Breaking isolation to form new networks: pH triggered changes in connectivity inside lipid nanoparticles

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18	KEYWORDS Lyotropic liquid crystals, hexosomes, micellosomes, pH-response, lipid
19	nanoparticles, SAXS, cryo-TEM, stimuli-responsive.

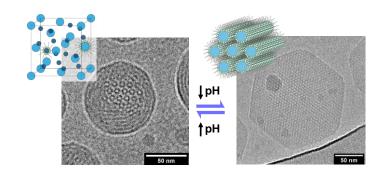
20 ABSTRACT

21 There is a growing demand to develop smart nanomaterials that are structure-responsive as they 22 have the potential to offer enhanced dose, temporal and spatial control of compounds and chemical 23 processes. The naturally occurring pH gradients found throughout the body make pH an attractive 24 stimulus for guiding the response of a nanocarrier to specific locations or (sub)cellular 25 compartments in the body. Here we have engineered highly sensitive lyotropic liquid crystalline 26 nanoparticles that reversibly respond to changes in pH by altering the connectivity within their 27 structure at physiological temperatures. At pH 7.4, the nanoparticles have an internal structure 28 consisting of discontinuous inverse micellar 'aqueous pockets' based on space group Fd3m. When 29 the pH is ≤ 6 , the nanoparticles change from a compartmentalized to an accessible porous internal 30 structure based on a 2D inverse hexagonal phase (plane group p6mm). We validate the internal 31 symmetry of the nanoparticles using Small Angle X-ray Scattering and cryogenic Transmission 32 Electron Microscopy. The high resolution electron microscopy images obtained have allowed us 33 for the first time to directly visualize the internal structure of the Fd3m nanoparticles and resolve 34 the two different-sized inverse micelles that make up the structural motif within the Fd3m unit 35 cell, which upon structural analysis reveal excellent agreement with theoretical geometrical 36 models.

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44 **TOC**



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46 **INTRODUCTION**

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48 Lyotropic liquid crystalline nanoparticles (LCNPs) have attracted enormous interest for 49 applications such as drug delivery, nanoreactor arrays, biosensors, templating, advanced 50 biomaterials and functional foods. These particles have non-lamellar internal nanostructrures that 51 possess two- or three-dimensional periodicity. LCNPs with internal nanostructures based on 52 inverse bicontinuous cubics (Q_{II}), 2D-hexagonal (H_{II}) or ordered micellar phases are termed 53 cubosomes, hexosomes and micellosomes respectively. They offer potential advantages over 54 current nanoformulations, including favourable payloads due to their high internal surface area, 55 simple preparation protocols, superior ease of conjugation with target biomolecules, 56 biodegradability of the host building blocks and the ability to encapsulate hydrophobic, hydrophilic and amphiphilic substances.¹⁻⁶ 57

58 Currently there is a large demand to develop smart nanocarriers that can respond to particular 59 environmental stimuli which could be used to release an active at a specific site of action and hence 60 minimize off target toxicity and unwanted side effects. Extrinsic factors such as ultrasound, 61 temperature, magnetic fields and light have been explored to trigger a response however these can 62 only be controlled via external sources.⁷ On the contrary, one can harness intrinsic stimuli such as enzymes overexpressed at disease sites or variations in pH throughout the body, such as that found
in the stomach, or the more acidic extracellular microenvironment of tumor cells compared to
healthy tissue. ⁸⁻¹⁰ Acidic environments are also present in other organs/organelles such as the skin
surface where the pH is around 4-6.5,¹¹ <4 in the gastric phase,¹² and between 4.5-6.5 in the
lysosomal and endosomal lumen,¹³ while the pH in the serum is 7.4. Acidic pH is also used *in vivo*to trigger processes such as protein-ligand binding and viral fusion.¹⁴

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Whilst the majority of pH responsive systems have been focused on polymers,¹⁵⁻¹⁶ LCNPs are 70 mainly made up of biological amphiphiles rendering them more biocompatible and less cytotoxic.⁶, 71 ¹⁷⁻¹⁸ Non-lamellar forming lipids are some of the most common building blocks to generate inverse 72 73 lyotropic liquid crystalline phases as they can form a variety of structures depending on composition, thermodynamic variables, pH and other parameters.¹⁹⁻²¹ The resulting phase behavior 74 75 is also dependent on the geometric packing of the lipids and can be tuned by increasing the 76 concentration of more strongly curved lipids which will increase the negative spontaneous 77 curvature towards the water and form phases with increasing negative interfacial curvature. 78 (Figure 1a). For example, by increasing the fatty acid content in monoolein (MO) based systems, 79 the structure can transform from Q_{II} to H_{II} and on further addition to a discontinuous inverse micellar cubic phase of space group Fd3m.²²⁻²⁴ In an analogous fashion, the phase behavior can be 80 81 tuned by introducing ionisable lipids where the lipid headgroup can be protonated or deprotonated 82 depending on the pH and ionic strength. An increase in surface charge density will cause 83 electrostatic repulsion between headgroups, an increase of the effective headgroup area and 84 consequently a decrease in the magnitude of the spontaneous inverse curvature and the adoption 85 of less curved phases (Figure 1a). Similarly, an increase in ionic strength will enhance charge screening and hinder the transition to less curved structures. Tuning the phase behavior of these systems is attractive as the release rate of encapsulated actives from LCNPs strongly correlates with the internal nanostructure symmetry as well as, for some LCNPs, the geometry and dimensions of their pores.^{10, 25-26}

90 Most studies have focused on pH-induced transitions between lamellar (L α) and Q_{II}, or between 91 Q_{II} and H_{II} phases. A MO: linoleic acid system was developed to change from Q_{II} at pH 7 to H_{II} at pH 2 to simulate intestinal and gastric phases respectively.²⁷ Negrini *et al.* further developed a 92 93 monolinolein: pyridinylmethyl linoleate system that switched from an H_{II} to a O_{II} phase when the 94 pH was ≤ 5.5 and showed the potential therapeutic role of this targeted system in treating cancer cells by exploiting their more acidic microenvironment.²⁸ A low pH-induced L α to Q_{II} phase 95 96 transition in a MO: dioleoylphosphatidylserine system showed that the L α phase directly transformed into an H_{II}, and subsequently, the H_{II} slowly converted into a O_{II} phase.²⁹ 97

98 On the contrary, pH-triggered transitions from ordered inverse micellar phases is still in its 99 infancy. These have an internal structure consisting of discontinuous micellar 'pockets' and, unlike 100 the porous Q_{II} and H_{II} phases, these are based on a discontinuous packing of inverse micelles, 101 containing an array of individual nanoscale aqueous compartments separated by fluid hydrophobic 102 regions, which could potentially offer containment control.

Salentinig *et al.* showed that by increasing the pH from 6.8 to 9 at 25°C in MO: oleic acid (OA) dispersions, an inverse micellar solution transformed to Fd3m micellosomes, to hexosomes, to cubosomes and finally to liposomes.³⁰ Similar phase transitions from LCNPs of OA doped with the antimicrobial human cathelicidin LL-37 peptide were observed upon increasing the pH from 6 to 8 at 25°C.³¹ Recently Fong *et al.* showed that at a certain MO: fatty acid composition Fd3m micellosomes were formed in water with a pH of 4.9 and very low ionic strength. When water was replaced by PBS (pH 7.4) the micellosomes transformed to hexosomes at 30°C. This transition
was however triggered by the combination of pH and ionic concentration changes, and thus cannot
be considered a pure pH response.³²

112 In this work we aim to develop LCNPs that are switchable between the confined Fd3m and 113 porous H_{II} phases at physiologically relevant temperature and pHs, confirmed with detailed 114 structural characterization by SAXS and cryo-TEM. We designed pH-responsive LCNPs based on 115 MO and oleyl alcohol (Olalc) doped with a small amount (3 mol%) of a pH-sensitive lipid. We 116 show that these LCNPs transform from Fd3m micellosomes at pH 7.4 to hexosomes when the pH 117 is ≤ 6 . To the best of our knowledge this is the first report of a pH triggered LCNP transition from 118 Fd3m micellosomes to hexosomes with decreasing pH and compared to previous research on 119 similar transitions, our system can reversibly transform at both room (25°C) and at a biologically-120 relevant temperature (37°C). We highlight that high resolution cryo-TEM images have allowed us 121 to directly visualize the internal structure of the Fd3m nanoparticles with unprecedented detail 122 allowing us to compare the internal structures of the nanoparticles with theoretical predictions, 123 using cryo-TEM for this purpose for the first time.

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125 **RESULTS AND DISCUSSION**

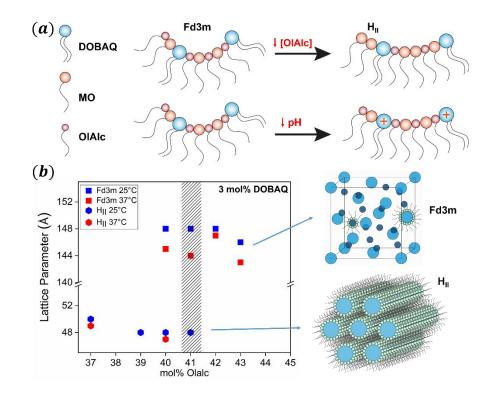
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Phase behavior of oleyl alcohol, monoolein and DOBAQ mixtures reveal an H_{II} to Fd3m transition

The phase diagram of MO in water has been widely studied;³³⁻³⁴ above the excess water point of 35 wt%, MO adopts a Pn3m bicontinuous cubic phase between approximately 20 and 80 °C, which then transforms to an inverse hexagonal (H_{II}) phase at higher temperatures. Generally, for the other pure component systems, DOBAQ forms liposomes in excess water,³⁵ whereas oleyl alcohol
 adopts an inverse micellar solution.²⁵

The phase behavior of MO with fatty acids, such as oleic acid (OA), has previously been reported: MO:OA dispersions, stabilized by the Pluronic F127 in milliQ water, typically require an excess of 50 mol% OA to form Fd3m micellosomes,^{30, 32} and when MO:OA dispersions are made in PBS at pH 7 and 100mM NaCl (above the pK^{app} of OA and hence the OA is negatively charged), over 80 mol% oleic acid is required to form the Fd3m phase.³⁶

139 Here, we have chosen to study mixtures of monoolein with oleyl alcohol, which is structurally 140 similar to OA but is not ionisable, doped with a small amount of the pH-sensitive lipid N-(4-141 carboxybenzyl)-N,N-dimethyl-2,3- bis (oleoyloxy) propan-1-aminium (DOBAO). DOBAO is 142 neutral at physiological pH and becomes cationic as the pH is lowered, with a pKa of approximately 6 when measured in DOPC:DOBAQ 3:1 liposomes.³⁵ Preliminary exploration of 143 144 the phase behavior of MO:Olalc:DOBAQ mixtures found that 3 mol% DOBAQ was optimal to 145 reproducibly switch between the Fd3m and H_{II} phases by lowering the pH. The phase behavior 146 and lattice parameter (a) dependence of MO:Olalc dispersions at a fixed 3mol% DOBAQ at 25 147 and 37 °C and pH 7.4 are shown in Figure 1b. At this fixed DOBAQ ratio the system forms hexosomes between 37 and 39 mol% Olalc. Increasing Olalc to 41 mol% at 37 °C or 42 mol% at 148 25 ° C transforms the system to Fd3m micellosomes, with a small area of phase coexistence 149 150 between 40 and 41 mol% Olalc at 25 °C and 40mol% at 37 °C.



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153 Figure 1. Design parameters to tune the negative interfacial curvature of the nanoparticles. (a) Increasing the amount of the weakly polar ampliphile OlAlc should drive the formation of more 154 155 curved structures (top). Lowering the pH will cause DOBAQ to become cationic, increase its 156 effective headgroup area and electrostatic repulsion between headgroups which should result in 157 the adoption of less curved phases (bottom). (b) Phase behavior and the effect on the lattice parameter of incorporating Olalc into MO dispersions, keeping the pH sensitive lipid DOBAQ 158 159 concentration fixed at 3 mol% in all samples at pH 7.4. The dashed region on the graph highlights 160 the composition that was further studied as a function of pH.

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Olalc is non-ionisable and has a slightly smaller headgroup compared to OA and hence lower concentrations are required to promote the Fd3m phase. This can be rationalized by increasing the magnitude of the spontaneous inverse monolayer curvature (H_0) towards water,³⁷ which is related to the structural parameters of the lipids as dictated by the critical packing parameter (CPP) in equation (1).

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$$CPP = \frac{v}{a_o l} \tag{1}$$

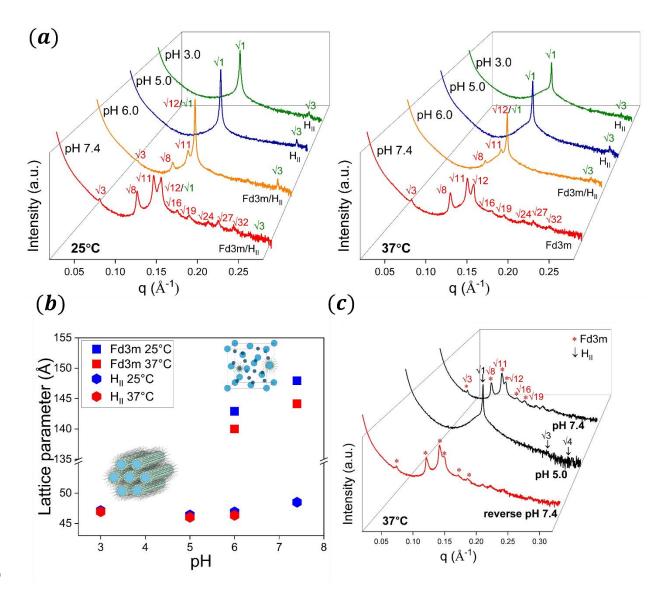
168 where *v* is the molecular volume of the fluid hydrocarbon chain(s), *l* is the length of a fully 169 extended hydrocarbon chain and a_o is the interfacial area per molecule at the polar-non-polar 170 interface.

Increasing Olalc concentration will decrease the headgroup area driving the formation of structures with increased negative curvature. This is evident in **Figure 1b** where an increase in Olalc causes a transition from hexosomes to the more inversely curved Fd3m micellosomes. Within the pure phase regions a reduction in the lattice parameters of both phases is observed, which is explained by the reduction in water concentration with increasing mean inverse interfacial curvature.

These nanoparticles were engineered and envisioned for future *in vitro/vivo* applications. Consequently, a composition that formed Fd3m micellosomes at physiological temperature was chosen to further study the nanoparticle phase behavior as a function of pH. MO:Olalc:DOBAQ (56:41:3 mol%) was selected as it lies very close to the phase boundary, making it easier to trigger structural transitions between the two phases by changing the pH.

182 Fd3m to H_{II} transitions can be triggered by decreasing pH at fixed composition

The pH dependent phase behavior as determined by SAXS shows that F127 stabilized MO:Olalc:DOBAQ (56:41:3 mol%) dispersions clearly undergo phase changes in response to pH and demonstrates that the designed system can be tuned to switch between the Fd3m and H_{II} phases (**Figure 2a**). In these experiments, MO:Olalc:DOBAQ dispersions were originally prepared at pH 7.4, aliquots taken and their pH subsequently adjusted by HCl.



190 **Figure 2.** Fd3m to H_{II} transitions can be triggered by decreasing pH and are fully reversible. (a) SAXS patterns of the 5 wt% F127 stabilized 56:41:3 mol % MO:Olalc:DOBAQ nanoparticles in 191 192 PBS as a function of pH at 25°C (left) and 37°C (right). At pH 7.4, nine Bragg peaks are observed in the ratios of $\sqrt{3}$: $\sqrt{8}$: $\sqrt{11}$: $\sqrt{12}$: $\sqrt{16}$: $\sqrt{19}$: $\sqrt{24}$: $\sqrt{27}$: $\sqrt{32}$ (corresponding Miller indices (hkl) are 111, 193 194 220, 131, 222, 400, 331, 422, 333/511 and 440), which index as cubic space group Fd3m (red 195 label). At 25°C, the Fd3m phase coexists with a small amount of a 2D inverse hexagonal phase 196 (H_{II}). At pH 6.0, the system adopts an H_{II} phase (green label), with a Bragg peak spacing ratio of $\sqrt{1}$: $\sqrt{3}$ (Miller indices (hk) are 10 and 11) indexing to plane group p6mm, coexisting with a small 197 198 amount of Fd3m phase. When the pH is \leq 5.0, only H_{II} peaks were observed so the micellar 199 cubosomes have completely transformed to hexosomes. (b) Phase behavior and effect on the lattice 200 parameter of the nanoparticles as a function of pH. The lattice parameters of Fd3m phase decrease with the lowering of pH from 7.4 to 6.0 at both temperatures, then the Fd3m completely transforms 201 202 to an H_{II} phase when the pH is 5.0. (c) Reversible structural transitions triggered by pH at 37 $^{\circ}$ C: 203 the pH of the dispersion was gradually decreased from 7.4 to 5.0 (black curve) using HCl and then 204 increased back to 7.4 (red curve) using NaOH. Indexing of the Fd3m (only the first 6 reflections

are indexed for clarity) and the H_{II} Bragg peaks are marked with red stars and black arrows respectively. There is no significant change in the lattice parameter of the Fd3m phase and no additional phases were observed before and after the pH switch, highlighting that the transition is fully reversible.

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211 At physiological pH, the system forms Fd3m micellosomes whereas at acidic pH the 212 nanoparticles transform to hexosomes. This is attributed to the pH-sensitive behavior of DOBAQ, 213 which is neutral at pH 7.4 due to a quaternary amine present in its headgroup and becomes cationic 214 at acidic pH via protonation of its carboxylate group. The protonation of DOBAQ imposes a 215 change in CCP, due to an increase in the surface charge density and enhanced electrostatic 216 repulsion between charged headgroups. This in turn, increases the effective headgroup area and 217 hence decrease the magnitude of the monolayer spontaneous inverse curvature driving the 218 formation of less negatively curved phases.^{2, 6, 38}

219 Figure 2b shows the variation in the structure and lattice parameter of the system with pH and 220 temperature. At 25°C and pH 7.4, the system adopts an Fd3m phase with a lattice parameter of 148 Å. An additional weak reflection occurring around $q \approx 0.15$ Å⁻¹ is due to a coexisting H_{II} phase 221 222 with a lattice parameter of 48 Å. At 37°C and pH 7.4 the system adopts a pure Fd3m phase with a 223 lattice parameter of 145 Å. Upon decreasing the pH from 7.4 to 6.0, the system transforms to hexosomes. This is supported by recording the characteristic $\sqrt{3}$ -reflection of the H_{II} phase (Figure 224 225 2a) with a small contribution of coexisting Fd3m micellosomes at both 25 and 37°C. We note that 226 diffraction peak intensities scale with the underlying material's volume fraction. Peak intensities 227 can therefore be used to estimate the amount of material adopted by each respective phase. This 228 transition is in agreement with the pKa of DOBAQ measured by Walsh et al. in a liposomal formulation (pH \approx 6.0).³⁵ We further note, that the Bragg peaks of the Fd3m phase shift to higher 229 q from pH 7.4 to 6, corresponding to a decrease in a_{Fd3m} to 140 Å and 142 Å at 25 °C and 37 °C 230

231 respectively. The effect of increasing temperature, which will increase the chain splay and H_0 232 resulting in a decrease in the lattice parameter of a mesophase, is consistent with the behavior seen 233 here and with most lyotropic liquid crystalline formulations. On the contrary, the observation of a 234 decrease in lattice parameter with an increase in charge is at first instance counter-intuitive, 235 because an increase in charge should reduce H₀ and hence cause the lattice parameter of the Fd3m 236 phase to increase. This trend could be rationalized by considering the size of the nanoparticles 237 which is also highlighted in the subsequent section on cryo-TEM data. As seen in Figures 3 and 238 4, Fd3m micellosomes have a range of sizes and vary in their lattice parameters, with smaller 239 nanoparticles displaying bigger lattice parameters and larger nanoparticles displaying smaller 240 lattice parameters. The larger nanoparticles offer a bigger confinement volume for lyotropic liquid 241 crystals to form, and as a consequence are less prone to structural defects and repulsive membrane 242 undulation forces which will result in smaller lattice spacings and also render them more stable. 243 We hypothesize that at pH 6, the weak reflections from the Fd3m structure are due to a few 244 remaining more stable, relatively bigger Fd3m nanoparticles which have smaller lattice parameters 245 (Figure 2b).

At pH 5.0, only the H_{II} phase was observed and hence the system has completely transformed from the initial Fd3m phase. Further decreasing the pH to 3 did not alter the phase behavior and the lattice parameter of the H_{II} phase varied little (maximum ±2Å) across all pH values measured.

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250 pH-triggered Fd3m to H_{II} transitions are reversible

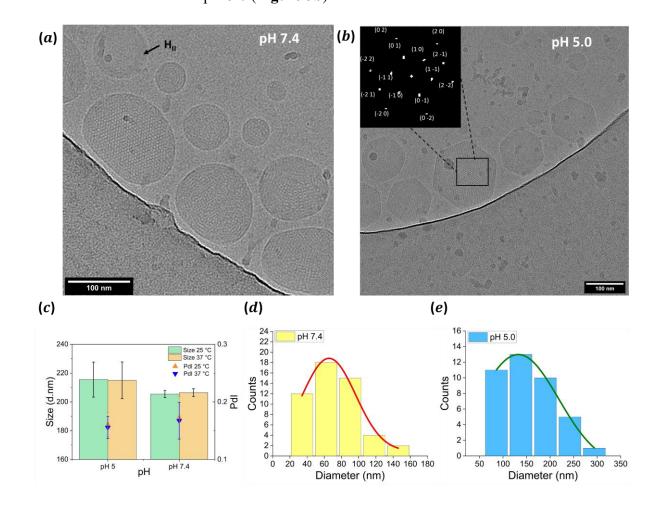
To evaluate the potential to reverse the structural transition in the designed system at 37° C, the pH of the sample was first lowered from pH 7.4 where the system adopted a pure Fd3m phase, to pH 5.0, where only the H_{II} phase was observed. The pH was then subsequently raised back to 7.4 in

254 the same sample leading to the reformation of the Fd3m phase. SAXS data demonstrate the 255 reversibility of the Fd3m to H_{II} transition by adjusting the pH of the PBS dispersions with NaOH 256 or HCl (Figure 2c). The lattice parameter of the sample in the Fd3m phase before (144.9 Å) and 257 after reversing the pH back to pH 7.4 (147.1 Å) is very similar, highlighting the truly reversible 258 responsiveness of the system. The structure reversibility of the system is due to the protonation 259 and deprotonation of the DOBAQ headgroup. When the pH is 7.4, the DOBAQ headgroup 260 deprotonates and becomes neutral whereas at lower pH protonation causes the headgroup to 261 become cationic. Repulsions between the gradually protonating or deprotonating carboxylic group 262 of 3 mol% DOBAQ embedded at the lipid-water interface, modifies the system's spontaneous 263 curvature.

264 The nanostructure of the designed system can be easily tuned by only a very small amount of 265 pH-sensitive lipid, and shows the excellent pH sensitivity and selectivity of this system compared 266 to previous studies where large amounts of ionisable lipids were required to switch between these 267 two structures and/or significant changes in ionic strength of the buffer. Moreover, whilst an Fd3m 268 to H_{II} transition has been reported in the literature by increasing pH (although none have 269 demonstrated this at 37°C), this is the first example of an Fd3m to H_{II} transition from physiological 270 to acidic pH. This transition could potentially be advantageous in nanomedicine, where a 271 hydrophilic active could be encapsulated into the inverse micelles of the Fd3m phase significantly 272 hindering its release in the serum, but by rearranging to a porous H_{II} phase, e.g. in the endosome, 273 can facilitate release. As an example, the diffusion coefficient of glucose from a system adopting 274 the H_{II} phase was shown to be approximately 15 times that observed in the Fd3m phase in bulk mesophases however how this translates to LCNPs is not known.²⁶ 275

277 Cryogenic Transmission Electron Microscopy (Cryo-TEM) facilitates quantitative
 278 structural characterization of individual LCNPs
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The cryo-TEM images of the designed MO:Olalc:DOBAQ 56:41:3 mol% system confirmed the pH-triggered nanostructural transitions observed by SAXS. At pH 7.4, the cryo-TEM image indicates the presence of Fd3m micellosomes coexisting with as small amount hexosomes, with the Fd3m micellosomes dominating in the dispersions (**Figure 3a**) at 25 °C. By contrast, only hexosomes were observed at pH 5.0 (**Figure 3b**).



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Figure 3. Representative cryo-TEM images of the MO:Olalc:DOBAQ 56:41:3 mol% system prepared at 25 °C and their size distributions. (*a*) Fd3m micellosomes at pH 7.4 coexisting with a small amount of hexosomes (black arrow), which likely give rise to the weak intensity of the $\sqrt{1}$ peak in the SAXS data in Figure 2*a*. Both SAXS and cryo-TEM data are in agreement that the

291 dominating phase at pH 7.4 at 25 °C is Fd3m. (b) pure hexosomes at pH 5.0. The insert in panel 292 b shows the corresponding intensity of the fast Fourier transform (FFT) applied to the black box 293 region of the individual nanoparticle and the assigned Miller indices. (c) Dynamic light scattering 294 (DLS) data of MO:Olalc:DOBAQ 56:41:3 mol% nanoparticles in PBS at different pH at 25 °C 295 (green) and 37 °C (orange). At 25 °C, Fd3m micellosomes at pH 7.4 have a mean size of ~ 205 296 nm, whilst hexosomes are ~216 nm at pH 5; At 37 °C Fd3m micellosomes have a mean size of 297 \sim 206 nm and hexosomes \sim 215nm. (d) and (e) Cryo-TEM size distribution of nanoparticles 298 hydrated at pH 7.4 and pH 5.0 respectively. Histograms were calculated from 51 nanoparticles at 299 pH 7.4 and 40 for pH 5.0 and fitted to a Gaussian function. From the fit we obtain a mean of 65 300 and 132 nm for the nanoparticles at pH 7.4 and pH 5 respectively. Both DLS and Cryo-TEM data 301 show nanoparticles at pH 5.0 generally have a slightly larger size compared to that at pH 7.4. 302

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304 The particle size distribution of the nanoparticles at 25 and 37 °C was investigated using dynamic 305 light scattering (DLS) and the results are shown in Figure 3c. The Fd3m micellosomes at pH 7.4 306 have a mean size of ~ 205 and 206 nm, whereas the hexosomes at pH 5 have a mean size of ~ 216 307 and 215 nm, at 25 and 37 °C respectively. The DLS results at 25 °C were compared with the 308 nanoparticle size analysis from Cryo-TEM data (51 nanoparticles analyzed at pH 7.4 and 40 at pH 309 5.0) shown in Figure 3d and 3e. The histograms were fitted to a Gaussian function and we obtain 310 a mean size of 65 and 132 nm for the nanoparticles at pH 7.4 and pH 5, respectively. The mean 311 size of the nanoparticles calculated differs between the two techniques, as DLS weighs the size 312 distribution differently with larger particles emphasized as they scatter light more strongly whereas 313 cryo-TEM often excludes larger particles from the thin ice films, emphasizing smaller particles in these polydisperse populations. Nonetheless, there is a clear trend that hexosomes are larger than 314 315 the micellar cubosomes. This is because a decrease in pH leads to protonation of the DOBAQ 316 headgroup resulting in a repulsive force at the lipid-water interface which pushes the elongation 317 of the Fd3m micellar 'pockets' to form a tubular structure in the H_{II} phase and an overall increase 318 in the water concentration. However, the overall increase in water volume is only about 6% when 319 hexosomes are formed, which would only account for a 2% increase in particle size (for 320 estimations please see Supporting information Section 1), thus this cannot be the only 321 explanation for the more strongly differing particle sizes. On a mesoscopic level though, there is 322 an unneglectable difference. While the micellosomes are spherical in shape and hence display a 323 maximized volume to surface ratio, hexosomes are by no means perfectly spherical. They display 324 different shapes, like flat hexagonal prisms (Figure 3b), and often possess even "spinning toplike" structures.³⁹ In any case, their shape deviates significantly from that of a sphere, and hence, 325 326 the apparent mean hydrodynamic size of hexosomes is bigger, whilst their volume has not 327 increased by much. This apparent size increase of hexosomes is even more pronounced in our 328 cryo-TEM measurements, since we measured the diameter of the hexagonal prism section, whilst 329 not considering the perpendicular short extension of the hexosomes.

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331 Traditionally, cryo-TEM cannot be used to unambiguously determine the space group of 332 lyotropic liquid crystalline phases due to the low resolution of the images leading to only a couple 333 of peaks to be observed after applying a fast Fourier transform to the image.⁴⁰ However, it is a 334 powerful complementary technique to SAXS. Whilst cubosomes based on bicontinuous cubic 335 phases, and hexosomes are easier to visualize with cryo-TEM and give rise to a number of peaks 336 in their FFTs,⁴¹⁻⁴² cryo-TEM images of Fd3m micellosomes reported to date in the literature are 337 of very low resolution, which is insufficient for the visualization of the internal nanostructure of 338 the phase.

Here we have been able to obtain high resolution images and directly visualize the internal structure of the Fd3m nanoparticles along two viewing orientations, which allow us to resolve the large and small micelles of the Fd3m structure and calculate structural information using cryo-TEM for the first time.

Figure 4 shows detailed images of Fd3m nanoparticles in two different orientations, image 344 345 analysis, indexing and simulated TEM diffraction patterns. Figure 4a highlights an Fd3m 346 micellosome along the [110] viewing direction with respect to the electron beam. The simulated 347 TEM diffraction pattern from an Fd3m phase diffraction pattern viewed down the (110) plane 348 normal (Figure 4b) is in excellent agreement with the experimentally determined FFT pattern. Figure 4c shows the FFT from the image in Figure 4a in which the $\sqrt{3}$, $\sqrt{8}$, $\sqrt{11}$ and $\sqrt{12}$ 349 350 reflections, corresponding to Miller planes (111), (220), (311) and (222) can be clearly observed. 351 Each theoretical reflection from the simulated diffraction pattern indexed in Figure 4b 352 corresponds to the same reflection in Figure 4c. The lattice parameter of the nanoparticle in Figure 353 4a was determined to be 149.3 Å (see also Supporting Information Section 2 for additional 354 information on determining the lattice parameter).

Figure 4e shows an Fd3m nanoparticle aligned along the [114] direction with respect to the electron beam in which the $\sqrt{8}$, $\sqrt{11}$, $\sqrt{27}$ and $\sqrt{32}$ reflections, corresponding to Miller planes (220), (311), (511) and (440) were observed. Each theoretical reflection from an Fd3m phase viewed down the (114) plane normal and indexed in Figure 4f directly matches the experimentally determined reflections in Figure 4g. The lattice parameter of the particle in Figure 4e was determined to be 137.0 Å based on the FFT analysis.

The lattice parameters of the individual nanoparticles calculated from the cryo-TEM data are slightly different to those obtained by SAXS, which is expected, as SAXS gives the average lattice parameter of all the nanoparticles in the measured sample whilst we focus on specific nanoparticles for the cryo-TEM analysis. Based on the cryo-TEM images collected, we observe that generally nanoparticles which have a smaller lattice parameter tend to be larger in size. This finding supports our hypothesis that smaller Fd3m nanoparticles undergo a faster structural transition compared to

- 367 larger particles, as they are expected to contain relatively more defects (cp. discussion above) and
- are thus less stable.

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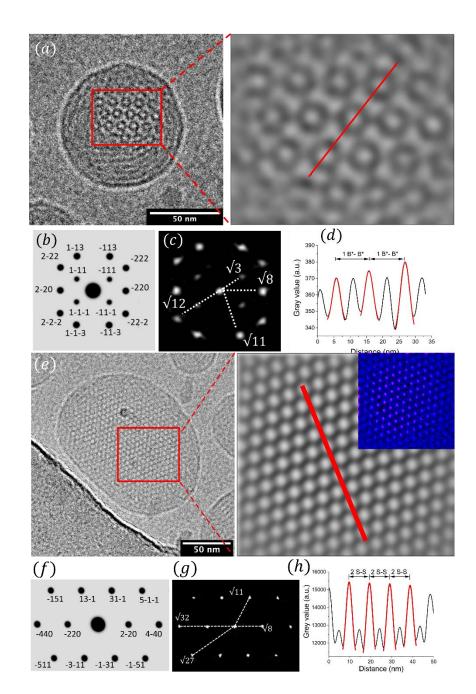


Figure 4. High resolution cryo-TEM images allow direct visualization of the internal structure of the Fd3m nanoparticles. (*a*) Cryo-TEM image on an Fd3m micellosome of MO:Olalc:DOBAQ 56:41:3 mol% prepared at 25°C and pH 7.4. The nanoparticle is aligned along the [110] orientation with respect to the electron beam. The red box indicates the region used to apply the FFT shown in 4c and the zoomed-in region on the right hand side shows the inverse FFT of 4c (after application

of rolling background subtraction and Gaussian blur), and was used to determine the $d_{B^*-B^*}$ 376 377 distance indicated by the red line. (b) Simulated transmission electron microscopy (TEM) 378 diffraction pattern viewed down the (110) plane normal of an Fd3m phase with assigned Miller 379 indices and (c) the corresponding intensity of the FFT applied to the red box region of 7a which is 380 in excellent agreement with the simulated pattern. Each theoretical reflection from the simulated 381 pattern indexed in 4b corresponds to the same reflection in 4c. (d) Gaussian fitting of the intensity 382 profile along the red line of the inverse FFT, shown in the zoomed in region of 4a, gave an average 383 distance between two interval big micelles $(d_{B^*-B^*})$ of 105.5 Å. The lattice parameter of the nanoparticle in 7a was determined to be 149.3 Å, which gives a theoretical $d_{B^*-B^*}$ value of 105.5 384 385 Å. (e) cryo-TEM image of an Fd3m nanoparticle aligned along the [114] orientation with respect to the electron beam. The red box indicates the region used to apply the FFT shown in 4g and the 386 387 zoomed-in region on the right hand side shows the inverse FFT of 4g (after application of rolling 388 background subtraction and Gaussian blur), and was used to determine the d_{s-s} distance indicated by the red line. The inset shows the overlay of the raw image of 4e on the left shown in blue and 389 390 the inverse FFT on the right shown in magenta which are in excellent agreement. (f) Simulated 391 transmission electron microscopy (TEM) diffraction pattern viewed down the (114) plane normal 392 of an Fd3m phase with assigned Miller indices and (g) the corresponding intensity of the FFT 393 applied to the red box region of 8a which is in excellent agreement with the simulated pattern. 394 Each theoretical reflection from the simulated pattern indexed in 4f corresponds to the same 395 reflection in 4g. (h) Gaussian fitting of the intensity profile along the red line of the inverse FFT, 396 shown in the zoomed in region of 8a, gave an average plane to plane distance of the small micelles $((d_{S-S}))$ of 48.5 Å. The lattice parameter of the nanoparticle in 8a was determined to be 137 Å, 397 398 which gives a theoretical d_{S-S} value of 48.4 Å.

399

400 The high resolution cryo-TEM images have allowed us to direct visualize the large and small

401 micelles of the Fd3m structure (eight large and sixteen small micelles per unit cell), determine the

402 micelle positions and compare them to theoretical distances for the Fd3m structure.

403 From geometry,⁴³ the big (B) micelle-to-micelle distance is given by equation 2:

404
$$d_{B-B} = \frac{\sqrt{3}}{4} a$$
 (2)

405 and the small (S) micelle-to-micelle distance is given by:

406
$$d_{S-S} = \frac{\sqrt{2}}{4} a$$
 (3)

407

408 Figure 4a shows an Fd3m micellosome aligned along the [110] orientation. The distribution of409 the different micelles along the (110) section will depend on where the section cuts through the

410 plane along the z direction. Here only the big micelles are seen, however this does not represent 411 the d_{B-B} micelle-to-micelle distance defined above which is the smallest distance between two 412 adjacent big micelles, but instead what we define as the d_{B*-B*} distance, which is the distance 413 between two interval big micelles (in a hexagonal arrangement) and is given by equation 4 (see 414 also **Supporting Information** Section 3):

415
$$d_{B*-B*} = 2d_{S-S} = \sqrt{\left(\frac{8}{3}\right)}d_{B-B} = \frac{\sqrt{2}}{2}a_{Fd3m}$$
 (4)

416

Further discussion on determining the d_{B*-B*} distance as well as comparing the excellent agreement of the inverse FFT (**Figure S2a**) obtained from **Figure 4c** with some 2-D serial sections of the 3-D electron density map from a previously published DOPC:DOG 1:2 mol% system adopting an Fd3m phase (**Figures S2b** and **S2c**)⁴⁴ can be found in **Supporting Information** Section 3.

Experimentally, the B*-B* distance was determined by taking the inverse FFT of **Figure 4c**, which has been background subtracted. The resulting, Gaussian blurred, inverse FFT shown on the right of **Figure 4a** was used to determine the B*-B* (d_{B*-B*}) distance by Gaussian fitting (**Figure 4d**) of its intensity profile along the red line in **Figure 4a** (right). The average d_{B*-B*} distance measured was 105.5 Å which is identical to the theoretical distance of 105.5 Å based on the experimentally determined lattice parameter of 149.3 Å (equation 4).

Figure 4e shows an Fd3m micellosome aligned along the [114] orientation and highlights the small micelles of the Fd3m phase. Based on the reflections of the FFT in Figure 4g, the lattice parameter was determined to be 137 Å, which gives a theoretical d_{S-S} micelle-to-micelle distance of 48.4 Å (equation 2). Note the $\sqrt{8}$ reflection also corresponds to the S-S micelle distance. The d_{S-S} distance was determined by taking the inverse FFT of Figure 4g, which has been background

433 subtracted. The resulting, Gaussian blurred, inverse FFT is shown in Figure 4e (right) was used 434 to determine the d_{S-S} distance by Gaussian fitting (Figure 4h) of its intensity profile along the red 435 line in Figure 4e (right). The overlay of the raw image of Figure 4e (left) shown in blue and 436 inverse FFT (from Figure 4g) shown in magenta are in excellent agreement (Figure 4a, right, 437 inset). It should be noted that in the [114] direction, d_{S-S} does not correspond to the distance 438 between two adjacent small micelles as shown in Figure Figure S2b for the (110) section but is 439 instead the plane to plane distance of the small micelles in this projection (Figure 4e (right), see 440 also Figure S3). The experimentally determined S-S plane distance (Figure 4h) and the (220) 441 reflection from Figure 4g were 48.5 and 48.3 Å respectively and match the theoretical distance of 442 48.4 Å determined above.

443

444 CONCLUSION

445 We have been able to generate highly sensitive pH responsive lyotropic liquid crystalline 446 nanoparticles that require only a very small amount (3 mol%) of pH sensitive lipid to switch 447 between a compartmentalized internal structure based on space group Fd3m at physiological pH 448 to an accessible porous 2D hexagonal structure when the pH is ≤ 6 at both at 25 and 37°C. The 449 transition is fully reversible by tuning the inverse spontaneous curvature by the protonation or 450 deprotonation of the pH sensitive lipid's headgroup. The internal symmetry of the nanoparticles 451 was confirmed by SAXS and cryo-TEM. Imaging of Fd3m nanoparticles has been challenging 452 with cryo-TEM however we have managed to acquire high resolution images of them and directly 453 visualize the structure in unprecedented detail for the first time. Depending on the direction the 454 particles are aligned with respect to the electron beam we can resolve the large and small inverse 455 micelles of the Fd3m phase which allowed us to calculate structural information such as the

456 positions and distances of the two different sized micelles and compare these to theory based on 457 geometrical considerations. These promising findings could pave the way to developing superior 458 stimuli-responsive soft nanoparticle formulations that change their connectivity upon encountering 459 acidic pH, which is known for example to be highly important both in human disease as well as 460 plant physiology and crop performance. They can potentially benefit a range of downstream 461 applications in the biomedical, food, agrochemical and environmental remediation industries.

462

- 463 MATERILAS AND METHODS
- 464

465 Preparation of MO/Olalc/DOBAO nanoparticles. Monoolein (MO; was a kind gift from 466 Croda Personal Care, Goole, UK), Oleyl alcohol (Olalc; Sigma Aldrich, Gillingham, UK), N-(4-467 carboxybenzyl)-N,N-dimethyl-2,3-bis(oleoyloxy)propan-1-aminium (DOBAQ; Avanti polar 468 lipids, AL, USA) were weighted and dissolved in chloroform (Sigma-Aldrich, Gillingham, UK), 469 then mixed at the desired MO:Olalc:DOBAQ molar ratios. MO had a purity of >92% whilst the 470 rest of the lipids had a purity of >99% and were used without further purification. The chloroform 471 solutions were dried using a stream of N_2 gas and the dry thin films were left under vacuum 472 overnight to remove any residual organic solvent. Thin films were then heated to 60°C and 473 hydrated with phosphate-buffered saline buffer (PBS; Sigma-Aldrich, Gillingham, UK) containing 474 6.923 mg/ml Pluronic F127, 5 wt% F127 of total lipids, (Sigma-Aldrich, Gillingham, U.K.) to 475 achieve a sample concentration of 100 mg/ml. Dispersed samples were prepared by tip sonication 476 (VibraCell 750 with a stepped microtip, Sonics & Materials Inc, Newtown, USA) for 30 minutes 477 in pulse mode (1s pulse, 1s break) at 35% of its maximum power (750 W). The pH of the NP 478 dispersions was readjusted to 7.4 using 0.1M NaOH (Fisher Scientific, Loughborough, UK) or 479 0.1M HCl (Fisher Scientific, Loughborough, U.K.). Samples were allowed to equilibrate at 37°C

480 overnight before further experiments. The pH of the dispersed nanoparticles was first gradually 481 decreased from 7.4 to 3.0, then increased back to 7.4 while taking out samples at each selected pH 482 point for SAXS measurements at both 25 °C and 37 °C. For the dynamic light scattering and 483 cryogenic transmission electron microscopy data, lipid nanoparticles were hydrated by PBS at pH 484 7.4 or pH 5.0 directly.

485

486 Synchrotron Small-Angle X-ray Scattering (SAXS). Synchrotron SAXS data were collected 487 on beamline I22 at Diamond Light Source. The synchrotron X-ray beam was set to 18 keV which 488 corresponds to a wavelength of 0.69 Å. The sample to detector distance was set at 6 or 8.7 m and 489 the 2-D powder diffraction patterns were recorded on a Pilatus 2M detector. SAXS data were 490 analyzed using the DAWN software.⁴⁵⁻⁴⁶ The lattice parameters of the Fd3m and H_{II} phases were 491 calculated using the equations below:

492

493
$$a_{Fd3m} = \frac{2\pi}{q_{hkl}} \sqrt{h^2 + k^2 + l^2}$$
(5)

494
$$a_{H_{II}} = \frac{4\pi}{\sqrt{3} q_{hk}} \sqrt{h^2 + k^2 + hk}$$
 (6)

495

496 where q_{hkl} or q_{hk} is the scattering vector and *hkl* or *hk* are the Miller indices of a given Bragg 497 peak. Samples were equilibrated at 25 °C and 37 °C for 5 min before taking measurements.

498

499 **Dynamic Light Scattering (DLS).** For DLS measurements, particles were made at a 500 concentration of 5mg/mL. Samples were diluted to 25 μ g/mL by isotonic PBS at different pH 501 before DLS measurement. The mean hydrodynamic radius and polydispersity index width (PDI) 502 of the nanoparticles were measured at pH 7.4 and pH 5.0 using a Malvern Zetasizer Nano ZSP 503 instrument (Malvern Panalytical, Malvern, UK) equipped with a 633 nm helium-neon laser. 504 Samples were measured at 25 °C or 37 °C at a fixed 173° backscattering angle. The refractive 505 index and absorption of material is set as 1.46 and 0.001 respectively. The refractive index of 506 dispersion is 1.334 and its viscosity is 0.9110 mPa.s at 25 °C and 0.7130 mPa.s at 37 °C.

507

508 Cryogenic-transmission electron microscopy (Cryo-TEM). Samples were diluted once (final 509 concentration of 50 mg/ml) in isotonic PBS at the required pH for the morphological 510 characterization using cryo-TEM. In brief, $3 \mu L$ of the diluted sample was applied to freshly glow 511 discharged Cu QUANTIFOIL grids (R2/R2, 300 or 400 mesh) with a hold time of 30 s. The 512 carbon-coated grids were glow discharged at 10 mA for 20 s for samples at pH 7.4 and 30 s for 513 samples at pH 5.0. The grids were blotted for 6 s with a blotting force of 7 at 25 °C under 100% 514 relatively humidity, then plunged into liquid ethane using a VitrobotTM mark IV (Thermo/FEI). 515 Grids were kept under liquid nitrogen before measurement.

516 Data acquisition was carried out on a Titan KRIOS microscope (Thermo Fisher Scientific, US) 517 with an accelerating voltage of 300 KV and a defocus value of -1 µm at a nominal magnification 518 of 45k or 75k. The pixel size for these images were 1.76 and 1.065 Å, respectively. Image 519 processing was done using Fiji.⁴⁷ The Fast Fourier Transforms (FFTs) of the raw images were 520 background subtracted. The d-spacing of each reflection in the FFT was determined using 521 TrackMate.⁴⁸ The micelle distances were calculated from the inverse FFTs after application of 522 rolling background subtraction and Gaussian blur using Fiji.

- 524
- 525

526	Simulation of TEM diffraction patterns
527	The program CrystalMaker® (CrystalMaker Software Ltd, Oxford, England-
528	www.crystalmaker.com) was used to visualize 2-D sections (110 and 114 planes) through the
529	model structure of the Fd3m cubic phase. Fd3m origin 2 (at $\overline{3}m$) was used. These sections were
530	then sent to the SingleCrystal TM program to simulate transmission electron microscopy (TEM)
531	diffraction patterns.
532	
533	ASSOCIATED CONTENT
534	Supporting Information
535	Discussion on the estimation of micellosome and hexosome size ratios, details on the calculation
536	of lattice parameters from cryo-TEM data and determination of the micelle positions in Fd3m
537	nanoparticles.
538	
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555	Author Contributions
556	A.I.I.T. conceived and designed the experiments. J.M.S, P.A.B., M.R. and A.I.I.T contributed to
557	study design. Z.X. performed all the experiments. Z.X., M.R. and A.I.I.T. analyzed the data. Z.X.,
558	P.A.B., M.R. and A.I.I.T. interpreted the results. Z.X. M.R. and A.I.I.T co-wrote the manuscript.
559	All authors discussed the results and commented on the manuscript.
560	Funding Sources
561	The research was supported by start-up funding awarded to A.I.I.T. from the University of Leeds
562	as a well as a PhD scholarship awarded to Z.X.
563	
564	Notes
565	The authors declare no competing financial interest.
566	
567	ACKNOWLEDGMENTS
568	We thank Diamond Light Source for the award of synchrotron beamtimes (SM18027-1, SM22659-
569	1 and SM24530-1) as well as Dr. Andy Smith, Dr. Tim Snow and Professor Nick Terrill for their

570 support and assistance. We thank Dr. Aleks Ponjavic from the University of Leeds for help with

571 some aspects of image processing and analysis and drawing figures. We also thank Dr. Rebecca

572 Thompson from the Astbury Biostructure Facility and Rashmi Seneviratne from the School of

573 Chemistry at the University of Leeds for their support with Cryo-TEM. The FEI Titan Krios

574 microscope used was funded by the University of Leeds (UoL ABSL award) and Wellcome Trust

- 575 (108466/Z/15/Z). The Bragg Centre for Materials Research at the University of Leeds is also
- 576 acknowledged.
- 577
- 578 References

Nguyen, T. H.; Hanley, T.; Porter, C. J.; Boyd, B. J., Nanostructured liquid crystalline
 particles provide long duration sustained-release effect for a poorly water soluble drug after oral
 administration. *J Control Release* 2011, *153* (2), 180-186.

- 582 2. Kim, H.; Leal, C., Cuboplexes: Topologically Active siRNA Delivery. ACS Nano 2015, 9
 583 (10), 10214-10226.
- 3. Praca, F. S. G.; Medina, W. S. G.; Petrilli, R.; Bentley, M. V. L. B., Liquid Crystal
 Nanodispersions Enable the Cutaneous Delivery of Photosensitizer for Topical PDT: Fluorescence
 Microscopy Study of Skin Penetration. *Current Nanoscience* 2012, 8 (4), 535-540.

Jain, V.; Swarnakar, N. K.; Mishra, P. R.; Verma, A.; Kaul, A.; Mishra, A. K.; Jain, N. K.,
Paclitaxel loaded PEGylated gleceryl monooleate based nanoparticulate carriers in chemotherapy. *Biomaterials* 2012, *33* (29), 7206-7220.

- 590 5. Rizwan, S. B.; McBurney, W. T.; Young, K.; Hanley, T.; Boyd, B. J.; Rades, T.; Hook, S., 591 Cubosomes containing the adjuvants imiquimod and monophosphoryl lipid A stimulate robust 592 cellular and humoral immune responses. *J Control Release* **2013**, *165* (1), 16-21.
- 593 6. Zhai, J.; Fong, C.; Tran, N.; Drummond, C. J., Non-Lamellar Lyotropic Liquid Crystalline
 594 Lipid Nanoparticles for the Next Generation of Nanomedicine. *ACS Nano* 2019, *13* (6), 6178595 6206.
- 596 7. Ganta, S.; Devalapally, H.; Shahiwala, A.; Amiji, M., A review of stimuli-responsive 597 nanocarriers for drug and gene delivery. *J Control Release* **2008**, *126* (3), 187-204.
- 598 8. Warburg, O., On the origin of cancer cells. *Science* **1956**, *123* (3191), 309-314.
- 599 9. Hrubý, M.; Koňák, Č.; Ulbrich, K., Polymeric micellar pH-sensitive drug delivery system 600 for doxorubicin. *Journal of Controlled Release* **2005**, *103* (1), 137-148.
- Fong, W. K.; Negrini, R.; Vallooran, J. J.; Mezzenga, R.; Boyd, B. J., Responsive selfassembled nanostructured lipid systems for drug delivery and diagnostics. *J Colloid Interface Sci* **2016**, 484, 320-339.
- 604 11. Boelsma, E.; van de Vijver, L. P.; Goldbohm, R. A.; Klöpping-Ketelaars, I. A.; Hendriks,
- 605 H. F.; Roza, L., Human skin condition and its associations with nutrient concentrations in serum 606 and diet. *The American journal of clinical nutrition* **2003**, 77 (2), 348-355.

- Cederberg, C.; Rohss, K.; Lundborg, P.; Olbe, L., Effect of once daily intravenous and oral
 omeprazole on 24-hour intragastric acidity in healthy subjects. *Scand J Gastroenterol* 1993, 28
 (2), 179-184.
- 610 13. Hu, Y.-B.; Dammer, E. B.; Ren, R.-J.; Wang, G., The endosomal-lysosomal system: from
- acidification and cargo sorting to neurodegeneration. *Translational Neurodegeneration* 2015, 4
 (1), 18.
- 613 14. Sorkin, A.; Von Zastrow, M., Signal transduction and endocytosis: close encounters of 614 many kinds. *Nat Rev Mol Cell Biol* **2002**, *3* (8), 600-614.
- 615 15. Kocak, G.; Tuncer, C.; Bütün, V., pH-Responsive polymers. *Polymer Chemistry* 2017, 8
 616 (1), 144-176.
- 617 16. Deirram, N.; Zhang, C.; Kermaniyan, S. S.; Johnston, A. P. R.; Such, G. K., pH-Responsive
 618 Polymer Nanoparticles for Drug Delivery. *Macromolecular Rapid Communications* 2019, 40 (10),
 619 1800917.
- 620 17. Mezzenga, R.; Seddon, J. M.; Drummond, C. J.; Boyd, B. J.; Schröder-Turk, G. E.;
- Sagalowicz, L., Nature-Inspired Design and Application of Lipidic Lyotropic Liquid Crystals.
 Advanced Materials 2019, *31* (35), 1900818.
- 18. Tan, A.; Hong, L.; Du, J. D.; Boyd, B. J., Self-Assembled Nanostructured Lipid Systems:
 Is There a Link between Structure and Cytotoxicity? *Advanced Science* 2019, *6* (3), 1801223.
- 625 19. Luzzati, V.; Husson, F., The structure of the liquid-crystalline phasis of lipid-water 626 systems. *The Journal of cell biology* **1962**, *12*, 207-219.
- 627 20. Luzzati, V.; Reiss-Husson, F., Structure of the Cubic Phase of Lipid-Water Systems.
 628 *Nature* 1966, *210* (5043), 1351-1352.
- Seddon, J. M., Structure of the inverted hexagonal (HII) phase, and non-lamellar phase
 transitions of lipids. *Biochim Biophys Acta* 1990, *1031* (1), 1-69.
- Guillot, S.; Moitzi, C.; Salentinig, S.; Sagalowicz, L.; Leser, M. E.; Glatter, O., Direct and
 indirect thermal transitions from hexosomes to emulsified micro-emulsions in oil-loaded
 monoglyceride-based particles. *Colloids and Surfaces A: Physicochemical and Engineering Aspects* 2006, 291 (1), 78-84.
- 435 23. Yaghmur, A.; de Campo, L.; Salentinig, S.; Sagalowicz, L.; Leser, M. E.; Glatter, O., Oilbioaded monolinolein-based particles with confined inverse discontinuous cubic structure (Fd3m). *Langmuir* 2006, 22 (2), 517-521.
- 638 24. Yaghmur, A.; de Campo, L.; Sagalowicz, L.; Leser, M. E.; Glatter, O., Emulsified 639 microemulsions and oil-containing liquid crystalline phases. *Langmuir* **2005**, *21* (2), 569-577.
- 640 25. Boyd, B. J.; Whittaker, D. V.; Khoo, S.-M.; Davey, G., Lyotropic liquid crystalline phases
- 641 formed from glycerate surfactants as sustained release drug delivery systems. *International* 642 *Journal of Pharmaceutics* **2006**, *309* (1), 218-226.
- 643 26. Phan, S.; Fong, W.-K.; Kirby, N.; Hanley, T.; Boyd, B. J., Evaluating the link between
- self-assembled mesophase structure and drug release. *International Journal of Pharmaceutics* **2011**, *421* (1), 176-182.
- 646 27. Negrini, R.; Mezzenga, R., pH-responsive lyotropic liquid crystals for controlled drug 647 delivery. *Langmuir* **2011**, *27* (9), 5296-5303.
- 648 28. Negrini, R.; Fong, W.-K.; Boyd, B. J.; Mezzenga, R., pH-responsive lyotropic liquid
- 649 crystals and their potential therapeutic role in cancer treatment. *Chemical Communications* 2015,
- 650 *51* (30), 6671-6674.

- 651 29. Oka, T.; Tsuboi, T.-a.; Saiki, T.; Takahashi, T.; Alam, J. M.; Yamazaki, M., Initial Step of 652 pH-Jump-Induced Lamellar to Bicontinuous Cubic Phase Transition in 653 Dioleoylphosphatidylserine/Monoolein. Langmuir 2014, 30 (27), 8131-8140.
- 654 30. Salentinig, S.; Sagalowicz, L.; Glatter, O., Self-assembled structures and pKa value of oleic acid in systems of biological relevance. Langmuir 2010, 26 (14), 11670-11679. 655
- 656 Gontsarik, M.; Mohammadtaheri, M.; Yaghmur, A.; Salentinig, S., pH-Triggered 31. 657 nanostructural transformations in antimicrobial peptide/oleic acid self-assemblies. Biomater Sci 658 **2018**, *6* (4), 803-812.
- 659 Fong, C.; Zhai, J.; Drummond, C. J.; Tran, N., Micellar Fd3m cubosomes from monoolein 32. 660 - long chain unsaturated fatty acid mixtures: Stability on temperature and pH response. Journal of 661 Colloid and Interface Science 2020, 566, 98-106.
- 662 Kulkarni, C. V.; Tang, T.-Y.; Seddon, A. M.; Seddon, J. M.; Ces, O.; Templer, R. H., 33. 663 Engineering bicontinuous cubic structures at the nanoscale-the role of chain splay. Soft Matter 664 **2010,** *6* (14), 3191-3194.
- 665 Briggs, J.; Chung, H.; Caffrey, M., The Temperature-Composition Phase Diagram and 34. 666 Mesophase Structure Characterization of Monoolein/Water System. Journal de Physique II 1996, 667 6 (5), 723-751.
- 668 Walsh, C. L.; Nguyen, J.; Szoka, F. C., Synthesis and characterization of novel zwitterionic 35. 669 lipids with pH-responsive biophysical properties. Chemical Communications 2012, 48 (45), 5575-
- 5577. 670
- 671 36. Nakano, M.; Teshigawara, T.; Sugita, A.; Leesajakul, W.; Taniguchi, A.; Kamo, T.; 672 Matsuoka, H.; Handa, T., Dispersions of Liquid Crystalline Phases of the Monoolein/Oleic 673 Acid/Pluronic F127 System. Langmuir 2002, 18 (24), 9283-9288.
- 674 Kollmitzer, B.; Heftberger, P.; Rappolt, M.; Pabst, G., Monolayer spontaneous curvature 37. 675 of raft-forming membrane lipids. Soft Matter 2013, 9 (45), 10877-10884.
- 676 38. Tyler, A. I.; Barriga, H. M.; Parsons, E. S.; McCarthy, N. L.; Ces, O.; Law, R. V.; Seddon,
- 677 J. M.; Brooks, N. J., Electrostatic swelling of bicontinuous cubic lipid phases. Soft Matter 2015, 678 11 (16), 3279-3286.
- 679 Boyd, B. J.; Rizwan, S. B.; Dong, Y.-D.; Hook, S.; Rades, T., Self-Assembled Geometric 39. 680 Liquid-Crystalline Nanoparticles Imaged in Three Dimensions: Hexosomes Are Not Necessarily 681 Flat Hexagonal Prisms. Langmuir 2007, 23 (25), 12461-12464.
- Sagalowicz, L.; Acquistapace, S.; Watzke, H. J.; Michel, M., Study of Liquid Crystal Space 682 40.
- Groups Using Controlled Tilting with Cryogenic Transmission Electron Microscopy. Langmuir 683 684 2007, 23 (24), 12003-12009.
- 685 Barauskas, J.; Johnsson, M.; Tiberg, F., Self-assembled lipid superstructures: beyond 41. 686 vesicles and liposomes. Nano Lett 2005, 5 (8), 1615-1619.
- 687 Demurtas, D.; Guichard, P.; Martiel, I.; Mezzenga, R.; Hebert, C.; Sagalowicz, L., Direct 42.
- 688 visualization of dispersed lipid bicontinuous cubic phases by cryo-electron tomography. Nat 689 Commun 2015, 6, 8915.
- 690 Duesing, P. M.; Templer, R. H.; Seddon, J. M., Quantifying Packing Frustration Energy in 43. 691 Inverse Lyotropic Mesophases. Langmuir 1997, 13 (2), 351-359.
- 692 Tyler, A. I.; Shearman, G. C.; Brooks, N. J.; Delacroix, H.; Law, R. V.; Templer, R. H.; 44.
- 693 Ces, O.; Seddon, J. M., Hydrostatic pressure effects on a hydrated lipid inverse micellar Fd3m 694 cubic phase. Phys Chem Chem Phys 2011, 13 (8), 3033-3038.
- 695 45. Basham, M.; Filik, J.; Wharmby, M. T.; Chang, P. C.; El Kassaby, B.; Gerring, M.;
- 696 Aishima, J.; Levik, K.; Pulford, B. C.; Sikharulidze, I.; Sneddon, D.; Webber, M.; Dhesi, S. S.;

- Maccherozzi, F.; Svensson, O.; Brockhauser, S.; Naray, G.; Ashton, A. W., Data Analysis
 WorkbeNch (DAWN). *J Synchrotron Radiat* 2015, *22* (3), 853-858.
- 699 46. Filik, J.; Ashton, A. W.; Chang, P. C. Y.; Chater, P. A.; Day, S. J.; Drakopoulos, M.;
- 700 Gerring, M. W.; Hart, M. L.; Magdysyuk, O. V.; Michalik, S.; Smith, A.; Tang, C. C.; Terrill, N.
- J.; Wharmby, M. T.; Wilhelm, H., Processing two-dimensional X-ray diffraction and small-angle
- scattering data in DAWN 2. *Journal of applied crystallography* **2017**, *50* (Pt 3), 959-966.
- 703 47. Schindelin, J.; Arganda-Carreras, I.; Frise, E.; Kaynig, V.; Longair, M.; Pietzsch, T.;
- Preibisch, S.; Rueden, C.; Saalfeld, S.; Schmid, B.; Tinevez, J. Y.; White, D. J.; Hartenstein, V.;
- Eliceiri, K.; Tomancak, P.; Cardona, A., Fiji: an open-source platform for biological-image
 analysis. *Nat Methods* 2012, 9 (7), 676-682.
- 707 48. Tinevez, J. Y.; Perry, N.; Schindelin, J.; Hoopes, G. M.; Reynolds, G. D.; Laplantine, E.;
- 708 Bednarek, S. Y.; Shorte, S. L.; Eliceiri, K. W., TrackMate: An open and extensible platform for
- single-particle tracking. *Methods* **2017**, *115*, 80-90.
- 710