values: Is It Possible to Prepare Both Negatively and Positively Charged Nanoparticles?," *Applied Sciences*, vol. 11, no. 23, p. 11559, 2021.
- [17] P. Pourali *et al.*, "The effect of temperature on antibacterial activity of biosynthesized silver nanoparticles," *Biometals*, vol. 26, no. 1, pp. 189-196, 2013.
- [18] B. Yahyaei and P. Pourali, "One step conjugation of some chemotherapeutic drugs to the biologically produced gold nanoparticles and assessment of their anticancer effects," *Scientific reports,* vol. 9, no. 1, pp. 1-15, 2019.

- [19] N. Naimi-Shamel, P. Pourali, and S. Dolatabadi, "Green synthesis of gold nanoparticles using Fusarium oxysporum and antibacterial activity of its tetracycline conjugant," *Journal de mycologie medicale,* vol. 29, no. 1, pp. 7-13, 2019.
- [20] N. Roy, A. Gaur, A. Jain, S. Bhattacharya, and V. Rani, "Green synthesis of silver nanoparticles: an approach to overcome toxicity," *Environmental toxicology and pharmacology*, vol. 36, no. 3, pp. 807-812, 2013.
- [21] M. Składanowski, P. Golinska, K. Rudnicka, H. Dahm, and M. Rai, "Evaluation of cytotoxicity, immune compatibility and antibacterial activity of biogenic silver nanoparticles," *Medical microbiology and immunology*, vol. 205, no. 6, pp. 603-613, 2016.
- [22] R. Křivohlavá, E. Neuhöferová, K. Q. Jakobsen, and V. Benson, "Knockdown of microRNA-135b in mammary carcinoma by targeted nanodiamonds: potentials and pitfalls of in vivo applications," *Nanomaterials,* vol. 9, no. 6, p. 866, 2019.
- [23] P. Uva *et al.*, "miRNA-135b contributes to triple negative breast cancer molecular heterogeneity: Different expression profile in Basal-like versus non-Basal-like phenotypes," *International Journal of Medical Sciences*, vol. 15, no. 6, p. 536, 2018.
- [24] K. Hua *et al.*, "miR-135b, upregulated in breast cancer, promotes cell growth and disrupts the cell cycle by regulating LATS2," *International journal of oncology*, vol. 48, no. 5, pp. 1997-2006, 2016.
- [25] P. Pourali, B. Yahyaei, and S. Afsharnezhad, "Bio-synthesis of gold nanoparticles by Fusarium oxysporum and assessment of their conjugation possibility with two types of β-lactam antibiotics without any additional linkers," *Microbiology*, vol. 87, no. 2, pp. 229-237, 2018.
- [26] P. Kesarwani, R. K. Tekade, and N. Jain, "Spectrophotometric estimation of paclitaxel," International Journal of Advances in Pharmaceutical Sciences, vol. 2, no. 1, 2011.
- [27] Z. Pavelek *et al.*, "Proteomic analysis of cerebrospinal fluid for relapsing-remitting multiple sclerosis and clinically isolated syndrome," *Biomedical reports*, vol. 5, no. 1, pp. 35-40, 2016.
- [28] E. Prochazkova *et al.*, "NMR Structure Elucidation of Naphthoquinones from Quambalaria cyanescens," *J. Nat. Prod.*, vol. 84, no. 1, pp. 46-55, 2020.
- [29] C. J. Ackerson, M. T. Sykes, and R. D. Kornberg, "Defined DNA/nanoparticle conjugates," *Proceedings of the National Academy of Sciences*, vol. 102, no. 38, pp. 13383-13385, 2005.
- [30] H.-Q. Wang and Z.-X. Deng, "Gel electrophoresis as a nanoseparation tool serving DNA nanotechnology," *Chinese Chemical Letters,* vol. 26, no. 12, pp. 1435-1438, 2015.
- [31] M. Hazekawa, T. Nishinakagawa, T. Kawakubo-Yasukochi, and M. Nakashima, "Evaluation of IC50 levels immediately after treatment with anticancer reagents using a real-time cell monitoring device," *Experimental and therapeutic medicine,* vol. 18, no. 4, pp. 3197-3205, 2019.
- [32] C. Li *et al.*, "Antitumor activity of poly (L-glutamic acid)-paclitaxel on syngeneic and xenografted tumors," *Clinical cancer research*, vol. 5, no. 4, pp. 891-897, 1999.
- [33] P. Pourali *et al.*, "Histopathological study of the maternal exposure to the biologically produced silver nanoparticles on different organs of the offspring," *Naunyn-Schmiedeberg's Archives of Pharmacology*, vol. 393, no. 5, pp. 867-878, 2020.
- [34] P. Pourali, V. Dzmitruk, O. Benada, M. Svoboda, and V. Benson, "Conjugation of microbialderived gold nanoparticles to different types of nucleic acids: evaluation of transfection efficiency," *Scientific Reports,* vol. 13, no. 1, p. 14669, 2023.
- [35] J. De Jong, P. J. van Diest, and J. Baak, "Number of apoptotic cells as a prognostic marker in invasive breast cancer," *British journal of cancer*, vol. 82, no. 2, pp. 368-373, 2000.
- [36] E. Koren and Y. Fuchs, "Modes of regulated cell death in cancer," *Cancer discovery*, vol. 11, no. 2, pp. 245-265, 2021.
- [37] Z.-g. Liu and D. Jiao, "Necroptosis, tumor necrosis and tumorigenesis," *Cell stress,* vol. 4, no. 1, p. 1, 2020.
- [38] G. M. Calaf, R. Ponce-Cusi, and F. Carrión, "Curcumin and paclitaxel induce cell death in breast cancer cell lines," *Oncology Reports*, vol. 40, no. 4, pp. 2381-2388, 2018.

- [39] T. H. Wang, H. S. Wang, and Y. K. Soong, "Paclitaxel-induced cell death: where the cell cycle and apoptosis come together," *Cancer: Interdisciplinary International Journal of the American Cancer Society*, vol. 88, no. 11, pp. 2619-2628, 2000.
- [40] Lukowski S. et al. "Fluorescent Nanodiamonds are Efficient, Easy-To-Use Cyto-Compatible Vehicles for Monitored Delivery of Non-Coding Regulatory RNAs." J Biomed Nanotechnol, vol. 14, pp. 1–13, 2018.
- [41] B. Yahyaei, P. Pourali, and M. Hassani, "Morphological Change of Kidney after Injection of the Biological Gold Nanoparticles in Wistar Rats," *Journal of Animal Biology*, vol. 13, no. 1, pp. 109-119, 2020.
- [42] A. Chaumet, G. D. Wright, S. H. Seet, K. M. Tham, N. V. Gounko, and F. Bard, "Nuclear envelope-associated endosomes deliver surface proteins to the nucleus," *Nature communications*, vol. 6, no. 1, p. 8218, 2015.
- [43] I. M. Degors, C. Wang, Z. U. Rehman, and I. S. Zuhorn, "Carriers break barriers in drug delivery: endocytosis and endosomal escape of gene delivery vectors," *Accounts of chemical research*, vol. 52, no. 7, pp. 1750-1760, 2019.
- [44] E. A. Egorova, G. E. Lamers, F. A. Monikh, A. L. Boyle, B. Slütter, and A. Kros, "Gold nanoparticles decorated with ovalbumin-derived epitopes: effect of shape and size on T-cell immune responses," *RSC advances,* vol. 12, no. 31, pp. 19703-19716, 2022.
- [45] R. Daniele *et al.*, "Influence of folate-targeted gold nanoparticles on subcellular localization and distribution into lysosomes," *Pharmaceutics*, vol. 15, no. 3, p. 864, 2023.
- [46] J.-W. Yoo, D. J. Irvine, D. E. Discher, and S. Mitragotri, "Bio-inspired, bioengineered and biomimetic drug delivery carriers," *Nature reviews Drug discovery*, vol. 10, no. 7, pp. 521-535, 2011.
- [47] C. Bechara and S. Sagan, "Cell-penetrating peptides: 20 years later, where do we stand?," *FEBS letters*, vol. 587, no. 12, pp. 1693-1702, 2013.
- [48] Y. Cesbron, U. Shaheen, P. Free, and R. Levy, "TAT and HA2 facilitate cellular uptake of gold nanoparticles but do not lead to cytosolic localisation," *PLoS One,* vol. 10, no. 4, p. e0121683, 2015.
- [49] M. E. Davis *et al.*, "Evidence of RNAi in humans from systemically administered siRNA via targeted nanoparticles," *Nature*, vol. 464, no. 7291, pp. 1067-1070, 2010.
- [50] Y. Tu, L. Zhao, D. D. Billadeau, and D. Jia, "Endosome-to-TGN trafficking: organelle-vesicle and organelle-organelle interactions," *Frontiers in cell and developmental biology*, vol. 8, p. 163, 2020.
- [51] I. Le Blanc *et al.*, "Endosome-to-cytosol transport of viral nucleocapsids," *Nature cell biology*, vol. 7, no. 7, pp. 653-664, 2005.
- [52] S. Behzadi *et al.*, "Cellular uptake of nanoparticles: journey inside the cell," *Chemical society reviews*, vol. 46, no. 14, pp. 4218-4244, 2017.

# Supplementary information

# Multicomponent delivery system based on biologically produced gold nanoparticles for targeted therapy of breast cancer *in vivo*

Parastoo Pourali<sup>1</sup><sup>†</sup>, Eva Neuhöferová<sup>1</sup><sup>†</sup>, Volha Dzmitruk<sup>2</sup>, Milan Svoboda<sup>3</sup>, Eva Stodůlková<sup>1</sup>,

Miroslav Flieger<sup>1</sup>, Behrooz Yahyaei<sup>4</sup> & Veronika Benson<sup>1\*</sup>

# Supplementary table 1.

Hydrodynamic diameter and zeta potential of default AuNPs and AuNPs conjugated with different cargoes measured by a Zetasizer. Individual measurements used for statistical analyses.

Tested material	Parameter / Repeat	1	2	3	4	5	Mean	SD
	Hydrodynamic diameter (nm)	11	13	15.2	13	13	13.04	<u>+</u> 1.33
AuNPs	Zeta potential (mV)	-35.1	-34.64	-35.7	-35.8	-37.7	-35.8	<u>+</u> 1.17
	Hydrodynamic diameter (nm)	68.7	59.1	64	68.7	79.9	68.1	<u>+</u> 7.71
AuNPs-Tf	Zeta potential (mV)	-35.5	-34.1	-33.6	-37.3	-35.6	-35.2	<u>+</u> 1.45
AuNPs-PTX	Hydrodynamic diameter (nm)	59.1	59.1	79.9	79.9	68.7	69.3	<u>+</u> 10.41
	Zeta potential (mV)	-27.6	-29.7	-31.5	-30.7	-31.7	-30.2	<u>+</u> 1.67
AuNPs-	Hydrodynamic diameter (nm)	28	38	32	32	32	32.4	<u>+</u> 3.2
antimiR	Zeta potential (mV)	-38.1	-42.7	-37.2	-38.1	-38.1	-38.84	<u>+</u> 1.97
	Hydrodynamic diameter (nm)	68.7	63	43.7	37.6	68.7	54.2	<u>+</u> 14.10
FP	Zeta potential (mV)	-28.3	-32.1	-33	-32.8	-33.4	-31.9	<u>+</u> 2.08

# Supplementary figure 1.

A) Color change observation after conjugation of AuNPs with different cargoes.

B - D) Standard curves of Tf, antimiR-135b, and PTX that served for the load estimate of individual component within AuNP conjugates.



### **Supplementary figure 2.**

A) Determination of free PTX remaining in supernatant after preparation of nanoparticles (starting concentration of PTX 107  $\mu$ g/ml, blue line). Chromatogram of standard solution of PTX (20  $\mu$ g/ml, black line) is given for the comparison.

B) Determination of free PTX remaining in supernatant after preparation of nanoparticles (starting concentration of PTX 545  $\mu$ g/ml, black line). Chromatogram of standard solution of PTX (20  $\mu$ g/ml, blue line) is given for the comparison.



### Supplementary table 2.

The calculated averages of the replicates obtained from the difference between absorbance at 570 nm compare to reference wavenumber (i.e., 630 nm).  $IC_{50}$  for each sample is determined and showed with \* sign. The rows are: A) FP in 4T1 cell line 0.6575, B1-B9) free PTX in 4T1 cell line 0.6601. B12) 4T1 cells without any treatment. C) FP in NIH/3T3 cell line 0.8103, D1-D9) free PTX in NIH/3T3 cell line 1.0884. D12) NIH/3T3 cells without any treatment.

Row/well	1	2	3	4	5	6	7	8	9	10	11	12
А	0.238	0.0611	0.0734	0.1303	0.3774	$0.6575^{*}$	0.7899	0.800	0.7021	0.742	0.6934	0.7623
В	0.1258	0.2558	0.6601*	0.7836	0.7252	0.8438	0.9318	0.801	0.8214	0.830	0.830	0.830
С	0.1902	0.3280	0.5210	0.8103*	1.1895	1.2285	1.3851	1.533	1.1949	1.327	1.156	1.216
D	0.14995	0.50375	1.0884*	1.34465	1.3197	1.3563	1.2812	1.4356	1.1990	0.830	0.830	1.2121